



Preparation of Cross-Linkable Waterborne Polyurethane-Acrylate Coating Films with Multifunctional Properties

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Abstract: Self-migration or unstable phase inversion occurs when the application conditions are varied, which limits the application of polyurethane-acrylate (PUA) composite films. In this paper, cross-linked polyurethane/poly(methyl methacrylate-co-borneol acrylate) shell microspheres were prepared by using the seeded emulsion polymerization method. The core-shell structure of these samples was identified by dynamic light scattering (DLS) and high-resolution transmission electron microscope (HR-TEM). Moreover, HR-TEM images indicated that the core-shell structure of the microsphere does not undergo complete phase inversion. In addition, with increasing content of borneol acrylate in the shell, the water resistance and antibacterial adhesion of films were improved. The X-ray photoelectron spectroscopy (XPS), Energy Dispersive Spectrometer (EDS), water contact angle (CA) measurements, antibacterial and anti-adhesion tests demonstrate that the C/N ratios of films from the inside to the upper surface had an obvious gradient in growth, indicating the shell component (polyborneol acrylate) was predominantly present at the surface of films after coalescence in cross-linked core-shell PUA. It was found that a suitable degree of cross-linking contributes to the segregation of the hydrophobic component (borneol groups) on the film surface. As a consequence, the excellent water resistance, cytocompatibility, and antibacterial properties endowed this series of polymer materials with promising application potential in the biomedical field.

Keywords: cross-linked; core-shell structure; antibacterial-adhesion coating; water resistance; cytocompatibility

1. Introduction

Bacterial infections are one of the most important risks for human health, which leads to significant mortality and morbidity worldwide [1,2]. The adherence of bacteria and subsequent formation of biofilms causes foreign bodies to become infected [3]. Thus, antibacterial coatings have become a



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focus of research during recent years. However, the antibacterial surface has both advantages and disadvantages. For instance, although the antibacterial surface can kill or prevent the initial adhesion of bacteria, this kind of surface is poor in biocompatibility, short-term antibacterial activity and easy degradation [4,5]. Furthermore, the use of antibacterial agents in the coating, such as antibiotics, is further limited due to the significant rise in antibiotic resistance [6].

The antibacterial-adhesion coating represents an attractive alternative to traditional antibacterial coatings, since it displays biocompatibility in various models and has broad-spectrum activity [7]. There are three main stages of development of bacterial adhesion: initial adhesion, multiplication to form colonies, and the formation of a biofilm. In stage of initial adhesion, the adhesive forces operating on bacteria are the Van der Waals force, electrostatic force, and hydrophilic and hydrophobic action. These forces are weak and the adhesion of bacteria to the surface is reversible, nonspecific and easily broken. After the adhesion of bacteria to the surface, the bacterial adhesion changes from reversible to irreversible and then the biofilm forms [8,9]. In response to this phenomenon, a large variety of surface types have been successfully developed to reduce the adhesion of bacteria during the initial adhesion phase, and these can consequently reduce the formation of biofilm. Hedrick et al. [10] prepared a series of polymers that were modified to introduce antimicrobial properties by improving hydrophobicity. Cui and Fan et al. [11] reported superhydrophobic coatings based on biodegradable polymers and modified silica microspheres, which could be conveniently fabricated through a co-electrospraying technique. The superhydrophobic film reduces the chance for cells or bacteria to firmly attach to the substrate because of the air trapped between the film and water [1,12–15].

Polymer surface stereochemistry is a practical and effective strategy to dramatically reduce bacterial attachment and biofilm formation due to interactions based on chiral stereochemistry [16]. Mitchell et al. [17] reported stereochemical-based knowledge could be used to improve the design of new antibacterial adhesion prophylactics. Inspired by the natural product, some researchers devoted attention to utilizing borneol to design a novel antibacterial adhesion polymer surface [18,19]. In addition, it is observed that borneol-based polymer is biocompatible and environmentally friendly, but the expensive price of monomers limits its effective application [16,20,21]. In general, core-shell microspheres composed of hydrophobic borneol components and hydrophilic components can solve this problem [22,23]. Because the microspheres with core-shell structure collapse to form films, the hydrophobic shell is enriched on the film surface due to surface tension. However, the moist environment and the chemical composition of core-shell microspheres can lead to the instability of self-migration or phase inversion [24–26].

With the above considerations in mind, the present work has been undertaken to synthesize hydrophobic borneol monomers which are then incorporated onto the shell layer of microspheres composed of methyl methacrylate (MMA) by means of a two-step polymerization technique. Cross-linked polyurethane (PU) core is selected because its cross-linking structure will limit the phase inversion of the core-shell structure and facilitate the migration of hydrophobic components to the film surface. In addition, it has good film-forming property and will not cause the cracking of membrane because of cross-linking. Therefore, this type of novel core-shell borneol-based PUA is of great potential to realize a convenient and effective strategy to prepare antibacterial adhesion films for antibacterial applications.

2. Materials and methods

2.1. Materials

Endo-L-Borneol, tetrahydrofuran (THF), triethylamine (TEA), acryloyl chloride, MMA, potassium peroxydisulfate and diethylenetriamine from Aladdin Chemistry Co., Ltd. (Shanghai, China) were used as received. Poly(propylene glycol) (PPG, Mw = 2000), isofordone diisocyanate (IPDI), 2,2-bis(hydroxymethyl)butyric acid (DMPA) and hydroxyethyl methacrylate (HEMA) from Sigma–Aldrich (St. Louis, MO, USA) were used as received.

2.2. Synthesis of Borneol Acrylate (BA) Monomer

Endo-L-Borneol (1.00 g) and TEA (0.98 g) were dissolved in 20 mL of THF. Acryloyl chloride (0.88 g) was added drop-wise and then the reaction mixture was stirred at 30 °C for 10 h. The reaction mixture was filtered and evaporated to obtain the crude product which was brown oil. The conversion rate of the product reached 63%. The ¹H NMR spectra of the BA and its detailed assignment of proton peaks is shown in Figure S1 (in the supporting information). ¹H NMR (600 MHz, CDCl₃) 6.42 (t, *J* = 24 Hz, 1H), 6.18–6.09 (m, 1H), 5.85 (dd, *J* = 24, 18 Hz, 1H), 5.03 (d, *J* = 24 Hz, 1H), 2.40–2.37 (m, 1H), 1.98–1.69 (m, 6H), 1.35–1.23 (m, 3H), 0.97 (d, *J* = 4.8 Hz, 3H), 0.87 (t, d, *J* = 4.8 Hz, 3H) [20].

2.3. Synthesis of PU Core Latex Particles

The synthetic procedures for making PU core latex particles were based on a previous report [27–29]. Briefly, PPG-2000 (80 g) and IPDI (28 g) were mixed in a three-necked round-bottom flask equipped with a thermometer, a mechanical stirrer and a refluxing condenser. After stirring for 5 min at room temperature, the system was heated to 110 °C. After 2 h, DMPA (5.5 g) was added into the system and reacted for 4 h. Then the system was cooled to 60 °C. 1 g HEMA and 30 g acetone were added and the temperature was maintained for 4 h. After the system was cooled to 50 °C, 3.8 g TEA was added with stirring for 10 min. Subsequently, 255 g deionized water was added and the reaction mixture was emulsified with vigorous stirring (1500 rpm). The emulsification was allowed to proceed for 5 min, then the mixture of 5.7 g and 50 g deionized water was added drop-wise with moderating stirring. The cross-linking reaction was allowed to proceed for 1 h. The conversion rate of each step of the reaction can be calculated by detecting the content of the unreacted NCO group through using dibutylamine back titration method because each step in previous three steps of the reaction involved NCO group. After testing, it was found that the conversion rate was 27.7% in the first step, 58.1% in the second step and 63.9% in the third step in Figure 1. In the fourth step, the degree of cross-linking was characterized with gel rate and the gel rate was 71.8%.

2.4. Preparation of the Core-shell Latex Particles

To a 100 mL three-necked flask, 12 g PU core seed latex, prescribed amount of Endo-L-borneol acrylate, 2.5 g methyl methacrylate and 15 g water were added. The system was stirred at 300 r/min and nitrogen was bubbled through it for 2 h. The polymerization was initiated by immersing the flask into the oil bath with the thermostat set at 80 °C. Meanwhile, the initiator (0.05 g KPS) dissolved in 10 mL water was slowly added drop-wise into the reactor. Lastly, the system was reacted for 8 h. The conversion rate was 91.8% which was tested by weighing method.

2.5. Film Preparation

A polytetrafluoroethylene (PTFE) mold (15 cm \times 15 cm \times 0.5 cm) was cleaned in an ultrasonic cleaning bath with acetone at 50 °C for 1 h and rinsed with deionized water three times. Then the latexes were directly cast in the pre-cleaned PTFE mold. The resultant films were allowed to dry at room temperature for 24 h and were then thermally treated in an oven at 120 °C for 48 h.

2.6. Characterization

Dynamic light scattering (DLS) measurements of latexes were performed on a Malvern Zetasizer Nano-ZS90 instrument (Malvern, UK) at room temperature. The average particle size was calculated via the Stoke–Einstein equation.

HR-TEM were measured on a JEM-2000EX instrument. The latexes were diluted in deionized water to a ratio of 1 to 300 and stained with 6% phosphotungstic acid solution. Then the diluted suspension was coated on a copper grid for measurements.

Attenuated total reflection Fourier transform infrared (ATR-FTIR) spectra of the microspheres were performed on an EQUINOX55 FTIR spectrometer (Bruker, Rheinstetten, Germany) equipped

with an ATR accessory, using an infrared beam fixed at an incident angle of 45°. The neat ATR element and wafer were measured as background spectra.

XPS analyses of the surfaces of latex films were performed on a Perkin Elmer ESCA 5600 spectrometer (Perkin Elmer, Shelton, CT, USA) with Mg K α X-ray source (1253.6 eV). Spectra were acquired at a take-off angle of 0°. The survey spectra from 0 to 1000 eV were acquired.

The gel contents (G) of the samples were measured to confirm the occurrence of cross-linking reaction. At first, the dried samples were weighed (W_i). Then the samples were soaked and stirred in acetone for 36 h at room temperature. The samples were isolated and reweighed after drying at 80 °C for 2 h (W_f), the percentage of gel contents were calculated according to Equation (1) [23,24]:

$$G = \frac{W_f}{W_i} \times 100\%$$
 (1)

CA of water was tested by a contact angle goniometer (Dataphysics, Germany) at room temperature. For each sample, two films were used for contact angle measurements; 4 μ L droplets were tested on three different places 100 s after depositing on the surface. The obtained values were averaged. Regarding deposition time of contact angle measurements, it was observed in preliminary experiments that most changes in drop roundness and contact angle values occurred during the initial 60 s. On the other hand, longer deposition times are inconvenient, which may lead to significant evaporation and induce irregular drop shapes. Therefore, the deposition time was set at 100 s [30]. The experimental errors of the contact angles are within ±2°.

Strains of the bacterium *Escherichia coli* (*E. coli*) were picked into a 50 mL sterile liquid medium, followed by overnight culturing at 37 °C with a shaking rate of 200 rpm. Finally, the *E. coli* solutions were diluted to a concentration of 10^7 CFU mL⁻¹ (colony-forming units) with sterile phosphate-buffered saline (PBS) solution.

A "prison break" experiment [16,21] was conducted to investigate interactions between bacteria and samples. The circular samples were fixed onto solid agar medium and sterilized under ultraviolet light. Then a small circular sterile agar block was fixed onto each sample, forming a special sandwich structure. After that, 5 μ L of *E. coli* suspension (10⁷ CFU mL⁻¹) was added on each of the small circular agar block and cultured at 37 °C. The results were recorded after 24 h by a camera.

The plate count method [31,32] was employed to investigate the anti-adhesion capability of samples. Firstly, each sample was cultured in 10 mL of *E. coli* suspension (10^7 CFU mL⁻¹) for 24 h. Second, to remove the non-adherent bacteria, each sample was gently rinsed with sterile water more than three times. Then each sample was placed into a 5 mL solution of sterile PBS, followed by ultrasonication in an ultrasonic bath to remove the bacteria from the surface of sample. In the end, 100 µL suspensions were coated on solid agar medium and then cultured for 24 h at 37 °C. The number of *E. coli* colonies was counted and each experiment was repeated at least three times.

Cytotoxicity of the film was examined by the in-vitro cytotoxicity-indirect cytotoxicity test. L929 mouse fibroblasts (ATCC NCTC clone 929:CCL 1) were cultivated with 10% Fetal Bovine Serum in Dulbecco's modified Eagle's medium. Incubation conditions were 5% CO₂ and higher than 90% relative humidity atmosphere at 37 °C. The films were immersed in the medium and incubated for 72 h. Then the films were interacted with L929 cells at 1×10^5 cells/mL densities in 96 well plates overnight. After 24 h, the mediums were changed with 10% 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) reagent and incubated at 37 °C for 4 h. The culture medium was removed and 100 µL propan-2-ol solution (with 0.04 M HCl) was added followed by incubation. The cell viability was tested using the MTT reduction assay and the absorbance was tested at 570 nm using a micro plate reader.

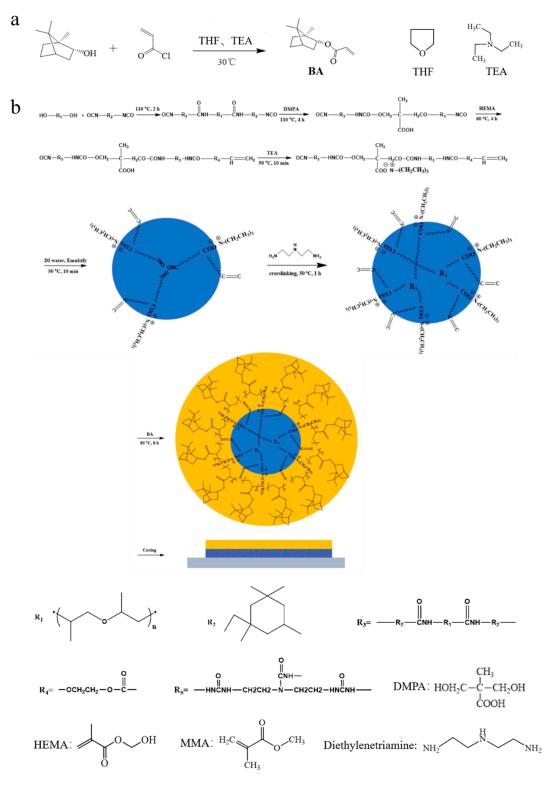


Figure 1. Schematic diagram of the fabrication process for (**a**) BA monomer and (**b**) Endo-L-Borneol based PUA film.

3. Results and Discussion

As illustrated in Figure 1, the cross-linked PU core containing vinyl groups-based PPG, IPDI and cross-linked diethylenetriamine was synthesized first. Subsequently, the mixture of Endo-L-Borneol acrylate and MMA was further copolymerized at the surface of PU core to produce the cross-linked core-shell PUA microsphere. Lastly, the latexes were directly cast in the pre-cleaned PTFE molds to

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produce Endo-L-Borneol PUA based films. In order to study the effect of core-shell structure of latex microspheres and content of Endo-L-Borneol acrylate on the property of latex films, the percentage of Endo-L-Borneol acrylate monomers in the copolymers was adjusted in the range from 0 wt.% to 54 wt.%.

The size distributions of PU particles and core-shell particles obtained were measured using the DLS method. The DLS curves for core and core-shell particles prepared with 0 wt.%, 23 wt.%, 37 wt.% and 54 wt.% Endo-L-Borneol acrylate, respectively, are presented in Figure 2. As can be seen, relative to the core particles, the curves of particles obtained in the second stage obviously shift towards the right. The DLS measurements indicate that a new layer has formed and coated the core surface to form a core-shell structure. The z-average diameter of PU core is 52.3 nm, while the z-average diameters of the core-shell particles are 75.6 nm, 83.2 nm and 108.9 nm, respectively. In addition, the core-shell structures of the Endo-L-Borneol acrylate based PUA microspheres were further confirmed by HR-TEM (Figure 3) and FTIR spectra (Figure 4). It is seen that the particles are spherical and uniform. The latex particles exhibit quite clear core-shell interfaces. The black core layer is the PU layer because the electron cloud is denser and the brighter shell layer is the acrylate layer containing borneol group [27,33]. Due to the effect of surface tension, the hydrophilic PU components often turn into the shell when the microspheres of PU core/polyacrylate shell are in the aqueous phase. It indicates that the cross-linked structures cause the core-shell microspheres not to undergo a phase inversion process. The gel contents of the samples were measured by swelling experiments in acetone to confirm the occurrence of cross-linking reaction. By calculation, the gel content of the cross-linked PU core is 71.8%. This demonstrates that the formation of cross-linked polymer networks in PU core, which supports the occurrence of cross-linking reaction. After being coated with polyacrylate shell, the FTIR spectra of PUA particles show apparent increase of C=O stretching vibration at 1725 cm⁻¹ and decrease of C–N stretching and N–H bending at 1526 cm⁻¹, compared to that of the PU core. These results verify the presence of polyacrylate on the PU core.

The Endo-L-Borneol acrylate based PUA emulsion was directly cast into a PTFE mold to prepare latex films whose weight ratios of Endo-L-Borneol acrylate to total weight were 0 wt.%, 23 wt.%, 37 wt.% and 54 wt.%. Then the films were removed from PTFE mold. The chemical compositions of upper and inside surface of films were studied by EDS.

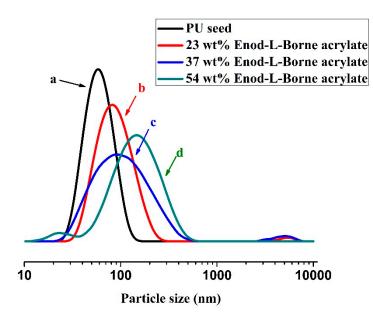


Figure 2. Size distribution curves of the core and core-shell latex particles: (**a**) PU seed; (**b**) 23 wt.% Endo-L-Borneol acrylate; (**c**) 37 wt.% Endo-L-Borneol acrylate; (**d**) 54 wt.% Endo-L-Borneol acrylate.

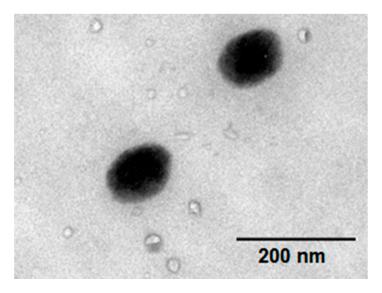
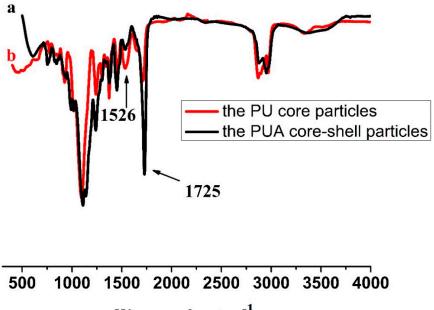


Figure 3. HR-TEM images of core-shell-structured latex particles.



Wavenumber (cm⁻¹)

Taking the film (37 wt.% Endo-L-Borneol acrylate) as an example, the EDS spectra of the upper and inside surface of film display the signals of C, O and N, as shown in Figure 5. Compared to the upper surface of film, the inside surface of film has a larger amount of O and N. The same results can be observed in mapping images. In addition, the mapping images show that the elements of O and N homogeneously distribute in the films. The reason may be that PUA core-shell latex particles tend to enrich on the shell layer when the films form. In this study, PUA shell contains a hydrophobic Endo-L-Borneol group, and the core contains a hydrophilic carboxyl group and these two polymer chain segments have different surface tensions. Therefore, when the microsphere collapses, the chain segments with different surface tensions have higher migration ability, resulting in more obvious phase separation of the film.

Figure 4. FTIR spectra of (a) the PUA core-shell particles and (b) the PU core particles.

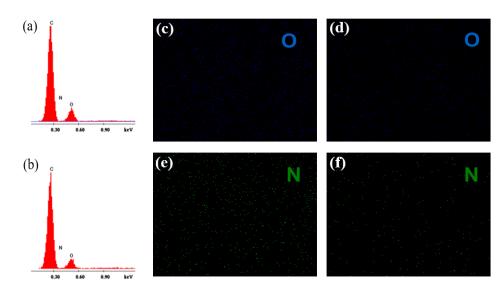


Figure 5. The EDS spectra and mapping images of the PUA latex films (37 wt.% Endo-L-Borneol acrylate). (**a**) The EDS spectrum of the inside surface of film. (**b**) The EDS spectrum of the upper surface. (**c**) The mapping image of the element O in the inside surface. (**d**) The mapping image of the element O of upper surface. (**e**) The mapping image of element N in the inside surface. (**f**) The mapping image of element N of the upper surface.

Due to the phase separation of the film, the hydrophobicity of upper surface differs that of inside surface. Thus, contact angle (CA) measurements were applied to check the surface wettability of upper and inside surfaces of three different films, and the larger static CA values indicate better hydrophobicity [34]. As shown in Figure 6, the static water CA values of upper and inside surfaces of three films (23 wt.%, 37 wt.% and 54 wt.% Endo-L-Borneol acrylate) range from 62.8° to 90.3°. Taking the film (23 wt.% Endo-L-Borneol acrylate) as an example, the upper surface has a static water CA value of 75.0°, while the inside surface displays a lower static water CA value of 62.8°. The same results can also be observed in other two films. This phenomenon can be attributed to the phase separation of the film which can be illustrated by the surface tension. And CA measurements can be used to calculate the solid surface tension (γ_{sv}) using the equation of state approach [23,25]:

$$1 + \cos \theta = 2 \sqrt{\frac{\gamma_{SV}}{\gamma_{IV}}} e^{-\beta (\gamma_{IV} - \gamma_{sv})^2}$$
(2)

where β is an empirical parameter and is found to be 0.0001247 (mN/m)⁻², while γ_{sv} and γ_{lv} denote the interfacial tensions of solid–air and liquid–air interfaces, respectively. θ is the contact angle of liquid. From the static water contact angles of the upper and inside surface of film (23 wt.% Endo-L-Borneol acrylate), the calculated surface tension of upper surface according to Equation (1) is 38.61 mN/m, while the surface tension of inside surface is 39.99 mN/m which is slightly higher than that of the upper surface. The same phenomenon can also be observed in the other two films. These results prove that the phase separation has taken place in the films.

This conclusion was further demonstrated by XPS spectra in Figure 7. It is observed that the peaks at 284, 532 and 401 eV correspond to C 1s, O 1s and N 1s. The experimental values of elemental concentration percentages of C, N and O elements in the upper surface of 37 wt.% Endo-L-Borneol acrylate is 78.63%, 1.18% and 20.19% and that of the inside surface is 68.19%, 2.71% and 29.10%. The elemental concentration percentages of C, N and O elements on upper surface of 54 wt.% Endo-L-Borneol acrylate is 82.82%, 1.06% and 16.13% and that on inside surface is 73.48%, 2.14% and 24.38%. These data indicate that the contents of O and N of the inside surface of film (37 wt.% Endo-L-Borneol acrylate) are higher than those of the upper surface as indicating phase separation

of film. The XPS survey spectra and high resolution C1s spectra for the upper and inside surface of film are shown in Figure 7. The signals of C–O locate at binding energy of 286.3 eV and the peak at 289.1 eV shows the presence of COO+ NH–C(=O)–O. The signal at 284.7 eV is corresponded to the other aliphatic and cycloaliphatic carbons [35,36].

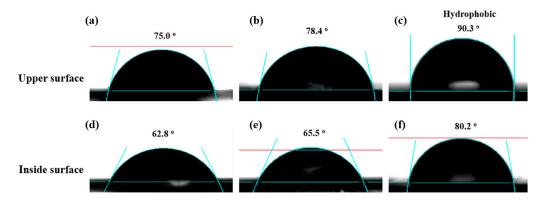


Figure 6. The static water CA measurements on upper and inside surfaces of three films: (**a**) upper surfaces of 23 wt.% Endo-L-Borneol acrylate; (**b**) upper surfaces of 37 wt.% Endo-L-Borneol acrylate; (**c**) upper surfaces of 54 wt.% Endo-L-Borneol acrylate; (**d**) inside surfaces of 23 wt.% Endo-L-Borneol acrylate; (**e**) inside surfaces of 37 wt.% Endo-L-Borneol acrylate; (**f**) inside surfaces of 54 wt.% Endo-L-Borneol acrylate.

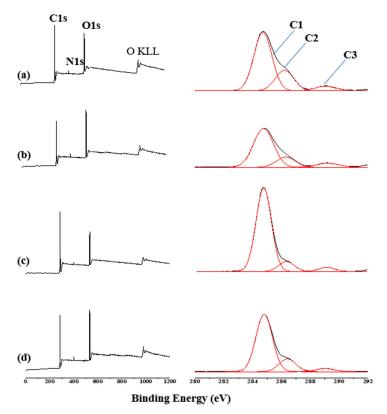


Figure 7. XPS spectra images of the PUA latex films and fine spectra fitting, C3 (COO+ NH–C(=O)–O), C2(C–O) and C1 (aliphatic and cycloaliphatic carbons). (a) upper surface of the film (37 wt.% Endo-L-Borneol acrylate) with C1/C3 atomic ratio of 11.2; (b) inside surface of the film (37 wt.% Endo-L-Borneol acrylate) with C1/C3 atomic ratio of 8.3, (c) upper surface of the film (54 wt.% Endo-L-Borneol acrylate) with C1/C3 atomic ratio of 18.2, (d) inside surface of the film (54 wt.% Endo-L-Borneol acrylate) with C1/C3 atomic ratio of 16.5.

C3 is the COO+ NH–C(=O)–O, C2 is C–O and C1 is aliphatic and cycloaliphatic carbons, as is shown in Figure 7. The C1/C3 atomic ratios as functions of the upper and inside surfaces of films which have different contents of Endo-L-Borneol acrylate (37 wt.% and 54 wt.%) is 11.2, 8.3, 18.2 and 16.5. The relative proportion of groups was computed from the areas under these curves in C1s. The ratio of C1/C3 atoms on the upper surface of film is higher than that on the inside surface. The COO and NH-C(=O)–O)/C–O groups belong to the PU core, and the C=O belongs to the PU core and polyacrylate shell. Because the ratio of C=O group and (COO + NH–C(=O)–O)/C–O) group is fixed on PU core layer, the results in Figure 7 show that more polyacrylate components are enriched on the upper surface, while more PU components are enriched on the inside surface of film. These results are consistent with EDS analysis. In addition, with higher content of Endo-L-Borneol acrylate, this ratio is higher.

To evaluate the effect of anti-adhesion properties, a method called the "prison break" experiment was employed to demonstrate the capacity of films and inhibit the diffusion of Gram-negative *E. coli* (Figure 8). After 24 h, *E. coli* successfully broke the restrictions of film in the control group to diffuse outside obviously. And neither the upper nor inside surface of film (23 wt.% Endo-L-Borneol acrylate) can completely restrict the outward spread of *E. coli*. The upper surface of film (37 wt.% Endo-L-Borneol acrylate) exhibits excellent restriction for the spreading out of *E. coli*, while the inside surface cannot efficiently inhibit the outward spread of *E. coli*. Meanwhile, both the upper and inside surface of film (54 wt.% Endo-L-Borneol acrylate) display excellent anti-adhesion performance to inhibit the diffusion of *E. coli*, which cannot break the 'film prison'.

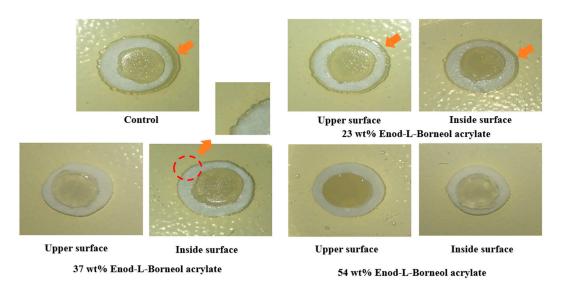


Figure 8. Photographs of modified 'prison break' experiments for antibacterial adhesion assays of the films.

Anti-adhesion capacities of all films were also investigated by classical methods. Figure 9 illustrates the plate count results of the films. The colony numbers of *E. coli* on the upper and inside surfaces of films (23 wt.%, 37 wt.% and 54 wt.% Endo-L-Borneol acrylate) are 1.3×10^6 , 7.5×10^6 , 8.6×10^5 , 1.6×10^6 , 0 and 0 units, respectively. Taking the film (23 wt.% Endo-L-Borneol acrylate) as an example, the number of bacteria adhering to the upper surface was reduced by 82.6%. It also suggests that the upper surface has better anti-adhesion performance compared with the inside surface. The phenomenon indicates that increasing content of Endo-L-Borneol acrylate leads to a gradually higher anti-adhesion effect. The upper surface has better anti-adhesion ability than the inside surface, which further confirms the existence of phase separation in films. Endo-L-Borneol acrylate migrates onto the upper surface, while PU is firmly fastened on the inside surface on account of the cross-linked structure. Because the content of Endo-L-Borneol acrylate in film (54 wt.% Endo-L-Borneol acrylate) is high and the inside surface also has Endo-L-Borneol acrylate, the inside surface has a good anti-adhesion capacity.

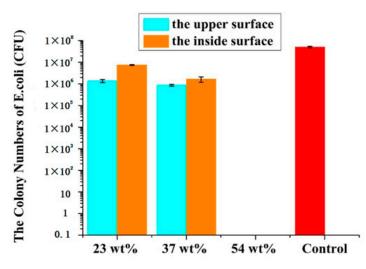


Figure 9. Anti-adhesion experiment: E. coli. colony numbers corresponding to E. coli on the films.

In order to demonstrate the cell toxicity of films, a tetrazolium-dye-based assay was employed. The results are displayed in Figure 10. PU was set as control group and the cell viability of PU reached nearly 100%. The cell viability of the inside surfaces of the three films (23 wt.%, 37 wt.% and 54 wt.% Endo-L-Borneol acrylate) were above 95%, indicating excellent cytocompatibility. The cell viability of the upper surfaces of three films (23 wt.%, 37 wt.% and 54 wt.% Endo-L-Borneol acrylate) were 96%, 94% and 92%, respectively. With increasing amounts of Endo-L-Borneol acrylate, the cell viability of the inside surface decreases slightly and that of the upper surface decreases more obviously than the inside surface. Therefore, this material has a promising potential for applications in the biomedical field due to its cytocompatibility.

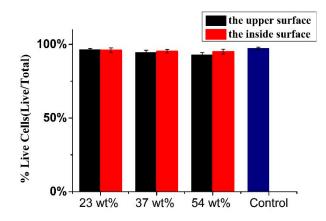


Figure 10. The in-vitro cytotoxicity tests of films.

4. Conclusions

In conclusion, high-quality cross-linked polyurethane/polymethyl methacrylate-borneol acrylate with adjustable shell thickness was prepared with PU seed particles as a core by controllable coating technology. The structures of these samples were characterized by DLS and HR-TEM. The results demonstrate that the samples have core-shell structures which are not completely reversed. With increasing content of borneol acrylate in shell, the hydrophobicity and antibacterial adhesion of films are improved. In addition, the ratio of C/N increases in a gradient from the inside surface to the upper surface of film with increasing content of Endo-L-Borneol acrylate. The results show that proper cross-linking is beneficial to the separation of hydrophobic borneol from the surface of film, which makes the film have excellent antibacterial adhesion. Furthermore, the film has good cellular compatibility, which endows it with a excellent prospects for future applications in the biomedical field.

Supplementary Materials: The following are available online at http://www.mdpi.com/2079-6412/10/1/65/s1, Figure S1: The ¹H NMR spectra of the BA.

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