

# **Disposable electrochemical sensors for highly sensitive detection of chlorpromazine in human whole blood based on the silica nanochannel array modified screen-printed carbon electrode**

*Qianqian Han<sup>1,‡</sup>, Tongtong Zhang<sup>2,‡</sup>, Meifang Wang<sup>1</sup>, Fei Yan<sup>1,\*</sup> and Jiyang Liu<sup>1,\*</sup>*

<sup>1</sup> Key Laboratory of Surface & Interface Science of Polymer Materials of Zhejiang Province, Department of Chemistry, Zhejiang Sci-Tech University, Hangzhou 310018, China

<sup>2</sup> Key Laboratory of Integrated Oncology and Intelligent Medicine of Zhejiang Province, Department of Hepatobiliary and Pancreatic Surgery, Affiliated Hangzhou First People's Hospital, Zhejiang University School of Medicine, Hangzhou, 310006, China

<sup>‡</sup> These two authors contributed equally.

\* Corresponding author. E-mail: feifei19881203@126.com or yanfei@zstu.edu.cn (F.Y.); liujy@zstu.edu.cn (J.L.)

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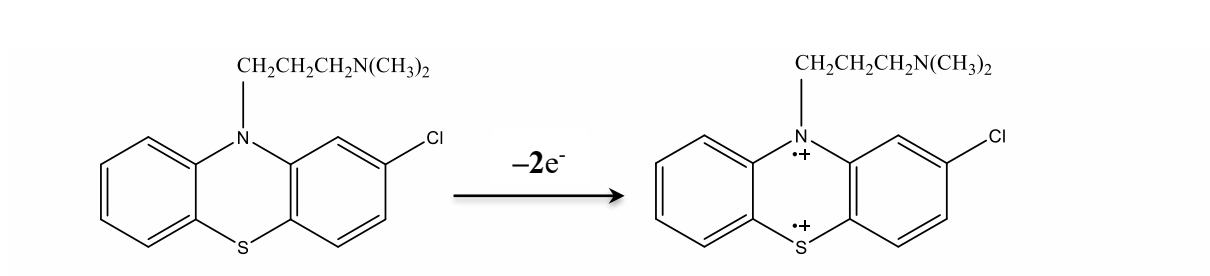
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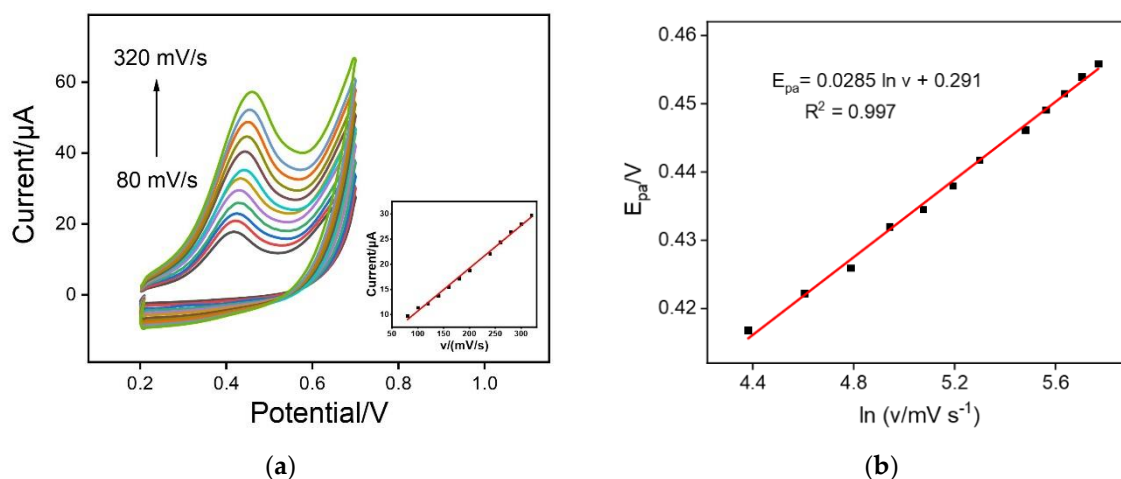
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### S1. Electrochemical reaction of CPZ on the electrode surface



**Scheme S1** Electrochemical reaction of CPZ on the electrode surface.

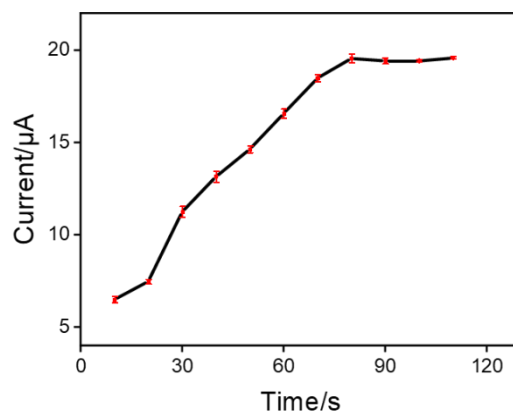
## S2. Effect of scan rate on the CV responses



**Figure S1** (a) Effect of scan rates ( $v$ ) on the redox behavior of 20  $\mu\text{M}$  CPZ in 0.1 M PBS (pH 6.0) at the VMSF/ErGO/SPCE. Inset depicts the linear relationship of anodic peak current with scan rate. (b) Relationship between anodic peak potential ( $E_{pa}$ ) and  $\ln v$ .

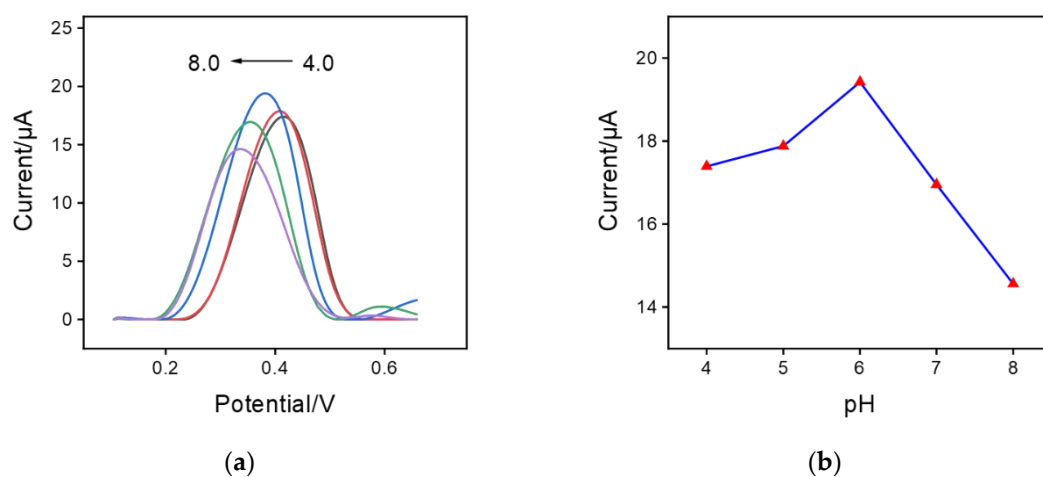
### S3. Optimization of experimental conditions

#### S3.1 preconcentration time



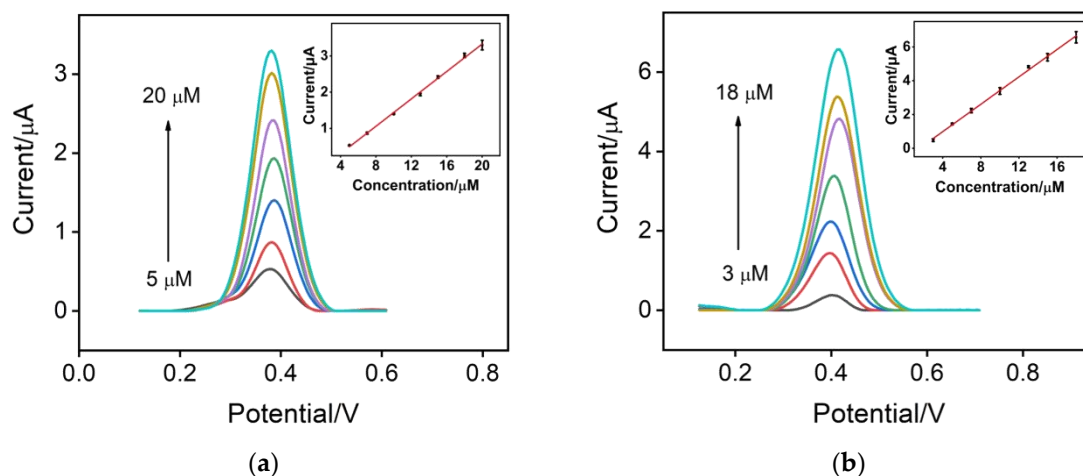
**Figure S2** Time-dependent plots at the VMSF/ErGO/SPCE in 0.1 M PBS solution (pH 6.0) containing 20  $\mu\text{M}$  CPZ. The error bars represent the standard deviation (SD) of three measurements.

### S3.2 pH of supporting electrolyte



**Figure S3** (a) DPV curves obtained at the VMSF/ErGO/SPCE in 0.1 M PBS solution containing 20  $\mu$ M CPZ at various pH values. (b) Effect of pH of supporting electrolyte on the anodic peak current of CPZ.

#### S4. Electrochemical detection of CPZ in human whole blood using bare SPCE and ErGO/SPCE

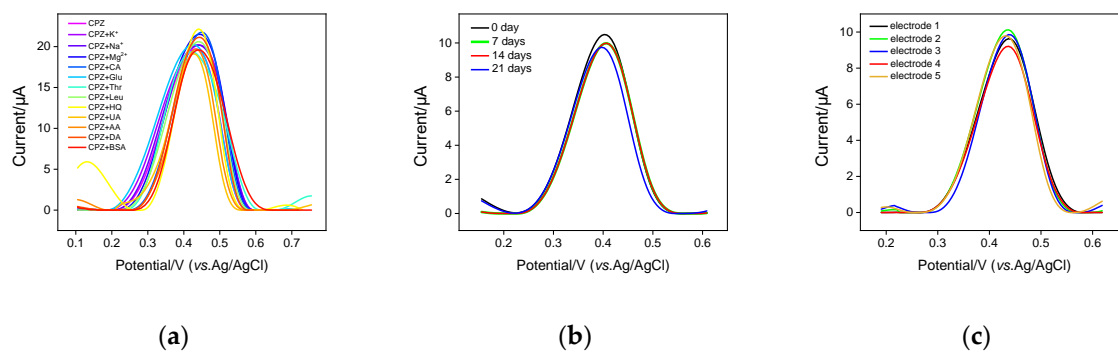


**Figure S4** DPV curves of bare SPCE **(a)** and ErGO/SPCE **(b)** in human blood samples diluted by a factor of 50 using 0.1 M PBS solution (pH 6.0) containing different concentrations of CPZ. Insets are corresponding calibration curves and the error bars represent the SD of three measurements.

**Table S1.** Comparison of electrochemical detection performance towards CPZ at the various electrodes in 50-time diluted human whole blood samples

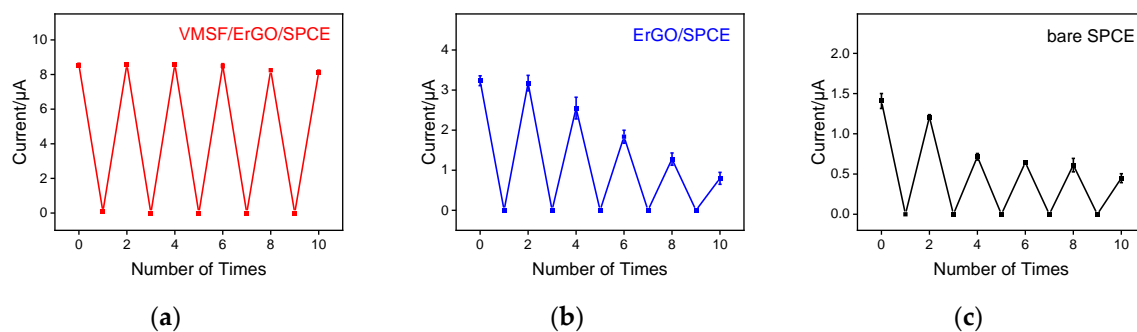
Electrode	Linear range (μM)	Sensitivity (μA μM <sup>-1</sup> )	LOD (nM)
bare SPCE	5–20	0.1889	31.8
ErGO/SPCE	3–18	0.4050	14.8
VMSF/ErGO/SPCE	0.5–20	0.9239	6.5

### S5. Anti-interference, stability and reproducibility ability of VMSF/ErGO/GCE



**Figure S5** (a) DPV curves obtained from VMSF/ErGO/SPCE for detection of 20  $\mu\text{M}$  CPZ in the presence and absence of added interfering species. The concentration of BSA is 6  $\mu\text{M}$  and the concentration of other interfering species are 1 mM. Stability (b) and reproducibility (c) of sensors.

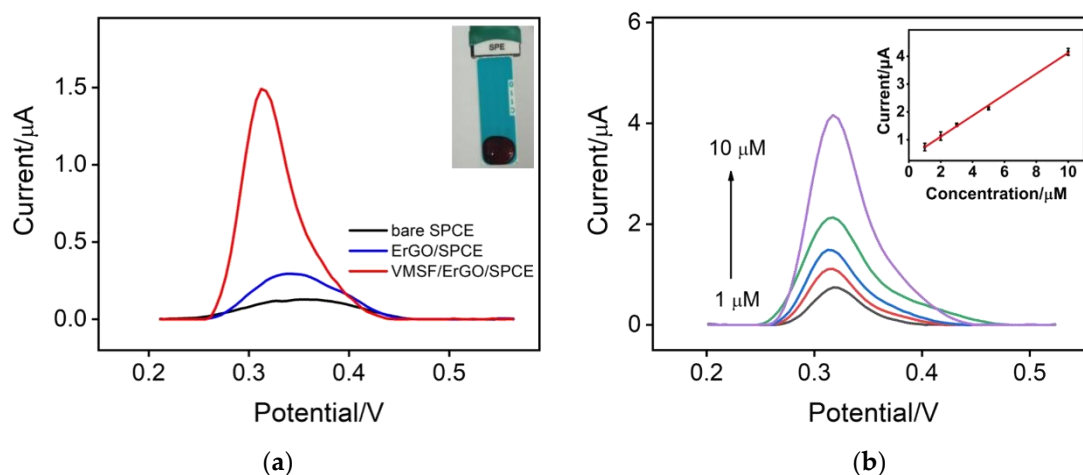
### S6. Regeneration ability of VMSF/ErGO/GCE, ErGO/SPCE and bare SPCE



**Figure S6** Peak currents and usage times curves of VMSF/ErGO/SPCE (a), ErGO/SPCE (b) and bare SPCE (c) in 50-time diluted human blood samples with or without 10  $\mu\text{M}$  CPZ. To realize the regeneration, electrodes were soaked into a HCl-ethanol solution.



### S7. Electrochemical detection of CPZ in undiluted human whole blood samples



**Figure S7** (a) DPV curves of bare SPCE, ErGO/SPCE and VMSF/ErGO/SPCE in human whole blood samples containing 3  $\mu\text{M}$  CPZ; Inset is the photograph of VMSF/ErGO/SPCE used for analysis of CPZ in undiluted human whole blood. (b) DPV curves of VMSF/ErGO/SPCE in human blood samples containing CPZ ranging from 1  $\mu\text{M}$  to 10  $\mu\text{M}$ . Inset is the corresponding calibration curve and the error bars represent the SD of three measurements.