



Article A Millimeter-Wave Fundamental Frequency CMOS-Based Oscillator with High Output Power

Thanh Dat Nguyen ¹, Hangue Park ² and Jong-Phil Hong ^{1,*}

- ¹ School of Electrical Engineering, Chungbuk National University, Cheongju 28644, Korea; ntdat@cbnu.ac.kr
- ² Department of Electrical and Computer Engineering, Texas A&M University, College Station, TX 77843, USA; hangue.park@tamu.edu
- * Correspondence: jphong@cbnu.ac.kr

Received: 24 September 2019; Accepted: 24 October 2019; Published: 27 October 2019



Abstract: The millimeter-wave imaging approach is a promising candidate to satisfy the unmet needs of real-time biomedical imaging, such as resolution, focal area, and cost. As a part of the endeavor to make millimeter-wave imaging more feasible, this paper presents a CMOS oscillator generating a high output power at the millimeter-wave frequency range, with a high fundamental oscillation frequency. The proposed oscillator adopts a frequency-selective negative resistance topology to improve the negative transconductance and to increase the fundamental frequency of oscillation. The proposed oscillator was implemented in a 65 nm bulk CMOS process. The measured highest output power is -2.2 dBm at 190 GHz while dissipating 100 mW from a 2.8 V supply voltage.

Keywords: oscillator; mm-wave; high output power; CMOS

1. Introduction

Real-time biomedical imaging is a crucial component of biomedical systems pursuing both a real-time diagnosis with the timely evaluation of the interested functional or pathophysiological conditions and a real-time treatment with the closed-loop optimization of the intervention [1,2]. Although high-resolution computed tomography (CT) and magnetic resonance imaging (MRI) provide the highest penetration depth over 10 cm with decent sub-mm resolution, they can be hardly used in real-time applications unless the resolution is significantly sacrificed, because of the time-consuming scanning and image processing [3,4]. Instead, ultrasound echography, X-ray mammography, confocal microscopy, near-infrared fluorescence (NIR), and optical coherence tomography (OCT) have been actively adopted for the real-time biomedical imaging applications for both clinical and research settings [5–7]. However, several limitations such as low resolution, small focal area, artifacts from bony structures, and high cost, still hinder the widespread usage of the real-time biomedical imaging.

The millimeter-wave (mm-wave) frequency range, which is defined as a range from 30 to 300 GHz, has recently gained a lot of attention from researchers due to its massive potential to be used for real-time high-resolution biomedical imaging, radar imaging, and spectroscopy [8–11]. The mm-wave imaging approach can provide several advantages over the currently-available imaging solutions, such as: (1) low cost with well-established semiconductor process, (2) high-resolution ranging from sub-mm to sub-cm range, (3) low safety risk with non-ionizing radiation, and (4) easy examination process for doctors and patients with integrated handheld devices [8–14]. The mm-wave imaging approach has been showing its feasibility in recent years. For example, a complete dielectric profile of breast cancer could be reconstructed [13] and properties of the early-stage skin cancer tissues could be detected [14], by the mm-wave imaging technique.

To implement the imaging system at the mm-wave frequency range, the implementation of a signal source with high output power is a big challenge because of the parasitic components that significantly

attenuate the output power. Note that the output power matters not just for the penetration depth but for the spatial resolution with a better signal-to-noise ratio. Among several candidates that can implement a high-quality signal source in the mm-wave frequency range, the CMOS technology stands out because of its reliability, low cost, compact size, and advantages of system-on-a-chip integration [15–17]. However, CMOS technology has difficulties in implementing signal source at mm-wave frequency range, because of the limited output power with ~300 GHz maximum oscillation frequency (f_{max}) where unilateral power gain becomes unity [18–20].

Recently, several works have been reported to address the challenges in the mm-wave signal source design [21-29]. An oscillator in [27] operates at a center frequency of 190.5 GHz with a maximum output power of -2.1 dBm. However, this oscillator was implemented with an advanced and expensive SiGe compound semiconductor. A signal source, which is presented in [28] and uses the harmonic frequency to overcome the low f_{max} of the CMOS technology, generates a low output power of -4.8 dBm at the 2nd harmonic frequency of 239 GHz. However, the generated output power from the harmonic oscillator is low. Another oscillator in [29] generates an output power of -3.8 dBm at the 2nd harmonic frequency of 163.5 GHz at a typical supply voltage of 1.2 V. However, the maximum output power of 1 dBm at 164.6 GHz was measured at the supply voltage of 2 V, which is much higher than the typical supply voltage guaranteed in a 65 nm CMOS process, which can cause voltage stress and raise reliability problems in active devices. In [25], another approach, a fundamental frequency cross-coupled oscillator (XCO) with a capacitive-load-reduction-circuit (CLRC) technique, was presented to address the limitations of the CMOS technology. This approach improves the oscillation frequency by suppressing the effect of the load capacitance on the oscillation frequency. Moreover, a differential to single (DTS) transformer is adopted at the output port of the presented topology to enhance the output power.

This paper proposes a novel mm-wave frequency CMOS oscillator with a high output power and a high oscillation frequency by stacking a frequency-selective negative resistance (FSNR) circuit on the top of the XCO with CLRC which is presented in [25]. The stack structure adds an additional negative resistance which is generated by a FSNR circuit in parallel with a negative resistance of the oscillator core, so a higher output power can be obtained. In addition, the proposed oscillator operates at a higher oscillation frequency since the equivalent inductive reactance of the FSNR circuit combines in parallel with CLRC. Measurement results of the proposed oscillator at 190 GHz show the highest output power among reported oscillators in similar oscillation frequency range, supply voltage, and 65 nm CMOS process.

In Section 2, the structure and effect of the FSNR circuit on the oscillation frequency and negative resistance of proposed mm-wave oscillator are analyzed. The oscillation frequency and the negative resistance of the conventional XCO, the XCO with CLRC, and the proposed oscillator are compared. Section 3 presents measurement setups and measurement results of the implemented proposed oscillator. Finally, Section 4 summarizes the findings in this paper.

2. The Proposed Millimeter-Wave Oscillator

Figure 1 shows the schematic of the conventional XCO, which consists of two NMOS transistors (M_1-M_2) , an inductor L_{tank} , and two buffer transistors (M_3-M_4) . In the conventional XCO, the buffer transistors are directly connected to the main resonant tank, so the parasitic capacitance C_{GS} at the gate terminals of buffer transistors decrease the fundamental oscillation frequency. Figure 1b shows the schematic the XCO with CLRC [25]. In the XCO with CLRC, the CLRC comprises the gates of buffer transistors that are connected to the main resonant tank through a transformer. The transformer in the CLRC couples with the signal from a primary winding L_1 to a secondary winding L_2 , by a coupling factor k_1 . The function of CLRC is to suppress the effect of the load capacitance on the fundamental oscillation frequency [25]. The DTS transformer is constructed by L_3 and L_4 , at the output port to improve the output power by converting two differential signals into one single-ended signal.

As a result, the oscillation frequency and the output power of the XCO with CLRC are higher than that of the conventional XCO.

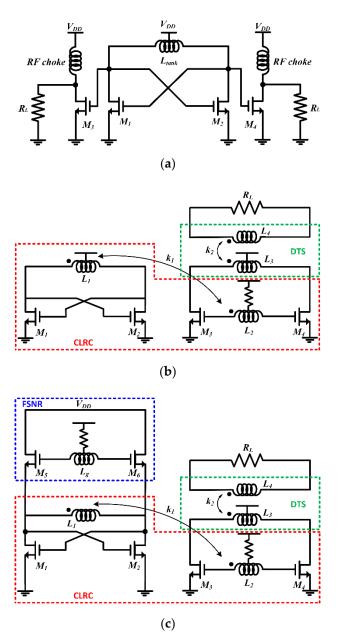


Figure 1. Schematics of (a) the conventional XCO; (b) the XCO with CLRC; (c) the proposed oscillator.

Figure 1c shows the proposed oscillator structure. The proposed oscillator is formed by stacking an FSNR at the top of the main resonant tank of the XCO and the oscillation signals are coupled through CLRC and the DTS transformer. The FSNR structure is formed by two transistors (M_5-M_6) and an inductor L_g that is connected at the gate terminals of M_5 and M_6 . Resistors are connected to the center taps of L_2 and L_g to guarantee the differential mode operation by suppressing the common mode operation of the proposed oscillator. These resistors also protect transistors from breakdown by limiting the inrush current flowing from a power supply to the gates of the transistors at the turn-on moment.

Figure 2a shows a half-circuit FSNR, so the inductance value of the L_g is half of L_g in the proposed oscillator. The FSNR circuit provides a selective characteristic depending on the oscillation frequency [12]. Figure 2b shows a small signal equivalent circuit of the half-circuit FSNR. A parasitic capacitance C_{gs} and a dependent current source $g_m V_1$ are the only components accounted for in the

small-signal equivalent circuit of a transistor to simplify the analysis and to obtain meaningful and tractable equations. The calculation of the input impedance looking at the source terminal of the transistor of the half circuit FSNR is based on the small-signal equivalent circuit in Figure 2b. The calculated input impedance of this circuit has two solutions. When the oscillation frequency of oscillator ω is lower than $\sqrt{2/LgCgs}$, the input impedance of the half circuit FSNR, shown in Figure 2c, is equivalent to a capacitor in parallel with a lossy resistance. Due to the lossy resistance, the total equivalent negative resistance is decreased, so the output power is decreased. In contrast, when $\omega > \sqrt{2/LgCgs}$, the input impedance of the half-circuit FSNR is equivalent to an inductor in parallel with a negative resistance as shown in Figure 2d. The solution in the case of $\omega > \sqrt{2/LgCgs}$ is preferred because it provides a high oscillation frequency and a high output power that are crucial in the mm-wave oscillator design.

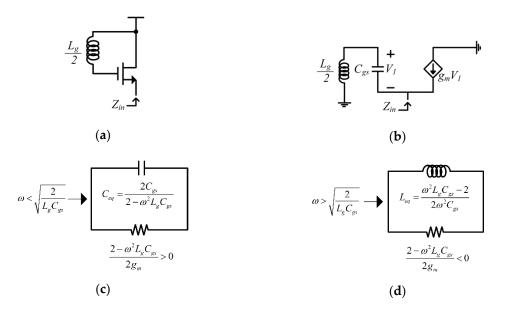


Figure 2. (**a**) The FSNR circuit; (**b**) its equivalent small-signal circuit, equivalent circuit of FSNR with; (**c**) capacitive reactance, and; (**d**) inductive reactance.

Figure 3 shows the small-signal equivalent circuits of the conventional XCO, the XCO with CLRC, and the proposed oscillator. From Figure 3a, the oscillation frequency of the conventional XCO is:

$$\omega_{XCO}^2 = \frac{1}{\sqrt{L_{tank}(C_{tank} + C_L)}} \tag{1}$$

where L_{tank} is the total inductance value of the oscillator tank, C_{tank} is the total capacitance value of the oscillator tank, and C_L is the total load capacitance. From Figure 3b, the oscillation frequency of the XCO witch CLRC is:

$$\omega_{CLRC}^2 = \frac{L_1 C_{tank} + L_2 C_L \mp \sqrt{L_1^2 C_{tank}^2 + L_2^2 C_L^2 - 2C_{tank} C_L (L_1 L_2 - 2M_1^2)}}{2(L_1 L_2 - M_1^2) C_{tank} C_L}$$
(2)

where L_1 is the total inductance value of the oscillator tank, L_2 is the total inductance value at the gate of the buffer transistor, and mutual conductance $M_1 = k_1 \sqrt{L_1 L_2}$ with k_1 being the coupling factor between L_1 and L_2 . From Figure 3c, the oscillation frequency of the proposed oscillator is:

$$\omega_{proposed}^{2} = \frac{LL_{1}C_{tank} + (LL_{2} + L_{1}L_{2} - M^{2})C_{L} \mp \sqrt{L^{2}L_{1}^{2}C_{tank}^{2} + (LL_{2} + L_{1}L_{2} - M^{2})^{2}C_{L}^{2} - 2C_{tank}C_{L}L(LL_{1}L_{g} + L_{1}^{2}L_{2} - (2L - L_{1})M_{1}^{2})}{2(L_{1}L_{2} - M_{1}^{2})LC_{tank}C_{L}}$$
(3)

where $L = (\omega^2 C_{gs} L_g - 2)/2\omega^2 C_{gs}$, and C_{gs} is the gate-source capacitance of transistors (M₅–M₆), L_g is the inductor at the gate terminal of transistors (M₅–M₆).

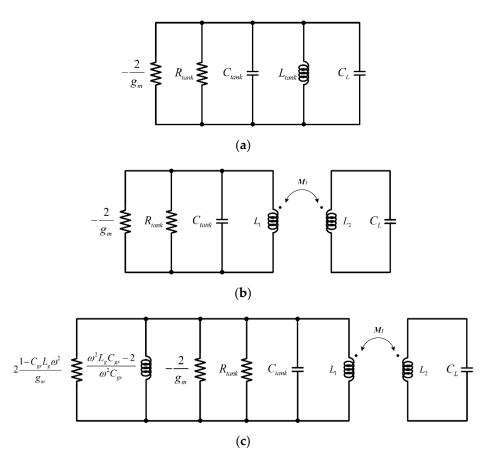


Figure 3. Small signal equivalent circuits of: (**a**) conventional XCO; (**b**) XCO with CLRC; (**c**) proposed oscillator.

Figure 4a shows the calculated oscillation frequencies of three topologies shown in Figure 1 versus L_g from Equations (1)–(3) with $g_m = 8$ mS, $C_{tank} = C_L = 10$ fF, $C_{gs} = 9$ fF, $L_{tank} = L_1 = L_2 = 40$ pH, and $M_1 = 20$ pH. In Figure 4a, the oscillation frequency of the proposed oscillator decreases with an increase of L_g . As can be seen in Figure 4a, the oscillation frequency of the proposed oscillator decreases with CLRC (142 GHz) and the conventional XCO (123 GHz), respectively. The circuit simulation was also carried out to verify the validity of the theory and the simulation results are plotted in Figure 4a. A BSIM4 model transistor was used in the circuit simulation. The simulation results agree with the theory equation about the trend of the oscillation frequency of the prosed oscillator with the change of L_g . The simulated oscillation frequency. This discrepancy is due to the simplification in the small-signal equivalent model of transistor. Nonetheless, the simulation results still show that the proposed oscillator has a higher oscillation frequency than that of the others, overall, in the simulated range of L_g . To operate around 200 GHz, an inductance value smaller than 100 pH of L_g was selected.

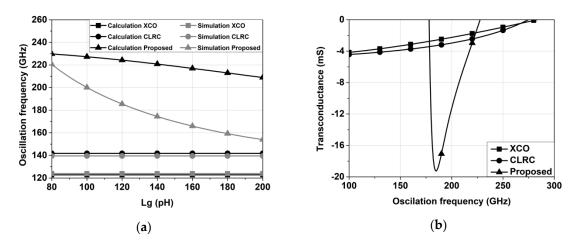


Figure 4. (a) Calculation and simulation results of oscillation frequency with various inductance values of L_g ; and (b) simulation results of the negative transconductance of conventional XCO, XCO with CLRC, and the proposed oscillator.

Moreover, the proposed oscillator has a better start-up condition and output power than those of the conventional XCO and the XCO with CLRC. The negative resistance of the conventional XCO and the XCO with CLRC is $-2/g_m$ while that of the proposed oscillator is $-2/g_m||2(1-C_{gs}L_g\omega^2)/g_m$. An additional negative resistance $2(1-C_{gs}L_g\omega^2)/g_m$ generated from the FSNR circuit gives rise to a better start-up condition and higher output power in the proposed oscillator. The circuit simulation was performed to verify the negative conductance improvement of the proposed oscillator. The simulated negative conductance of three structures with an identical oscillation frequency of 200 GHz is shown in Figure 4b. At 200 GHz target frequency, the negative resistance of the conventional XCO and XCO with CLRC is -2.2 mS and -2.9 mS, respectively, whereas the negative resistance of the proposed oscillator is -11.3 mS, as shown in Figure 4b. Therefore, the negative resistance of the proposed oscillator is almost 4 times higher than that of the XCO with CLRC, and five times higher than that of the conventional XCO with CLRC.

Passive devices are designed and simulated using the HFSS electromagnetic simulation tool. Figure 5 shows the passive devices of the proposed oscillator. Passive devices are implemented at two top metal layers that are a UTM metal layer with a thickness of 3.3 μ m and a thick metal layer with a thickness of 0.9 μ m. The CLRC transformer is implemented as a coplanar structure on the UTM metal to obtain a high Q-factor, where the Q-factor of L_1 is 35 and Q-factor of L_2 is 43. When the space between the primary inductor L_1 and secondary inductor L_2 is 3 μ m, the coupling factor k_1 is 0.4. The gate inductor L_g is also implemented on the UTM metal layer with an inductance value of 88 pH and a Q-factor of 34. The DTS transformer is implemented as a vertical stack structure to maximize the coupling factor, and, thus, the DTS transformer has a high coupling factor k_2 of 0.73. A capacitor with the capacitance value of 5 fF is implemented at the output port of the DTS transformer to maximize the output power transferred to the output load.

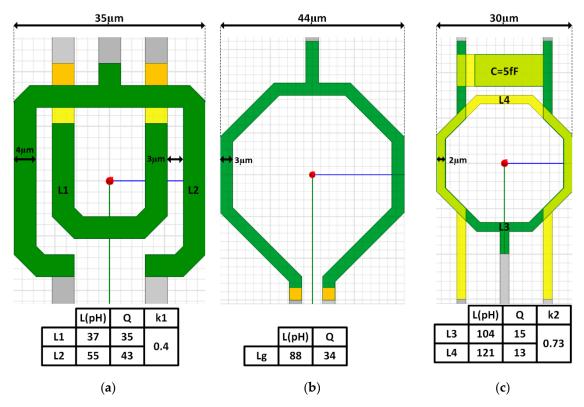


Figure 5. Layout of (a) the CLRC transformer; (b) the gate inductor L_g ; (c) the DTS transformer.

3. Measurement Results

The proposed oscillator is fabricated in a 65 nm bulk CMOS process. Figure 6 shows the implemented chip micrograph of the proposed oscillator with an area including pads of $360 \times 283 \,\mu\text{m}^2$. The area of the output pad is designed smaller than the power pads (V_{DD} and V_C) and ground pads (GND) to minimize parasitic capacitance and loss due to coupling with the lossy substrate.

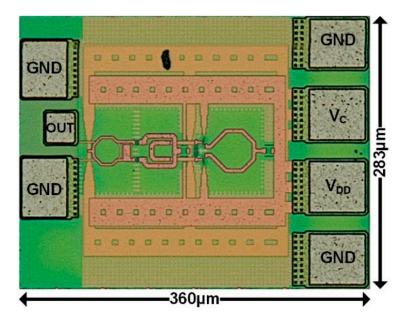


Figure 6. Chip micrograph of the proposed oscillator.

The output spectrum of the proposed oscillator was measured based on the measurement setup using the spectrum analyzer, as shown in Figure 7a. A GGB DC Probe was connected to the power

pads of the fabricated chip. The GGB DC probe with a GPPG pin configuration provided two paths to supply two different DC voltage levels to operate the fabricated circuit. The output pads were connected to a GGB model 220 probe with GSG pin configuration to sense the output power. Then the output power was conducted through the WR-5 waveguide to an OML WR-5 harmonic mixer. At the harmonic mixer, the output signal from the proposed oscillator was down-converted by mixing it with a LO signal generated from an R&S FSW26 spectrum analyzer. The down-converted output signal from the harmonic mixer was received, and the oscillation frequency was automatically calculated, by the R&S FSW26 spectrum analyzer. Figure 8a shows the measured oscillation frequency of 190 GHz. Figure 9a shows the effect of voltage supply on oscillation frequency. The measurement result shows that the oscillation frequency changed from 193.1 to 190.1 GHz when V_{DD} was increased from 1.4 to 2.8 V. At $V_{DD} = 2.8$ V, the measured oscillation frequency was 10 GHz lower than the simulated oscillation frequency because of the extrapolation model of active devices at mm-wave frequency range.

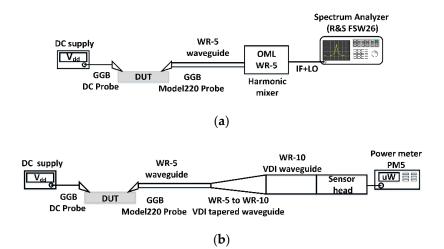


Figure 7. (a) Output spectrum measurement setup; (b) output power measurement setup.

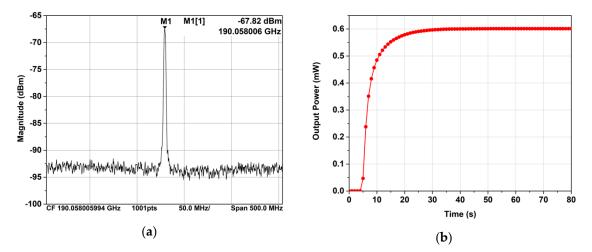


Figure 8. Measured (a) output spectrum; (b) output power of the proposed oscillator.

The output power of the fabricated proposed oscillator was measured by the measurement setup using a power meter, as shown in Figure 7b. The output power was transferred to a power meter PM5 through a GGB model 220 probe, a WR-5 waveguide, a WR-5 to WR-10 VDI tapered waveguide, a WR-10 VDI waveguide, and a sensor head. The total transmission loss from the probe to the WR-10 VDI waveguide was 5.1 dB. The output power level was calculated by a PM5 power meter. Figure 8b shows the highest measured output power was 0.6 mW or -2.2 dBm at $V_{DD} = 2.8$ V and $V_C = 1$ V. At $V_{DD} = 2.8$ V, the voltage across each transistor was approximately 1.4 V because of the

stack structure. Figure 9b shows the effect of voltage supply on output power. The measured output power increased from 0.254 to 0.6 mW and the simulated output power increased from 1.1 to 5.9 mW when V_{DD} increased from 1.4 to 2.8 V. The large discrepancy between the measured output power and the simulated output power was due to the extrapolation model of active devices at mm-wave frequency range.

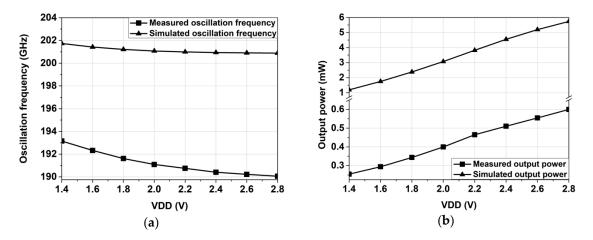


Figure 9. (a) Measured oscillation frequency and simulated oscillation frequency; (b) measured output power and simulated output power of the proposed oscillator with the change of voltage supply V_{DD} .

Table 1 shows the performance comparison of this work with the previous state of the art. The proposed oscillator generates a competitive output power at a high fundamental frequency with a compact chip area. Though the power consumption of the proposed oscillator is higher than that of the oscillator in [25], the output power of the proposed oscillator is 0.8 dB or 17% higher than the output power of the oscillator in [25]. This is a worthy trade-off in designing an mm-wave CMOS oscillator.

	[27]	[28]	[29]	[25]	This Work
Technology	0.13 μm SiGe	65 nm CMOS	65 nm CMOS	65 nm CMOS	65 nm CMOS
Harmonic	2nd Harmonic	2nd Harmonic	2nd Harmonic	Fundamental	Fundamental
Frequency (GHz)	190.5	239	164.6	219	190
Pout (dBm)	-2.1	-4.8	1	-3	-2.2
# cores	1	1	1	1	1
DC Power (mW)	183/294	18.5	88	24	100
DC-to-RF eff. (%)	0.22	1.79	1.43	2	0.6
Area (mm ²)	0.64	0.18	0.1	0.105	0.1
Measurement	Probe	Probe	Probe	Probe	Probe

Table 1. Performance comparison with state-of-the-art mm-wave oscillators.

4. Conclusions

A CMOS oscillator with a high fundamental oscillation frequency, which is suitable for generating a high output power at the mm-wave frequency range, is introduced in this paper. Firstly, a high fundamental frequency and high output power CLRC oscillator presented in [25] is adopted. Next, a FSNR circuit is stacked on top of the CLRC oscillator core to increase output power by adding a negative resistor in parallel to the oscillator core, and to increase oscillation frequency by adding an equivalent inductor in parallel to the oscillator core. The proposed oscillator at 190 GHz shows the highest measured output power among reported oscillators in a similar oscillation frequency range, supply voltage, and 65 nm CMOS process. The proposed topology can be used as a compact and high-resolution signal source for bio-imaging systems. Author Contributions: Conceptualization, T.D.N. and J.-P.H.; methodology, T.D.N. and J.-P.H.; circuit analysis, T.D.N. and J.-P.H.; investigation, T.D.N. and J.-P.H.; Writing—Original draft preparation, T.D.N., J.-P.H. and H.P.; Writing—Review and editing, T.D.N., J.-P.H. and H.P.

Funding: This work was supported by the LG Yonam Foundation (Korea). This work was also supported by the Basic Science Research Program through the National Research Foundation of Korea (NRF) funded by the Ministry of Education (NRF-2018R1D1A1B07042607).

Conflicts of Interest: The authors declare no conflict of interest. The funders had no role in the design of the study; in the collection, analyses, or interpretation of data; in the writing of the manuscript, or in the decision to publish the results.

References

- Goyal, S.; Kataria, T. Image guidance in radiation therapy: Techniques and applications. *Radiol. Res. Pract.* 2014, 2014, 705604. [CrossRef] [PubMed]
- 2. Krook-Magnuson, E.; Gelinas, J.N.; Soltesz, I.; Buzsáki, G. Neuroelectronics and biooptics: Closed-loop technologies in neurological disorders. *JAMA Neurol.* **2015**, *72*, 823–829. [CrossRef] [PubMed]
- 3. Müller, N.L. Computed tomography and magnetic resonance imaging: Past, present and future. *Eur. Respir. J.* **2002**, *19* (Suppl. 35), 3s–12s.
- 4. Wang, X.; Li, L.; Hu, C.; Qiu, J.; Xu, Z.; Feng, Y. A comparative study of three CT and MRI registration algorithms in nasopharyngeal carcinoma. *J. Appl. Clin. Med. Phys.* **2009**, *10*, 3–10. [CrossRef]
- 5. Huang, Q.; Zeng, Z. A review on real-time 3D ultrasound imaging technology. *BioMed Res. Int.* 2017, 2017, 6027029. [CrossRef]
- 6. Fear, E.C.; Li, X.; Hagness, S.C.; Stuchly, M.A. Confocal microwave imaging for breast cancer detection: Localization of tumors in three dimensions. *IEEE Trans. Biomed. Eng.* **2002**, *49*, 812–822. [CrossRef]
- Neuman, B.P.; Eifler, J.B.; Castanares, M.; Chowdhury, W.H.; Chen, Y.; Mease, R.C.; Ma, R.; Mukherjee, A.; Lupold, S.E.; Pomper, M.G.; et al. Real-time, near-infrared fluorescence imaging with an optimized dye/light source/camera combination for surgical guidance of prostate cancer. *Clin. Cancer Res.* 2015, 21, 771–780. [CrossRef]
- 8. Taylor, Z.D.; Garritano, J.; Sung, S.; Bajwa, N.; Bennett, D.B.; Nowroozi, B.; Tewari, P.; Sayre, J.W.; Hubschman, J.P.; Deng, S.X.; et al. THz and mm-wave sensing of corneal tissue water content: In vivo sensing and imaging results. *IEEE Trans. Terahertz Sci. Technol.* **2015**, *5*, 184–196. [CrossRef]
- 9. Wu, T.; Rappaport, T.S.; Collins, C.M. The human body and millimeter-wave wireless communication systems: Interactions and implications. In Proceedings of the 2015 IEEE International Conference on Communications (ICC), London, UK, 8–12 June 2015; pp. 2423–2429.
- 10. Fahad, A.K.; Ruan, C.; Chen, K. A Wideband Terahertz Transmissive Polarization Manipulator Based on Metasurfaces. *Electronics* **2019**, *8*, 1068. [CrossRef]
- 11. Meng, J.; Zhang, D.; Ji, G.; Yao, C.; Jiang, C.; Liu, S. Design of a 335 GHz Frequency Multiplier Source Based on Two Schemes. *Electronics* **2019**, *8*, 948. [CrossRef]
- 12. Shayei, A.; Kavehvash, Z.; Shabany, M. Improved-resolution millimeter-wave imaging through structured illumination. *Appl. Opt.* **2017**, *56*, 4454–4465. [CrossRef] [PubMed]
- Di Meo, S.; Matrone, G.; Pasian, M.; Bozzi, M.; Perregrini, L.; Magenes, G.; Mazzanti, A.; Svelto, F.; Summers, P.E.; Renne, G.; et al. High-resolution mm-Wave imaging techniques and systems for breast cancer detection. In Proceedings of the 2017 IEEE MTT-S International Microwave Workshop Series on Advanced Materials and Processes for RF and THz Applications (IMWS-AMP), Pavia, Italy, 20–22 September 2017; pp. 1–3.
- 14. Mirbeik-Sabzevari, A.; Tavassoian, N.; Ashinoff, R. Ultra-High-Resolution Millimeter-Wave Imaging: A New Promising Skin Cancer Imaging Modality. In Proceedings of the 2018 IEEE Biomedical Circuits and Systems Conference (BioCAS), Cleveland, OH, USA, 17–19 October 2018; pp. 1–4.
- 15. Wang, Z.; Chiang, P.Y.; Nazari, P.; Wang, C.C.; Chen, Z.; Heydari, P. A CMOS 210-GHz fundamental transceiver with OOK modulation. *IEEE J. Solid-State Circuits* **2014**, *49*, 564–580. [CrossRef]
- 16. Park, J.D.; Kang, S.; Niknejad, A.M. A 0.38 THz fully integrated transceiver utilizing a quadrature push-push harmonic circuitry in SiGe BiCMOS. *IEEE J. Solid-State Circuits* **2012**, *47*, 2344–2354. [CrossRef]
- 17. Cooper, K.B. A high-resolution imaging radar at 580 GHz. *IEEE Microw. Wireless Compon. Lett.* **2008**, *18*, 64–66. [CrossRef]

- Choi, K.U.; Nguyen, T.D.; Choi, S.G.; Hong, J.P. High Frequency Buffer-Feedback Oscillator with an RF Negative-Resistance Circuit. *IEEE Access* 2018, *6*, 20964–20970. [CrossRef]
- 19. Bamer, H.; Momeni, O. A high-gain mm-Wave amplifier design: An analytical approach to power gain boosting. *IEEE J. Solid-State Circuits* **2017**, *52*, 357–370. [CrossRef]
- 20. Razavi, B. A 300-GHz fundamental oscillator in 65-nm CMOS technology. *IEEE J. Solid-State Circuits* **2011**, *46*, 894–903. [CrossRef]
- 21. Li, C.H.; Ko, C.L.; Kuo, C.N.; Kuo, M.C.; Chang, D.C. A 340 GHz Triple-Push Oscillator with Differential Output in 40nm CMOS. *IEEE Microw. Wireless Compon. Lett.* **2014**, *24*, 863–865. [CrossRef]
- 22. Grzyb, J.; Zhao, Y.; Pfeiffer, U.R. A 288-GHz Lens-Integrated Balanced Triple-Push Source in a 65 nm CMOS Technology. *IEEE J. Solid-State Circuits* 2013, *48*, 1751–1761. [CrossRef]
- 23. Jameson, S.; Halpern, E.; Socher, E. 20.4 A 300 GHz Wirelessly Locked 2x3 Array Radiating 5.4dBm with 5.1% DC-to-RF Efficiency in 65nm CMOS. In Proceedings of the 2016 IEEE International Solid-State Circuits Conference (ISSCC), San Francisco, CA, USA, 31 January–4 February 2016; pp. 348–349.
- Tousi, Y.M.; Momeni, O.; Afshari, E. A 283-to-296GHz VCO with 0.76 mW Peak Output Power in 65 nm CMOS. In Proceedings of the 2012 IEEE International Solid-State Circuits Conference(ISSCC), San Francisco, CA, USA, 19–23 February 2012; pp. 258–260.
- 25. Kwon, H.T.; Nguyen, D.; Hong, J.P. A 219-GHz fundamental oscillator with 0.5 mW peak output power and 2.08% DC-to-RF efficiency in a 65nm CMOS. In Proceedings of the 2016 IEEE MTT-S International Microwave Symposium (IMS), San Francisco, CA, USA, 22–27 May 2016; pp. 1–3.
- 26. Lee, T.H. *The Design of CMOS Radio-Frequency Integrated Circuits*, 2nd ed.; Cambridge University Press: New York, NY, USA, 2003; Volume 200, p. 311.
- 27. Kananizadeh, R.; Momeni, O. A 190-GHz VCO with 20.7% Tuning Range Employing an Active Mode Switching Block in a 130 nm SiGe BiCMOS. *IEEE J. Solid-State Circuits* 2017, *52*, 2094–2104. [CrossRef]
- 28. Koo, H.; Kim, C.; Hong, S. Design and analysis of 239 GHz CMOS Push-Push transformer-based VCO with high efficiency and wide tuning range. *IEEE Trans. Circuits Syst. I* **2015**, *62*, 1883–1893. [CrossRef]
- Khamaisi, B.; Socher, E. A 159–169GHz Frequency source with 1.26 mW peak output power in 65 nm CMOS. In Proceedings of the European Microwave Integrated Circuits Conference, Nuremberg, Germany, 6–10 October 2013; pp. 536–539.



© 2019 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (http://creativecommons.org/licenses/by/4.0/).