

Disposable electrochemical sensors for highly sensitive detection of chlorpromazine in human whole blood based on the silica nanochannel array modified screen-printed carbon electrode

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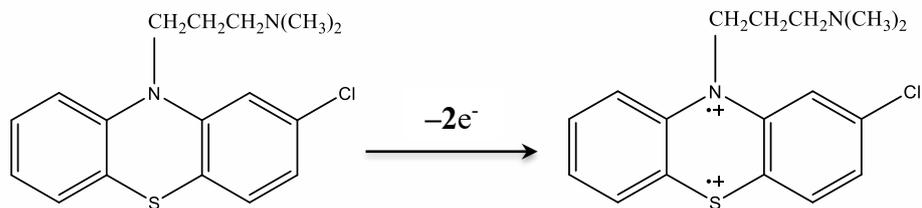
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S1. Electrochemical reaction of CPZ on the electrode surface



Scheme S1 Electrochemical reaction of CPZ on the electrode surface.

S2. Effect of scan rate on the CV responses

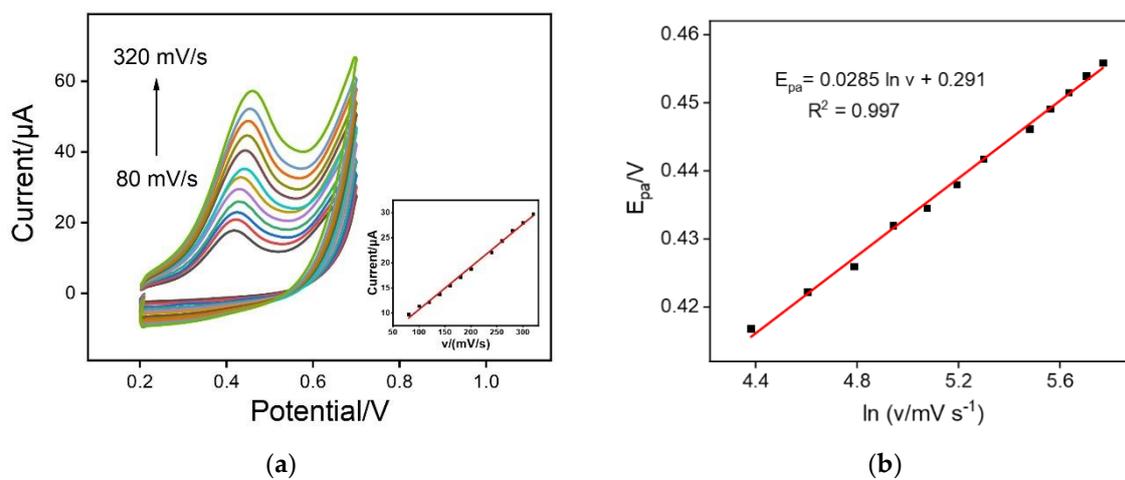


Figure S1 (a) Effect of scan rates (v) on the redox behavior of 20 μM CPZ in 0.1 M PBS (pH 6.0) at the VMSF/ErGO/SPCE. Inset depicts the linear relationship of anodic peak current with scan rate. (b) Relationship between anodic peak potential (E_{pa}) and $\ln v$.

S3. Optimization of experimental conditions

S3.1 preconcentration time

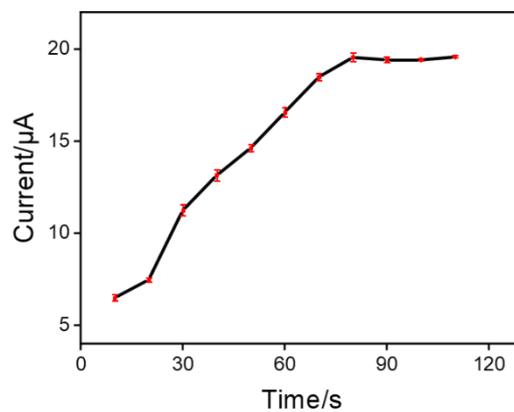


Figure S2 Time-dependent plots at the VMSF/ErGO/SPCE in 0.1 M PBS solution (pH 6.0) containing 20 μ M CPZ. The error bars represent the standard deviation (SD) of three measurements.

S3.2 pH of supporting electrolyte

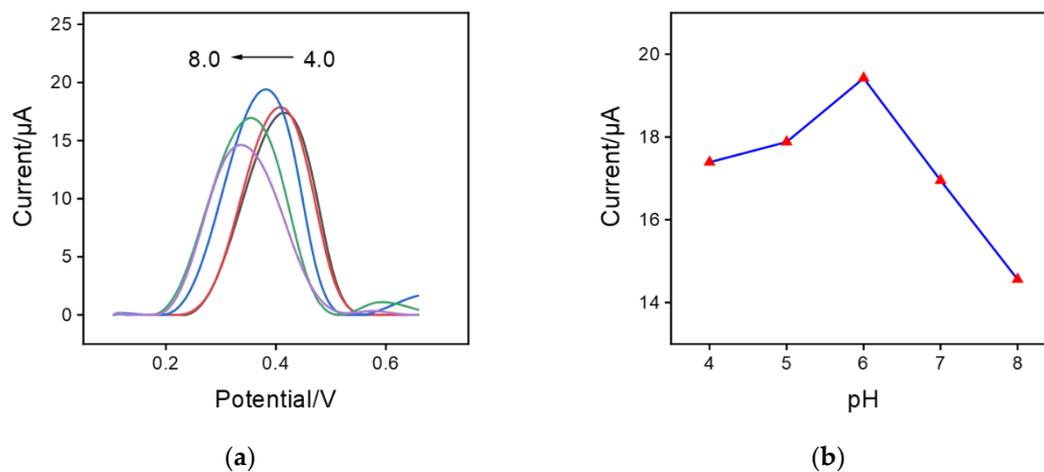


Figure S3 (a) DPV curves obtained at the VMSF/ErGO/SPCE in 0.1 M PBS solution containing 20 μ M CPZ at various pH values. (b) Effect of pH of supporting electrolyte on the anodic peak current of CPZ.

S4. Electrochemical detection of CPZ in human whole blood using bare SPCE and ErGO/SPCE

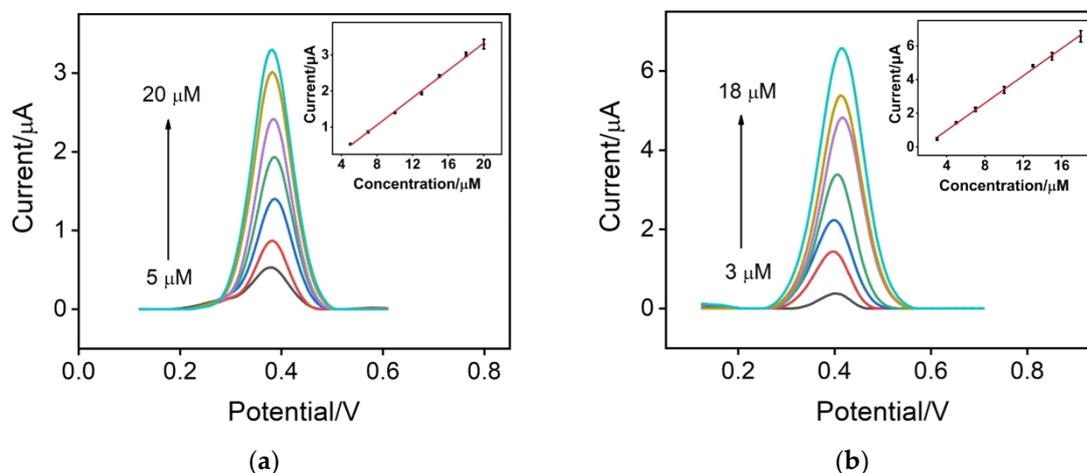


Figure S4 DPV curves of bare SPCE **(a)** and ErGO/SPCE **(b)** in human blood samples diluted by a factor of 50 using 0.1 M PBS solution (pH 6.0) containing different concentrations of CPZ. Insets are corresponding calibration curves and the error bars represent the SD of three measurements.

Table S1. Comparison of electrochemical detection performance towards CPZ at the various electrodes in 50-time diluted human whole blood samples

Electrode	Linear range (μM)	Sensitivity ($\mu\text{A } \mu\text{M}^{-1}$)	LOD (nM)
bare SPCE	5–20	0.1889	31.8
ErGO/SPCE	3–18	0.4050	14.8
VMSF/ErGO/SPCE	0.5–20	0.9239	6.5

S5. Anti-interference, stability and reproducibility ability of VMSF/ErGO/GCE

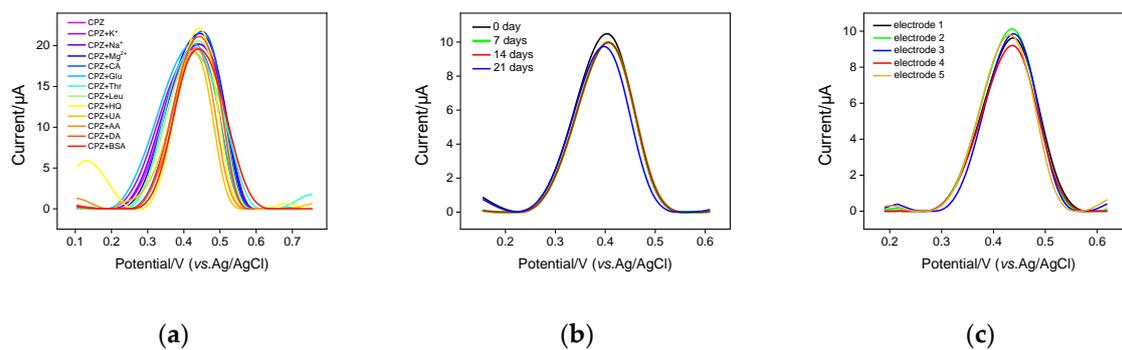


Figure S5 (a) DPV curves obtained from VMSF/ErGO/SPCE for detection of 20 μM CPZ in the presence and absence of added interfering species. The concentration of BSA is 6 μM and the concentration of other interfering species are 1 mM. Stability (b) and reproducibility (c) of sensors.

S6. Regeneration ability of VMSF/ErGO/GCE, ErGO/SPCE and bare SPCE

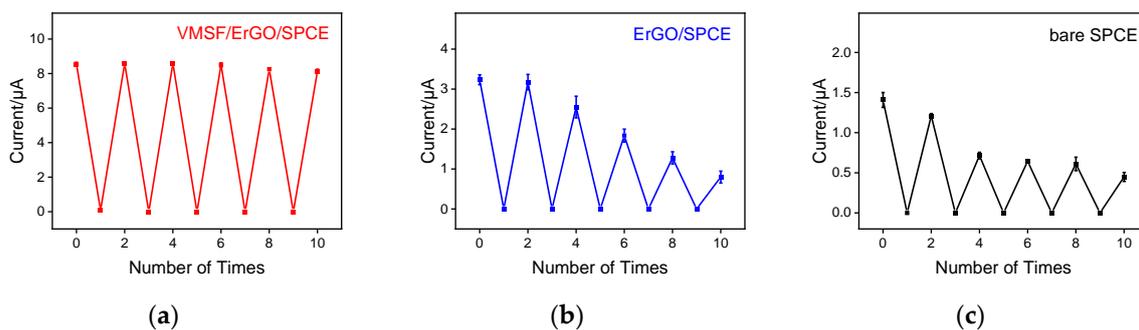


Figure S6 Peak currents and usage times curves of VMSF/ErGO/SPCE (a), ErGO/SPCE (b) and bare SPCE (c) in 50-time diluted human blood samples with or without 10 μM CPZ. To realize the regeneration, electrodes were soaked into a HCl-ethanol solution.

S7. Electrochemical detection of CPZ in undiluted human whole blood samples

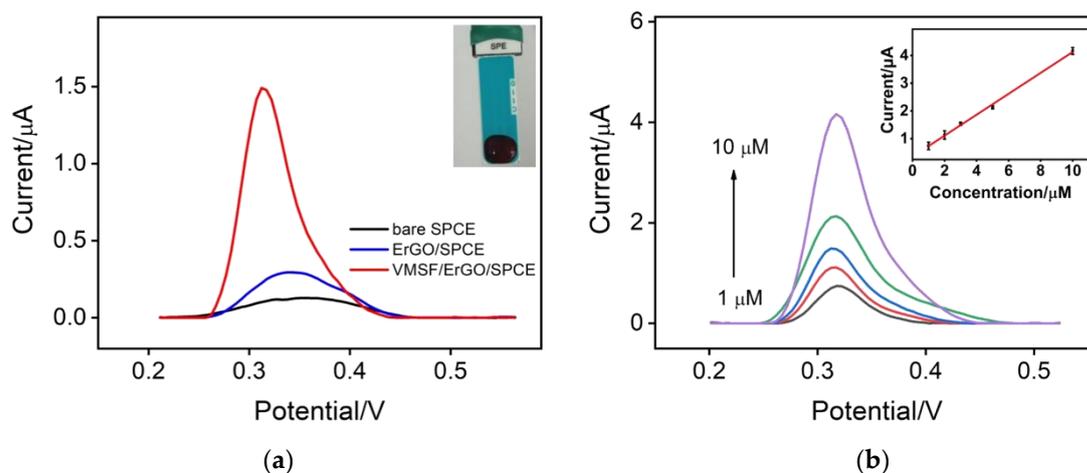


Figure S7 (a) DPV curves of bare SPCE, ErGO/SPCE and VMSF/ErGO/SPCE in human whole blood samples containing 3 μM CPZ; Inset is the photograph of VMSF/ErGO/SPCE used for analysis of CPZ in undiluted human whole blood. (b) DPV curves of VMSF/ErGO/SPCE in human blood samples containing CPZ ranging from 1 μM to 10 μM . Inset is the corresponding calibration curve and the error bars represent the SD of three measurements.