

Supplementary File S2. Walkbot human–robotic interactive gait training system

The Walkbot system, which comprises the important biomechanical features of the interlimb ankle-knee-hip joint locomotor control to generate and assist the natural gait pattern, was developed based on the inverted pendulum model [1]. Its biomechanical features include the built-in kinematic and kinetic computing software (P&S Mechanics, Seoul, Korea), which synchronously analyses both kinematic (e.g., angular displacement) and kinetic (e.g., active and resistive ankle-knee-hip joint forces and torques) [1]. Kinematic data were sampled at 36 Hz using a built-in potentiometer in the Walkbot system. Each joint angle data was determined by the following equations in the schematic model (Figure S1):

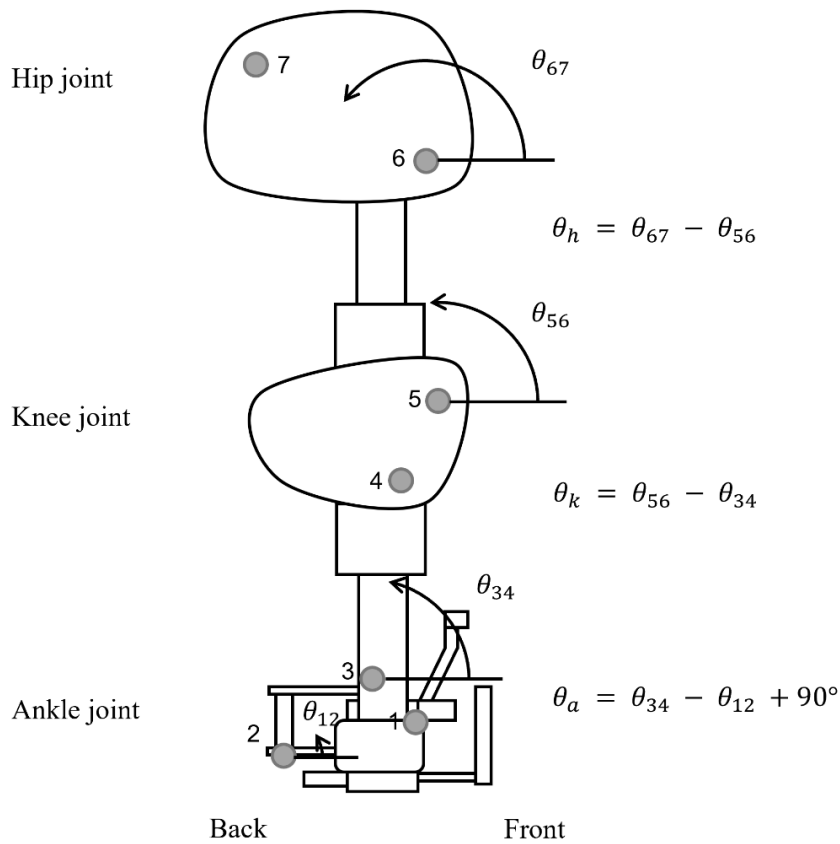


Figure S1. Lower-extremity kinematic joint angle calculation of the Walkbot system. Reproduced with permission from reference [2]. Reproduced with permission from Park C, Oh-Park M, Bialek A, Friel K, Edwards D, You JSH. published by Scientific Reports, 2021.

Kinetic software enables measurement of the forces and torques of the ankle-knee-hip joint related to walking and provides real-time biomechanical feedback to maximize the human-robotic interactive gait training. Based on the kinematic and anthropometric data, the force data were automatically computed and converted to joint torques. All ankle-knee-hip joint torque data were acquired by servomotors mounted in the Walkbot robotic system and used to accurately generate the most natural gait pattern [3] using each

patient's anthropometric data. The specific scheme of the position-based impedance control algorithm is illustrated in Figure S2.

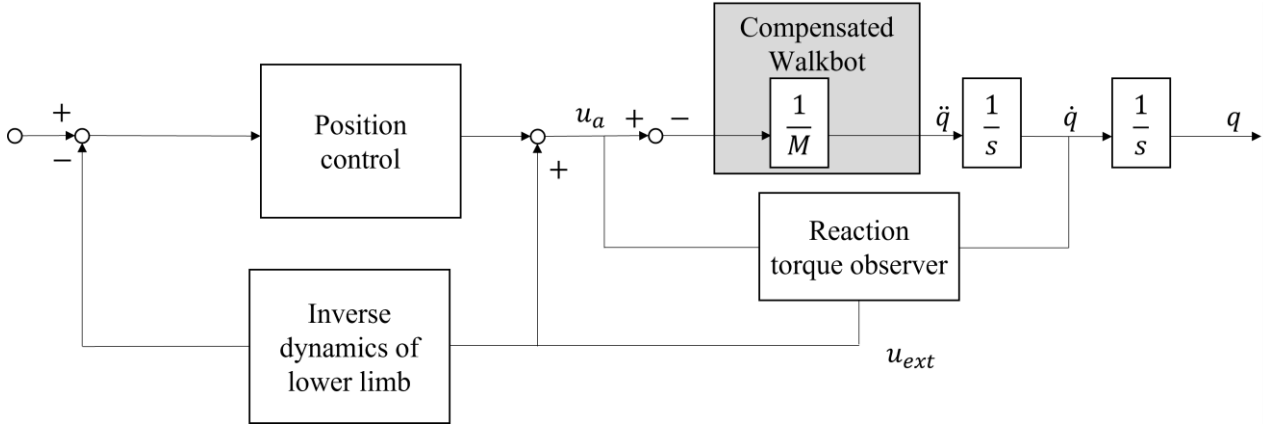


Figure S2. Scheme of the position-based impedance control system. Reproduced with permission from reference [2]. Reproduced with permission from Park C, Oh-Park M, Bialek A, Friel K, Edwards D, You JSH. published by Scientific Reports, 2021.

The force equation is formulated as:

$$u_{ext} = \frac{g}{s + g} (u_a + g\hat{F}(q)\dot{q} + \hat{F}(q)\dot{q}) - g\hat{F}(q)\dot{q}$$

where u_{ext} represents the estimated external torque from the reaction torque observer, $\frac{g}{s + g}$ is a lowpass filter, and g is its cutoff frequency.

References

1. Van Tran, Q.; Kim, S.; Lee, K.; Kang, S.; Ryu, J. Force/torque sensorless impedance control for indirect driven robot-aided gait rehabilitation system. In Proceedings of the 2015 IEEE International Conference on Advanced Intelligent Mechatronics (AIM), 2015; pp. 652-657.
2. Park, C.; Oh-Park, M.; Bialek, A.; Friel, K.; Edwards, D.; You, J.S.H. Abnormal synergistic gait mitigation in acute stroke using an innovative ankle-knee-hip interlimb humanoid robot: A preliminary randomized controlled trial. *Scientific Reports* **2021**, *11*, 22823.
3. Winter, D.A. *Biomechanics and motor control of human movement*; John Wiley & Sons: 2009.