



Article Magneto-Tactile Sensor Based on a Commercial Polyurethane Sponge

Ioan Bica¹, Gabriela-Eugenia Iacobescu^{2,*} and Larisa-Marina-Elisabeth Chirigiu³

- ¹ Advanced Environmental Research Institute, West University of Timisoara, Bulevardul Vasile Pârvan 4, Nr. 4, 300223 Timisoara, Romania
- ² Department of Physics, University of Craiova, Strada Alexandru Ioan Cuza, Nr. 13, 200585 Craiova, Romania
- ³ Department of Pharmacy, "Constantin Brâncuşi" University of Târgu-Jiu, Strada Tineretului, Nr. 4, 210185 Târgu-Jiu, Romania
- * Correspondence: gabriela.iacobescu@edu.ucv.ro

Abstract: In this paper, we present the procedure for fabricating a new magneto-tactile sensor (MTS) based on a low-cost commercial polyurethane sponge, including the experimental test configuration, the experimental process, and a description of the mechanisms that lead to obtaining the MTS and its characteristics. It is shown that by using a polyurethane sponge, microparticles of carbonyl iron, ethanol, and copper foil with electroconductive adhesive, we can obtain a high-performance and low-cost MTS. With the experimental assembly described in this paper, the variation in time of the electrical capacity of the MTS was measured in the presence of a deforming force field, a magnetic field, and a magnetic field superimposed over a deformation field. It is shown that, by using an external magnetic field, the sensitivity of the MTS can be increased. Using the magnetic dipole model and linear elasticity approximation, the qualitative mechanisms leading to the reported results are described in detail.

Keywords: sensor; polyurethane sponge; carbonyl iron; electrical capacity; magnetic field

1. Introduction

In recent years [1–5], portable and flexible tactile sensors have attracted the attention of the academic community due to their applications, which include measuring physiological parameters in medicine [6–8], the robotics industry [9], human-computer interactions [10–12], and the creation of portable devices [13–16]. In general, tactile sensors mimic the human perception of pressure and have the ability to detect the shapes and slipping conditions of objects they come in contact with. As compared with silicon-based devices, flexible materials are more suitable for tactile applications due to their good adhesion, average tensile values, and flexibility [17-21]. Flexible materials such as polyethylene [22], polydimethylsiloxane [23,24], polyurethane [25], and polyimide [26] have been used for manufacturing tactile sensors. Depending on the response function of the sensors, piezoresistive touch sensors [27-29], capacitive touch sensors [30], piezoelectric touch sensors [31,32], and optical touch sensors [33] have been developed. To obtain these sensors, metal particles [10], carbon nanotubes (CNT) [34,35], carbon black [36], graphene [37–39], or nanowires [22,40] have been introduced into the polymer used in the sensor. In a recent paper [41], a magnetoresistive sensor was fabricated with permanent magnets in the form of Fe-Ga wires and Hall sensors to detect static and dynamic force fields and the degree of rigidity of an object touched. It was a piezoresistive sensor with a sensitivity of 166 mV/m, which was able to detect forces with values up to 3 N and had applications in making prostheses or robots with a precise grip and an intelligent control of objects touched. The development of electrical devices whose

Citation: Bica, I.; Iacobescu, G.-E.; Chirigiu, L.-M.-E. Magneto-Tactile Sensor Based on a Commercial Polyurethane Sponge. *Nanomaterials* **2022**, *12*, 3231. https://doi.org/ 10.3390/nano12183231

Academic Editors: Pilar Marín and Daniel Matatagui

Received: 22 July 2022 Accepted: 13 September 2022 Published: 18 September 2022

Publisher's Note: MDPI stays neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Copyright: © 2022 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (https://creativecommons.org/license s/by/4.0/). response functions are sensitized by the use of an external magnetic field was reported in [42–45]. In [42,43], the fabrication of mechanical deformation sensors using cotton fiber fabrics with iron carbonyl microparticles and barium titanate nanoparticles was reported. It was shown that the electrical response (resistive, capacitive, and piezoelectric) of electrical devices was stable in time and adjustable in a magnetic field for certain values of hydrostatic pressure. In [44], the magnetic and dielectric effects induced by the magnetic field in a new composite fabric made of cotton fibers and carbonyl iron (CI) microparticles was reported. In [45], the authors reported on the fabrication of a magnetic composite (MS) consisting of a cylindrical polyurethane sponge in which CI microparticles were electrostatically assembled. By applying a static magnetic field, with gradients of up to 1800 kA/m^2 , superimposed on a medium frequency electric field (f = 1 kHz), a relevant magnetodielectric response was reported. However, the response to repetitive mechanical stress could not be obtained in MS. The manufacturing of magnetotactile sensors, using the process from [45], is difficult. For this reason, in this paper, we use a commercial low-cost polyurethane sponge with dimensions of $20 \times 25 \times 5 \text{ mm}^3$ and a biphasic liquid solution consisting of ethyl alcohol (99%) and CI microparticles to obtain a magnetizable polyurethane sponge (MPS). To fabricate an electrical device, the magneto-tactile sensor (MTS), MPS, and copper foil electrodes are used. The copper foil, 0.50 mm thick and 20 mm wide, has electroconductive adhesive on one side. The adhesive ensures the mechanical-electrical contact between the copper foil and the MPS composite. The purpose of this study is to investigate the response of MTS to compressions exerted on its surface in the absence and presence of the magnetic field. With an RLC bridge, data are obtained regarding the electrical response of the MTS, as well as the response to mechanical and magnetic excitations. On the basis of the results, we conclude that the MTS has a good electrical response for low values of repetitive compressive forces. Moreover, the electrical response of the MTS, for the same mechanical deformations, increases when using a magnetic field.

2. Materials and Methods

2.1. Materials

The materials used for fabricating the MTS have the technical characteristics provided by the manufacturing companies. The morphology of the materials and the analysis of the chemical elements were performed by scanning electron microscopy (SEM) using an Inspect S PANalytical system (Malvern Panalytical, Malvern, UK) coupled with an energy dispersive X-ray analysis detector (EDX), as follows:

(a) Carbonyl iron microparticles (Sigma-Aldrich, St. Louis, MO, USA) have an average diameter of $d_m = 5\mu m$ and an iron content of at least 97%. The mass density of the CI microparticles is $\rho_{CI} = 7.86 \text{ g/cm}^3$. The particles visualized using SEM were spheres and were confirmed to have an average diameter of $5 \mu m$ (Figure 1a). They have a high degree of purity, as shown in Figure 1b.



Figure 1. (**a**) SEM morphology of CI microparticles; (**b**) EDX spectra for the elemental analysis of CI microparticles.

The magnetization slope of the CI microparticles is shown in Figure 2. It was plotted using the experimental set-up described in [46].



Figure 2. Magnetization slope for the CI microparticles.

Figure 2 shows a linear dependence of the relative magnetization of the CI microparticles with the intensity of the magnetic field. For magnetic field intensities of $H \ge 540 \text{ kA/m}$, the relative saturation magnetization of the CI microparticles is $\sigma_{SCI} = 195 \text{ Am}^2/\text{kg}$.

(b) Super absorbent cloth (AC), of the type "Scotch-Brite" (3M, Saint Paul, MN, USA) ($20 \times 18 \times 0.5$ cm), is made in Italy and contains (see officedirect.ro) 48% viscose, 12% polyester, 25% polyurethane foam, and 15% latex. A piece with the dimensions $20 \times 25 \times 5$ mm³ is cut from AC (Figure 3a). By exfoliating a face, the polyurethane sponge (PS) from Figure 3b is obtained, with the dimensions $20 \times 25 \times 4$ mm.



Figure 3. Photo images: (a) Super absorbent cloth (AC); (b) polyurethane sponge (PS).

The absorbent PS from Figure 3b consists of cells and microfibers, as revealed by the SEM analysis (Figure 4a). Fine and ultrafine particles can be stored in the PS cells. The PS microfibers (Figure 4b) contain carbon and oxygen atoms. The Al atoms are due to the support plate.



Figure 4. (a) SEM morphology of PS; (b) EDX spectra for the elemental analysis of PS.

- (c) Laboratory Reactive Ethyl Alcohol (EA) was purchased from MedAz.ro and has an alcohol content of 96.0%.
- (d) Copper foil with electroconductive adhesive (CS) (Huizhou Yunze Electronic Technology, Huizhou, China) has a length of 20 m, a width of 3 cm, and a thickness of 0.05 mm. It was acquired from Frugo (Hong Kong, China).

2.2. Procedure for Making the MPS and Designing the MTS

The procedure for making the MPS involved the following five stages:

Stage 1: The PS from Figure 3b, with a volume $V_{PS} = 2 \text{ cm}^3$, is weighed using an ALN60 type balance (produced by AXIS, Gdansk, Poland). The value obtained is $m_{PS} = 0.050 \text{ g}$.

Stage 2: The PS is soaked until saturated with distilled water. The mass of the sponge soaked in distilled water is $m_{PSw} = 0.204 \text{ g}$; the mass of water in the sponge is $m_w = m_{PSw} - m_{PS} = 0.154 \text{ g}$. The volume occupied by the water is $V_w = m_w / \rho_w = 0.154 \frac{g}{1} \text{ g}/\text{cm}^3 = 0.154 \text{ cm}^3$. We consider that water replaces the volume of air in the PS. Based on this hypothesis, we find that the volume of air in the PS is $V_a = 0.154 \text{ cm}^3$. Under normal conditions of temperature and pressure, the air density is $\rho_a = 1.29 \cdot 10^{-3} \text{ g/cm}^3$. Then, the mass of air in the volume of PS is $m_a = V_a \cdot \rho_a \cong 0.198 \cdot 10^{-3} \text{ g}$. The volume of polyurethane fibers in the PS is $V_f = V_{PS} - V_a = 1.846 \text{ cm}^3$.

Stage 3: Using the same balance, we weigh 3400 g (5 cm³) of EA and 3153 g (1 cm³) of CI microparticles. The weighed products are mixed in a Berzelius vessel for about 300 s at a temperature of 70 °C \pm 5 °C. The temperature, at the surface of the mixture, is measured using an infrared thermometer, Type AX-6520 from AXIOMET (Bielsko-Biała, Poland) (manufactured in Poland and distributed by Transfer Multisort Elektronic S.R.L., Timișoara, Romania) At the end of this stage, a biphasic liquid (BL) is obtained.

Stage 4: In BL, at a temperature of 70 °C \pm 5 °C, we insert the PS (from Figure 3b) and continue mixing. After about 200 s, the PS is extracted with absorbed BL and fixed in a vacuumed electric jar (Auto-Vacuum Food System type, made in Taiwan). In the vacuum volume, the excess BL is drained and the EA evaporated. After about 48 h, the MPS is obtained (Figure 5a,b).



Figure 5. MPS photos: (a) Front view; (b) side view.

Stage 5: Using the same balance, the mass of the MPS is obtained as $m_{MPS} = 0.122 \text{ g}$, and the mass of the microparticles in MPS is $m_{CI} = m_{MPS} - m_{PS} = 0.072 \text{ g}$; it occupied, in the body of MPS, a volume of $V_{CI} = m_{CI}/\rho_{CI} = 0.0092 \text{ cm}^3$. The volume of air in the MPS body is $V_{aMPS} = V_{PS} - (V_f + V_{CI}) = 0.1448 \text{cm}^3$. The air mass in the MTS is $m_{aMPS} = V_{aMPS} \cdot \rho_a \approx 0.001 \text{g}$.

The mass and volumetric fractions of the CI microparticles, the polyurethane microfibers, and the air in the MTS body are given in Table 1.

Table 1. Mass (Φ) and volumetric (φ) fractions for MS_i , where i = 1, 2, and 3 denote sample numbers.

$\Phi_{CI}(\% wt.)$	$\Phi_f(\% wt.)$	$\Phi_a(\% wt.)$	φ _{CI} (%vol.)	$\varphi_f(\% vol.)$	$\varphi_a(v\% vol.)$
59	40	1	0.46	92.3	7.24

For the calculation of the mass fractions, we refer to the mass m_{MPS} and to the mass deduced for the CI microparticles, polyurethane microfibers, and air. Instead, for the volume fractions, we refer to the volume of MPS, identical to that of PS, and to the volumes of CI microparticles of polyurethane microfibers, deduced above.

Photographs of the MTS were taken with a zoom-type manual digital microscope (ANDYLUC BESTMAG SRL, China). It is observed (Figure 6a) that the CI microparticles from the MTS are fixed on the polyurethane microfibers. In the presence of the magnetic field (Figure 6b), the CI microparticles are oriented along the magnetic field lines. Highlighting of the columns was performed by supplementing the number of CI microparticles deposited on the MTS.



Figure 6. The MPS viewed under a digital microscope: (a) In the absence of the magnetic field; (b) in the presence of the magnetic field ($H \approx 40 \text{ kA/m}$).

The MPS has, in its structure C, O, and Fe atoms (Figure 7a). The crystallographic structure of the MPS is shown in Figure 6b. The crystal phase of the MPS was investigated using a PANalytical diffractometer, with Cu-K α radiation (λ = 0.15406 mm) and 2 θ range from 10° to 90°. It is observed from Figure 7b that, in the MPS structure, there is a crystal-line phase specific to CI microparticles [47,48] and an amorphous phase characteristic of polyurethane nanofibers [49]. The peak in Figure 7b is characteristic of nanometric crystallites, of type α -Fe, for CI microparticles that are not chemically treated [50].



Figure 7. (a) EDX spectra for the elemental analysis of MPS; (b) XRD analysis of MPS.

It is known that the saturation magnetization of composites is dependent on the volume fraction of CI microparticles [51,52]. Based on this conclusion, the Equation $\mu_0 \sigma_{SMTS} = \varphi_{CI} \mu_0 \sigma_{SCI}$ can be obtained (where μ_0 is the vacuum permeability, σ_{SMTS} is the relative saturation magnetization of MPS, φ_{CI} is the volume fraction of the CI microparticles in MPS, and σ_{SCI} is the relative saturation magnetization of composition of the microparticles CI)



Figure 8. Magnetization slope for the MPS.

It can be seen from Figure 8 that the MPS magnetization slope has the same shape as that of the CI microparticles. However, due to the volume fraction of the CI microparticles, i.e., value $\varphi_{CI} = 0.46$ vol%, the saturation magnetization of the MTS sponge is 266 times lower compared with that of the CI microparticles from Figure 2.

The adhesive part of the CS is applied on the faces of the MPS by rolling. At the end of this step, the MTS device from Figure 9 is obtained.



Figure 9. (a) Front view photo of the MTS; (b) lateral view photo of the MTS (1, copper foil; 2, MTS; 3, electrical connection).

It can be seen from Figure 9 that the MTS device has a stable mechanical configuration and is provided with copper wires for electrical connections. The copper foil with a thickness of 0.05 mm is molded on the rough surface of the MTS sponge, which explains the unevenness, shown in Figure 9, on the faces of the MTS.

2.3. Experimental Set-Up and Measurements

The experimental set-up for the study of the MTS in a magnetic field superimposed with the action of the mechanical force field is shown in Figure 10.



Figure 10. Experimental set-up (overall configuration): (1) Magnetic yoke; (2) coil; (3) non-magnetic axis; (4) plate; (5) marked mass made of lead. BR, RLC bridge; DCS, direct current source; Gs, Gaussmeter; N and S, magnetic poles; MTS, magneto-tactile sensor; h, Hall probe; \vec{F} , compression force vector; \vec{H} , magnetic field strength vector.

The set-up includes a direct current electromagnet, consisting of a magnetic core (Figure 10, (1)) and a coil (Figure 10, (2)) connected to the direct current source (type RXN-3020D, from Electronics Co., Ltd., Nagoya, Japan). The MTS is fixed by the axis (Figure 10, (3)) between the magnetic poles N and S. By adjusting the intensity of the direct current discharged by the DCS source through the electromagnet coil, the H value of the intensity of the incident magnetic field is adjusted at the MTS and measured by the Hall probe (h) connected to the gaussmeter (Gs) (type DX-102, from DexingMagnet, Xiamen, China). The MTS sensor is inserted between two stratisticlotextolite plates, which, for simplicity, are not represented in Figure 10. The mechanical resistance of these plates favors the uniform application of the force F, exerted by the weight of the non-magnetic masses (5), on the MTS through the axis (3). The marked mass (m) exerts compression pressure (mechanical stress) (*p*) (Figure 11) on the MTS without affecting the Hall probe.



Figure 11. Compression force (F) and compression pressure (*p*) induced on the MTS by the marked masses (m).

The RLC bridge (BR) (model 8846A, Fluke, Everett, WA, USA) connected to the MTS is used to measure, in time and for determined durations, the electrical capacity depending on the force, F, in the absence and in the presence of the magnetic field.

3. Results and Discussion

The RLC bridge is set on the electrical capacity measurement range, C, at time intervals $\Delta t = 1$ s.

The C values of the electrical capacity of MTS as a function of time, t, over a period of 180 s, in the presence of the compression force, F, but in the absence of the magnetic field, are plotted in Figure 12a.



Figure 12. (a) The electrical capacity, C, of MTS, as a function of time, t, with the force F as a parameter; (b) the average capacity C_m of MTS as a function of F; (c) the components ε_{zz} of the deformations of MPS as a function of F (dots are experimental data and lines are the first-order polynomial fit).

It can be seen from Figure 12a that the electrical capacity values, C, are constant in time but vary with increasing F. It is observed that, for an increase in the force F to a value of F + Δ F, the quantities C increase to values of C + Δ C, where Δ C = 0.001 nF, for Δ F = 1 N. When repeating the measurements, after five cycles of five recorders, the deviations were within ±2%, identical to the measurement error of the RLC bridge. When applying forces F higher than 5 N, the electrical capacity, C, of the MTS remains constant in time. For m ≥ 650g, the values of C do not return to the initial values when the deformation is removed.

In order to explain the behavior of MTS subjected to external magnetic and deformation fields, in the Appendix, we propose a model of MTS for three different situations: A. MTS subjected to a field of compression forces; B. MTS subjected to a magnetic field; C. MTS subjected to a magnetic field superimposed on a field of compression forces. In Equation (4) from the Appendix, we introduce the quantities C_{m0} and C_m using the function $C_m = C_m(F)$ from Figure 12b, and we obtain $\varepsilon_{zz} = \varepsilon_{zz}(F)$, as shown in Figure 12c. Figure 12c shows that the deformation of MPS has a linear dependence on F, and the modulus of the deformation components increases with an increase in F.

Using the model described at point A from the Appendix, with $h_0 = 0.4$ mm, and with the data from Figure 12b,c, we obtain the elasticity constant value $k \approx 12.26$ kN/m and the Young's modulus E = 10kPa of MPS in the absence of the magnetic field.

Next, for the fixed quantities F and H, we measure, at intervals $\Delta t = 1$ s for a duration of 180 s, the C_H values of the electrical capacity of the same MTS. The obtained values are plotted in Figure 13.



Figure 13. The electrical capacity of MTS, C_H , as a function of time and intensity of the magnetic field applied on the direction of the deformation force: (a) F = 0 N; (b) F = 1 N; (c) F = 2 N; (d) F = 3 N.

It can be observed from Figure 13 that, on the one hand, the quantities C_H for fixed F and H values are constant in time. On the other hand, the C_H values for constant F quantities increase with the increasing H intensity of the magnetic field. To appreciate the

variation with time, t, of the electrical capacity, we calculate the average value of the functions $C_H = C(t)_{F,H}$ from Figure 13, and we obtain the functions $C_{Hm} = C_{Hm}(H)_F$, as shown in Figure 14a.



Figure 14. (a) The average electrical capacity, C_{Hm} , depending on the intensity of the magnetic field, H, for the force, F, as a parameter; (b) the components e_{zzH} depending on the intensity of the magnetic field, H, for the force, F, as a parameter (dots are experimental data and lines are the second-order polynomial fit).

It can be seen from Figure 14a that the functions $C_{Hm} = C_{Hm}(H)_F$ can be approximated by:

$$C_{Hm} = C_{Hm_0} + \alpha_C \cdot H - \beta_C \cdot H^2$$
⁽¹⁾

where C_{Hm_0} , α_C , and β_C have the values shown in Table 2.

Table 2. Values of C_{Hm_0} , α_C , and β_C for $F = 0 \div 3N$.

F(N)	$C_{Hm_0}(nF)/\nu$	$\alpha_{c}(nF \cdot m/kA)/\nu$	$eta_{C}(nF\cdot m^{2}/kA^{2})/ u$
0	$0.04367/5.86282 \cdot 10^{-4}$	$1.75845 \cdot 10^{-4} / 9.78162 \cdot 10^{-6}$	$2.20238 \cdot 10^{-7} / 3.359092 \cdot 10^{-8}$
1	0.04786/0.00271	$2.99281 \cdot 10^{-4} / 4,51904 \cdot 10^{-5}$	$4.54501 \cdot 10^{-7} / 1.55184 \cdot 10^{-7}$
2	0.05001/0.0036	$4.52734 \cdot 10^{-4} / 6.00749 \cdot 10^{-5}$	$6.12388 \cdot 10^{-7} / 2.06298 \cdot 10^{-7}$
3	0.05264/0.0048	$6.09759 \cdot 10^{-4} / 8.00487 \cdot 10^{-5}$	$6.72545 \cdot 10^{-7} / 2.74888 \cdot 10^{-7}$

Here, ν is the standard error.

Using the model of the dipolar magnetic approximation (Figure A2 of the Appendix) from Equation (A32), it is observed that the electric capacity of MTS, in the absence of F, increases significantly with the increase in the magnetic field, H, in agreement with the data obtained in Figure 14a for F = 0 N. On the other hand, when applying F and H, according to the model from paragraph B of the Appendix given by Equation (A36), the effects are cumulative, in accordance with the corresponding experimental data from Figure 14a.

The components e_{zzH} of the deformations of MPS located in the field of deforming forces superimposed over a magnetic field are defined by the Equation (A39):

$$e_{zzH} = \frac{h_m}{h_0} - 1 = \frac{C_{Hm_0}}{C_{Hm}} - 1$$
(2)

where h_m is the thickness of MPS in MTS, with the electrical capacity m, at values $H \neq 0$ and $F \neq 0$, and h_0 is the thickness of MPS in MTS, with the electrical capacity C_{Hm_0} , at values $H \neq 0$ and F = 0.

In Equation (2), we introduce the values of C_{Hm_0} and C_{Hm} corresponding to the functions $C_{Hm} = C_{Hm}(H)_F$, from Figure 14a, and we obtain the functions $e_{zzH} = e_{zzH}(H)_F$, represented in Figure 14b. It is observed from Figure 14b that, in the magnetic field superimposed over the field of mechanical forces, the allure of the functions $e_{zzH} = e_{zzH}(H)_F$ is that of a second-order polynomial function and not that of a linear polynomial function obtained in Figure 12c for MTS subjected only to the action of F. From the same figure, it is observed that the modulus of the quantities e_{zzH} increases with an increase in the quantity H, at values F = const. Likewise, for the same H, the modulus of the values of the deformation components increases with the increasing size of F.

The contribution α_F brought by the force F to an increase in the electrical capacity of MTS, in the absence of the magnetic field, can be obtained from the equation:

$$\alpha_F(\%) = \left(\frac{c_{\rm m}}{c_{\rm m0}} - 1\right) 100\tag{3}$$

where C_m and C_{m0} are the electric capacities of the MTS for $F \neq 0$ and F = 0, respectively.

If, in Equation (3), we introduce the function $C_m = C_m(F)$ from Figure 12b, we obtain $\alpha_m = \alpha_m(F)$, represented in Figure 15a.



Figure 15. (a) The variation of α_F as a function of the deformation force, F; (b) the contribution α_H as a function of the magnetic field intensity, H, for the deforming force, F, as a parameter.

It is observed from Figure 15a that α_F increases linearly with F values. For F = 5 N, we obtain α_F = 11.11%.

For the MTS located in the magnetic field, H, superimposed over the field of deforming forces, F, we denote by α_H the contribution brought by the magnetic field to an increase in the value of the electrical capacity of MTS, which can be expressed by the equation:

$$\alpha_H(\%) = \left(\frac{C_{Hm}}{C_{m_0}} - 1\right) 100$$
(4)

where C_{Hm} is the electrical capacity of MTS for $H \neq 0$ and $F \neq 0$, and C_{m_0} is the electrical capacity of MTS in the absence of both magnetic and deformation fields.

In Equation (4), we introduce the functions $C_{Hm} = C_{Hm}(H)_F$ from Figure 14a, and we obtain the function $\alpha_H = \alpha_H(H)_F$, as in Figure 15b.

$$\alpha_F = \begin{cases} 2.22\% \text{ for } F = 1N \\ 4.44\% \text{ for } F = 2N \\ 6.66\% \text{ for } F = 3N \end{cases}$$
(5)

When applying the magnetic field in the absence of deforming forces (Figure 15b), the contribution brought to an increase in the electrical capacity of MTS is 73.21% at H = 280 kA/(m). Then, when applying the deforming forces superimposed over the magnetic field of intensity H = 280 kA/m, the contribution brought by H to an increase in C_{Hm} is:

$$\alpha_{H} = \begin{cases} 100,64\% \text{ for F} = 1N\\ 157,46\% \text{ for F} = 2N\\ 224,15\% \text{ for F} = 3N \end{cases}$$
(6)

From the results (5) and (6), it is observed that, by applying the magnetic field, the sensitivity of MTS to the action of the deforming forces increases significantly.

Using Equations (A39)–(A42) from the Appendix in correlation with the magnitudes of electrical capacities from Figure 14a, we obtain the function $k_{\mu F} = k_{\mu F}(H)$, as shown in Figure 16a, and the function $E_{HF} = E_{HF}(H)$, as shown in Figure 16b, when MTS is subjected to a magnetic field superimposed on a field of compression forces.



Figure 16. (a) The variation of the elastic constant of MPS, $k_{\mu F}$, as a function of the magnetic field intensity, H; (b) the variation of Young's modulus, E_{HF} , as a function of the magnetic field intensity, H.

It can be seen from Figure 16a,b that the effects generated by the magnetic field, H, and the deformation forces, F, overlap. The dependence of the two elasticity constants on the magnetic field is due to magnetoconstriction. The effect is specific to materials containing magnetizable microparticles [42–45,51,54].

4. Conclusions

The magneto-tactile sensor (MTS) is fabricated by using a commercially used polyurethane sponge (Figure 3), ethanol, carbonyl iron microparticles, and copper foil with electroconductive self-adhesive (Figure 9). With the installation in Figure 10, the electrical capacity of the MTS is measured in time and for determined durations. The values of the electric capacity do not change in the time of measurements and increase linearly with an increase in the deforming forces (Figure 12) in the absence of a magnetic field. When applying a magnetic field, and in the absence of mechanical deformations, the electrical capacity of the MTS (Figure 14a,b) increases significantly with increasing magnetic field strength. By superimposing the magnetic field over the field of deformations, consisting of forces up to 3 N, (Figure 14a), a significant increase in the electrical response provided by the MTS is observed, (Figure 15b). Therefore, by applying a magnetic field, it is possible to achieve a controlled increase in the MTS sensitivity.

The elasticity constant (Figure 16a) and Young's modulus (Figure 16b) are strongly influenced by the external magnetic field. The proposed theoretical model (see Appendix) qualitatively describes the mechanisms leading to the experimental results obtained in this paper.

Author Contributions: Conceptualization, I.B., G.-E.I., and L.-M.-E.C.; methodology, I.B.; validation, G.-E.I.; formal analysis, I.B. and G.-E.I.; investigation, I.B.; data curation, I.B.; writing—original draft preparation, I.B.; writing—review and editing, G.-E.I.; visualization, I.B.; supervision, G.-E.I. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Institutional Review Board Statement: Not applicable

Informed Consent Statement: Not applicable

Acknowledgments: The authors would like to thank Paula Sfirloaga from INCEMC-Timisoara, Păunescu Podeanu, for performing the SEM analyses and crystallographic analyses.

Conflicts of Interest: The authors declare no conflicts of interest.

Appendix A

Appendix A.1. MTS Subjected to a Field of Compression Forces

Suppose we perform a cross section through MTS, as shown in Figure A1.



Figure A1. Cross section through MTS: (**a**) in the absence of the magnetic field and the deforming forces, (**b**) after applying the compression force, $F \neq 0$ (CI, carbonyl iron microparticles; Cu, copper foil; PS, polyurethane sponge; k, elasticity constant; \vec{F} , compression force vector, Oz, coordinate axis; δ and z, distances between the mass centers of the CI microparticles for F = 0 and $F \neq 0$, respectively).

According to the model represented graphically in Figure A1, the polyurethane sponge, PS, consists of identical fibers of elastic constant k. In the MTS bulk, we consider the fibers interconnected by means of CI microparticles, forming parallel and equidistant columns. The extremities of each column chain are in electrical contact with the copper foil by means of metal microparticles. In the absence of deformations (F = 0), the thickness of MPS is h_0 . When applying the mass, m, the gravitational force F acts on MTS. The effect of F is a reduction in the MPS thickness to a value $h < h_0$. Consequently, deformations in the direction of the Oz axis occur in the MPS body.

$$e_{zz} = \frac{h}{h_0} - 1 \tag{A1}$$

where the notations are as outlined above.

From the definition of the electrical capacity of a planar capacitor, we obtain the thicknesses of the MPS of the form:

$$h_0 = \frac{\varepsilon_0 \cdot \varepsilon' L \cdot l}{c_{m0}}$$
 for $F = 0$ (A2)

and

$$h = \frac{\varepsilon_0 \cdot \varepsilon' L \cdot l}{c_m} \text{ for } F \neq 0$$
(A3)

where ε_0 and ε' are the dielectric constant of the vacuum and the dielectric permittivity of MPs, respectively; L and l are the length and width of MPS, respectively; and C_{m0} and C_m are the electrical capacity of MTS in the absence and in the presence of the deformation forces, respectively.

By replacing Equations (A2) and (A3) in Definition (A1), we obtain:

$$e_{zz} = \frac{c_{m0}}{c_m} - 1 \tag{A4}$$

Between the components of the deformation along the Oz axis, e_{zz} , and the variation in MPS thickness, Δh , there is the equation:

$$\Delta h = h_0 \cdot e_{zz} \tag{A5}$$

For linear and perfectly elastic MPS, between the force, F, and the variation in MPS thickness, Δh , the following equation is fulfilled:

$$F = -k \cdot \Delta h \tag{A6}$$

where k is the elastic constant of MPS in the absence of the magnetic field. From Equations (A4)–(A6), we obtain:

$$F = -k \cdot h_0 \cdot e_{zz} \tag{A7}$$

where the notations are as outlined above.

Between the hydrostatic pressure, p, and the components of the deformation along the Oz axis, e_{zz} , there is a relation of form:

$$\frac{F}{S} = p = -E \cdot e_{zz} \tag{A8}$$

where E is Young's modulus.

The existence of additives (holes and microfibers in MPS) affects the initial distance between the mass centers of the CI microparticles [52], as:

$$\delta = \frac{d_{CI}}{\sqrt[3]{\varphi_{CI}/(1+\varphi_f + \varphi_a)}} \tag{A9}$$

where the notations are as outlined above.

If, in Equation (A9), we introduce the values $d_{CI} = 5 \,\mu m$, $\varphi_{CI} = 0.46 \,$ %vol, $\varphi_f = 92.3 \,$ %vol., and $\varphi_a = 7.24 \,$ %vol., we find that the initial distance between the CI microparticles, before the application of the mass, m, and/or the magnetic field, is:

$$\delta \approx 2169 \,\mu m$$
 (A10)

The result of this model, given by Equation (A10), assumes that $\delta \gg d_{CI}$.

Two neighboring metal particles, from each chain, form an electric microcapacitor. The electrical capacity of an electric microcapacitor, represented in Figure A2, is [55,56]:

$$C = 4 \cdot \pi \cdot \varepsilon_0 \cdot \varepsilon' \cdot \frac{r^2}{d} \cdot \left(1 + \frac{r^2}{d^2 - 2 \cdot r^2} + \frac{r^4}{d^4 - 4 \cdot d^2 \cdot r^2 + 3 \cdot r^3} + \cdots\right)$$
(A11)

where ε_0 is the dielectric constant of the vacuum, ε' is the relative dielectric permittivity of MPS, r is the radius of the metallic particles, and d is the distance between the mass centers of CI microparticles.



Figure A2. Two metal particles forming an electric capacitor [55,56].

In the case of the MPS in Figure A1a, two neighboring CI microparticles form, along the Oz axis, an electric microcapacitor similar to the two metal balls in Figure A2, in which the radius of the CI microparticle is $r = 0.5 \cdot d_{CI}$ and the distance between the mass centers is $d = \delta$. For $d = \delta \approx 2169 \,\mu\text{m}$ and $r = 0.5 \cdot d_{CI} = 2.5 \,\mu\text{m}$, the condition $d^2 \gg r^2$ is fulfilled, and we can use Equation (A11) [55,56]. Then, for $\delta^2 \gg (0.5 \cdot d_{CI})^2$, the electrical capacity of the microcapacitors from Figure A2 is:

$$C_1 = 4 \cdot \pi \cdot \varepsilon_0 \cdot \varepsilon' \cdot \frac{d_{CI}^2}{\delta} \tag{A12}$$

where the notations are as outlined above.

We estimate the number of CI microparticles in MTS by the equation:

$$n = \frac{\varphi_{CI} \cdot V_{MTS}}{V_{CI}} = \frac{6 \cdot \varphi_{CI} \cdot L \cdot l \cdot h_0}{\pi \cdot d_{CI}^3}$$
(A13)

where φ_{CI} is the volumetric fraction of the CI microparticles; V_{MTS} is the volume of MTS; V_{CI} is the volume of a CI microparticle; L, l, and h_0 are the length, width, and thickness of MTS, respectively; and d_{CI} is the diameter of the microparticle CI.

For the thickness h_0 of MTS, the number n_1 of solid microparticles, from each column, can be approximated with the expression:

$$n_1 = \frac{h_0}{d_{Cl}} \tag{A14}$$

We consider the columns with n_1 microparticles uniformly distributed in the volume of the PS sponge. Then, the number n_2 of columns with CI microparticles is $n_2 = n/n_1$ and, taking into consideration Equations (A13) and (A14), it results in:

1

$$n_2 = \frac{6 \cdot \varphi_{CI} \cdot L \cdot l}{\pi \cdot d_{CI}^2} \tag{A15}$$

The number of capacitors, connected in series, in a column of CI microparticles is $(n_1 - 1)$. Then, from Equations (A12) and (A14), we obtain the expression of the electrical capacity of a column of microparticles CI, C_c as follows:

$$C_{c} = C_{1}/(n_{1} - 1) = C_{1}/n_{1} = 4\pi\varepsilon_{0}\varepsilon' d_{CI}^{3}/h_{0}\delta, \text{ for } n_{1} \gg 1$$
(A16)

In Equation (A16), we introduce the quantity δ from Equation (A9), and we obtain:

$$C_c = \frac{4\pi\varepsilon_0\varepsilon'd_{CI}^2}{h_0} \cdot \sqrt[3]{\varphi_{CI}\cdot\left(1+\varphi_f+\varphi_a\right)}$$
(A17)

The electrical capacity C_0 of MTS from Figure A1a is obtained from the n_2 capacities C_c , electrically connected, in parallel, via copper foil, that is:

$$C_0 = n_2 \cdot C_c \tag{A18}$$

If we introduce Equations (A15) and (A17) into the definition (A18), we obtain:

$$C_0 = \frac{A}{h_0'}$$
 for $F = 0$ (A19)

where

$$A = 24\varepsilon_0\varepsilon'\cdot\varphi_{CI}\cdot L\cdot l\cdot\sqrt[3]{\varphi_{CI}\cdot\left(1+\varphi_f+\varphi_a\right)}$$
(A20)

It is observed from the expression (A19) with the notation (A20) that C_0 is determined by the geometric dimensions of MTS and by the volumetric fractions of the CI microparticles, φ_{CI} , of the polyurethane fibers, φ_f , and of the halls from PS occupied by ambient air, φ_a .

In the force field F, the thickness of MPS takes values $h < h_0$; then, based on the same arguments, the C_m capacity of MTS is:

$$C_m = \frac{A}{h} > C_0, \text{ for } F \neq 0 \tag{A21}$$

Appendix A.2. MTS Subjected to a Magnetic Field

We assume that when applying an external magnetic field, the CI microparticles instantly transform into magnetic dipoles and they remain anchored to the ends of the polyurethane fibers, as shown in Figure A3.



Figure A3. Cross section by MTS: (**a**) in the absence of the magnetic field and the deforming forces; (**b**) after the application of the magnetic field ($\vec{\mu}$, magnetic moment vector; Cu, copper foil; PS, polyurethane sponge; k, k_µ, elastic constants before and after the application of the magnetic field, respectively; \vec{H} , magnetic field intensity vector; Oz, coordinate axis; δ , the initial distance between the mass centers of the CI microparticles; z_{μ} , the distance between the magnetic dipoles at the moment t from the application of H).

The magnetic moments, $\vec{\mu}$, are aligned in the direction of the Oz axis, parallel to that of \vec{H} . The size μ is calculated with the formula [44]:

$$\mu = 0.5\pi d_{CI}^3 H \tag{A22}$$

where d_{CI} is the diameter of $\vec{\mu}$, identical to that of the CI microparticles.

Magnetic interactions occur between the dipoles $\vec{\mu}$. The calculation of the interaction intensity, for $B = \mu_0 H$, projected on the Oz axis and used in [52,54], takes the following form:

$$F_{m_z} = -\frac{3\mu_0 \cdot \mu^2}{2\pi z_{\mu}^4}$$
(A23)

where $\mu_0 = 4\pi \cdot 10^{-7} H/m$, the vacuum permeability, and z_{μ} is the distance between the centers of mass of the magnetic dipoles.

From Equations (A22) and (A23), for $z_{\mu} = d_{CI}$, we obtain:

$$F_{m_z} = -\frac{3}{8}\pi \,\mu_0 d_{CI}^2 H^2 \tag{A24}$$

where the notations are as outlined above.

Assuming that, in each column of dipoles (Figure A3), the force F_{m_z} is the same, then, the n_2 columns of dipoles create the total magnetic force:

$$F_m = n_2 F_{m_z} \tag{A25}$$

From Equations (A15), (A24), and (A25), we obtain:

$$F_m = -2,25 \cdot \varphi_{Cl} \cdot L \cdot l \cdot \mu_0 \cdot H^2 \tag{A26}$$

It is observed from Equation (A26) that the magnetic force induced by the magnetic field in MPS, F_m, is independent of the diameter of the magnetic dipoles but depends on the geometric dimensions of MPS and is significantly influenced by the intensity H of the magnetic field.

According to the Third Law of Dynamics, the action force F_m is opposed by a resistive force, which, in the case of MPS, is the elastic force, that is:

$$F_{el.m} = -k_{\mu} \cdot (h_H - h_0) \tag{A27}$$

where k_{μ} is the elastic constant, h_{H} is the thickness of MPS in Figure A3b, and h_{0} is the thickness of MPS in Figure A3a.

At equilibrium, we have the following equality:

$$F_m = -F_{el.m} \tag{A28}$$

We introduce Equations (A26) and (A27) in the equality (A28), and we obtain:

$$h_{H} = h_{0} - \frac{2,25 \cdot \varphi_{CI} \cdot L \cdot l \cdot \mu_{0} \cdot H^{2}}{k_{\mu}}$$
(A29)

where the notations used have been previously defined.

It is observed from Equation (A29) that the thickness h_H decreases significantly with an increase in the size H.

The electrical capacity of MTS, considered a flat capacitor, is calculated with the formulae:

$$C_0 = \frac{\varepsilon_0 \cdot \varepsilon' L \cdot l}{h_0}$$
, for $F = 0$ and $H = 0$ (A30)

$$C_H = \frac{\varepsilon_0 \cdot \varepsilon' L \cdot l}{h_H}$$
, for $F = 0$ and $H \neq 0$ (A31)

With the result (A29) introduced in Formula (A31), and taking into consideration (A30), we obtain:

$$C_{H} = \frac{C_{0}}{1 - \frac{2.25 \cdot \varphi_{CI} \cdot l \cdot \mu_{0} \cdot H^{2}}{h_{0} k_{\mu}}} \text{ for } F = 0 \text{ and } H \neq 0$$
(A32)

From Equation (A32), it is observed that, in the absence of deforming forces, the values of $C_{\rm H}$ are significantly influenced by the intensity of the magnetic field applied to the MTS.

Appendix A.3. MTS Subjected to a Magnetic Field Superimposed on a Field of Compression Forces

If a field of mechanical forces overlaps the magnetic field, $F \neq 0$ and $H \neq 0$ (Figure A4b), the following reaction force arises in the MPS body in the direction of the Oz axis:

$$F_{el.mF} = -k_{\mu F} \cdot (h_{HF} - h_0) \tag{A33}$$

where $k_{\mu F}$ is the elastic constant of the microfibers, h_{HF} is the thickness of MPS in Figure A4b, and h_0 is the thickness of MPS in Figure A4a.



Figure A4. Cross section by MTS: (**a**) in the absence of the magnetic field and deforming forces; (**b**) after the application of the magnetic field superimposed over the field of deforming forces ($\vec{\mu}$, magnetic moment vector; Cu, copper foil; PS, polyurethane sponge; $k_{\mu F}$, elastic constant at the application of H and F; \vec{H} , magnetic field intensity vector; Oz, coordinate axis; δ , the initial distance between the mass centers of the CI microparticles; $z_{\mu F}$, the distance between the magnetic dipoles at the moment t from the application of H and F).

At equilibrium, between the quantities F, F_m, and F_{el.mF}, there is the equation:

$$-(F + F_m) = -F_{el.mF} \tag{A34}$$

If, in Equation (A34), we introduce Equations (A26) and (A31), we obtain:

$$h_{HF} = h_0 \cdot \left(1 - \frac{F + 2,25 \cdot \varphi_{CI} \cdot L \cdot l \cdot \mu_0 \cdot H^2}{h_0 \cdot k_{\mu F}} \right)$$
(A35)

From Equation (A35), it is observed that the thickness of MPS, under magnetic field and deforming mechanical actions, strongly decreases, $h_{HF} \ll h_0$.

By introducing h_{mF} in the well-known formula for calculating the electrical capacity of the flat capacitor, we obtain:

$$C_{HF} = \frac{C_{HF_0}}{1 - \frac{F + 2.25 \cdot \varphi_{CF} L \cdot l \cdot \mu_0 \cdot H^2 r}{h_0 k_{\mu F}}} \text{ for } F \neq 0 \text{ and } H \neq 0$$
(A36)

where, by C_{HF_0} , we note:

$$C_{HF_0} = \frac{\varepsilon_0 \cdot \varepsilon' L \cdot l}{h_0} \equiv C_0$$
, for $F = 0$ and $H = 0$ (A37)

It is observed from Equation (A36) that, in the absence of the magnetic field, by applying forces, F, the electrical capacity of MTS increases linearly with an increase in F. Instead, when the magnetic field, H, overlaps the field of the deforming forces, F, the electrical capacity of MTS increases with an increase in F, but the significant increasing influence comes from H.

From Equation (A36) we obtain the elastic constant of MPS, $k_{\mu F}$, as:

$$k_{\mu F} = \frac{F + 2,25 \cdot \varphi_{CI} \cdot L \cdot l \cdot \mu_0 \cdot H^2}{h_0 \cdot \left(1 - \frac{C_{HF_0}}{C_{HF}}\right)}$$
(A38)

where F is the compressive force, φ_{CI} is the volumetric fractions of the CI microparticles, L, l, and h₀ are the length, width, and thickness of MPS, respectively, μ_0 is the vacuum permeability, C_{HF_0} is the electrical capacity of MPS in the absence of both magnetic and deformation fields, and C_{HF} is the electrical capacity of MPS in a magnetic field in the presence of mechanical deformations.

The deformation components are defined by the equation:

$$\varepsilon_{HF} = \frac{h_{HF}}{h_0} - 1 = \frac{C_{HF_0}}{C_{HF}} - 1$$
(A39)

The pressure exerted by the force field, F, and the magnetic field, H, on MPS is:

$$r_{HF} = \frac{F}{L \cdot l} + 2,25 \cdot \varphi_{CI} \cdot \mu_0 \cdot H^2 \tag{A40}$$

Assuming that MPS is a linear and elastic medium, between the tension τ_{HF} and the components ε_{HF} of the deformations, there is the relation:

$$\varepsilon_{HF} = E_{HF} \cdot \varepsilon_{HF} \tag{A41}$$

From Equation (A41), with Equations (A33) and (A39), we obtain the Young's modulus of MPS in a magnetic field, H, superimposed on mechanical deformations, F, as:

$$E_{HF} = \frac{h_0 \cdot k_{\mu F}}{L \cdot l} \tag{A42}$$

References

- Sun, X.; Sun, J.; Li, T.; Zheng, S.; Wang, C.; Tan, W.; Zhang, J.; Liu, C.; Ma, T.; Qi, Z.; Liu, C.; Xue, N. Flexible Tactile Electronic Skin Sensor with 3D Force Detection Based on Porous CNTs/PDMS Nanocomposites. *Nano-Micro Lett.* 2019, 11, 57.
- Chittibabu, S.K.; Chintagumpala, K.; Chandrasekhar, A. Porous dielectric materials based wearable capacitance pressure sensors for vital signs monitoring: A review. *Mater. Sci. Semicond. Process.* 2022, 151, 106976. https://doi.org/10.1016/j.mssp.2022.106976.
- Gao, Y.; Xiao, T.; Li, Q.; Chen, Y.; Qiu, X.; Liu, J.; Bian, Y.; Xuan, F.-Z. Flexible microstructured pressure sensors: Design, fabrication and applications. *Nanotechnology* 2022, 33, 322002. https://doi.org/10.1088/1361-6528/ac6812.
- 4. Weng, X.; Zhang, C.; Feng, C.; Jiang, H. Facile Fabrication of an Ultrasensitive All-Fabric Wearable Pressure Sensor Based on Phosphorene-Gold Nanocomposites. *Adv. Mater. Interfaces* **2022**, *9*, 2102588. https://doi.org/10.1002/admi.202102588.
- Kang, D.; Pikhitsa, P.V.; Choi, Y.W.; Lee, C.; Shin, S.S.; Piao, L.; Park, B.; Suh, K.Y.; Kim, T.I.; Choi, M. Ultrasensitive mechanical crack-based sensor inspired by the spider sensory system. *Nature* 2014, *516*, 222–226. https://doi.org/10.1038/nature14002.
- 6. Alfadhel, A.; Kosel, J. Magnetic Nanocomposite Cilia Tactile Sensor. *Adv. Mater.* 2015, 27, 7888–7892. https://doi.org/10.1002/adma.201504015.
- Wang, H.L.; Guo, Z.H.; Pu, X.; Wang, Z.L. Ultralight Iontronic Triboelectric Mechanoreceptor with High Specific Outputs for Epidermal Electronics. *Nano-Micro Lett.* 2022, 14, 86. https://doi.org/10.1007/s40820-022-00834-4.
- 8. Kurup, L.A.; Arthur, J.N.; Yambem, S.D. Highly Sensitive Capacitive Low-Pressure Graphene Porous Foam Sensors. *ACS Appl. Electron. Mater.* **2022**, *4*, 3962–3972. https://doi.org/10.1021/acsaelm.2c00616.
- Wu, D.; Cheng, X.; Chen, Z.; Xu, Z.; Zhu, M.; Zhao, Y.; Zhu, R.; Lin, L. A flexible tactile sensor that uses polyimide/graphene oxide nanofiber as dielectric membrane for vertical and lateral force detection. *Nanotechnology* 2022, 33, 405205. https://doi.org/10.1088/1361-6528/ac73a4.
- 10. Kim, H.; Kim, G.; Kim, T.; Lee, S.; Kang, D.; Hwang, M.-S.; Chae, Y.; Kang, S.; Lee, H.; Park, H.-G.; et al. Transparent, Flexible, Conformal Capacitive Pressure Sensors with Nanoparticles. *Small* **2018**, *14*, 1703432. https://doi.org/10.1002/smll.201703432.
- 11. Pavel, I.-A.; Lakard, S.; Lakard, B. Flexible Sensors Based on Conductive Polymers. *Chemosensors* **2022**, *10*, *97*. https://doi.org/10.3390/chemosensors10030097.
- Xie, L.; Chen, X.; Wen, Z.; Yang, Y.; Shi, J.; Chen, C.; Peng, M.; Liu, Y.; Sun, X. Spiral Steel Wire Based Fiber-Shaped Stretchable and Tailorable Triboelectric Nanogenerator for Wearable Power Source and Active Gesture Sensor. *Nano-Micro Lett.* 2019, *11*, 39. https://doi.org/10.1007/s40820-019-0271-3.
- 13. Hua, Q.; Sun, J.; Liu, H.; Bao, R.; Yu, R.; Zhai, J.; Pan, C.; Wang, Z.L. Skin-inspired highly stretchable and conformable matrix networks for multifunctional sensing. *Nat. Commun.* **2018**, *9*, 244. https://doi.org/10.1038/s41467-017-02685-9.

- Lo, L.-W.; Zhao, J.; Aono, K.; Li, W.; Wen, Z.; Pizzella, S.; Wang, Y.; Chakrabartty, S.; Wang, C. Stretchable Sponge Electrodes for Long-Term and Motion-Artifact-Tolerant Recording of High-Quality Electrophysiologic Signals. ACS Nano 2022, 16, 11792– 11801. https://doi.org/10.1021/acsnano.2c04962.
- Chen, H.; Song, Y.; Guo, H.; Miao, L.; Chen, X.; Su, Z.; Zhang, H. Hybrid porous micro structured finger skin inspired selfpowered electronic skin system for pressure sensing and sliding detection. *Nano Energy* 2018, *51*, 496–503. https://doi.org/10.1016/j.nanoen.2018.07.001.
- 16. Wang, X.; Ling, X.; Hu, Y.; Hu, X.; Zhang, Q.; Sun, K.; Xiang, Y. Electronic skin based on PLLA/TFT/PVDF-TrFE array for Multi-Functional tactile sensing and visualized restoring. *Chem. Eng. J.* **2022**, 434, 134735. https://doi.org/10.1016/j.cej.2022.134735.
- Tao, Z.; Huang, Y.-A.; Liu, X.; Chen, J.; Lei, W.; Wang, X.; Pan, L.; Pan, J.; Huang, Q.; Zhang, Z. High-Performance Photo-Modulated Thin-Film Transistor Based on Quantum dots/Reduced Graphene Oxide Fragment-Decorated ZnO Nanowires. *Nano-Micro Lett.* 2016, *8*, 247–253. https://doi.org/10.1007/s40820-016-0083-7.
- Bai, S.; Zhang, S.; Zhou, W.; Ma, D.; Ma, Y.; Joshi, P.; Hu, A. Laser-Assisted Reduction of Highly Conductive Circuits Based on Copper Nitrate for Flexible Printed Sensors. *Nano-Micro Lett.* 2017, *9*, 42. https://doi.org/10.1007/s40820-017-0139-3.
- Kim, Y.; Chortos, A.; Xu, W.; Liu, Y.; Oh, J.Y.; Son, D.; Kang, J.; Foudeh, A.M.; Zhu, C.; Lee, Y.; et al. A bioinspired flexible organic artificial afferent nerve. *Science* 2018, *360*, 998–1003. https://doi.org/10.1126/science.aa00098.
- 20. Nguyen, T.-D.; Lee, J.S. Recent Development of Flexible Tactile Sensors and Their Applications. *Sensors* 2021, 22, 50. https://doi.org/10.3390/s22010050.
- Jiang, C.; Liu, J.; Yang, L.; Gong, J.; Wei, H.; Xu, W. A Flexible Artificial Sensory Nerve Enabled by Nanoparticle-Assembled Synaptic Devices for Neuromorphic Tactile Recognition. *Adv. Sci.* 2022, *9*, 2106124. https://doi.org/10.1002/advs.202106124.
- Liu, W.; Liu, N.; Yue, Y.; Rao, J.; Cheng, F.; Su, J.; Liu, Z.; Gao, Y. Piezoresistive Pressure Sensor Based on Synergistical Innerconnect Polyvinyl Alcohol Nanowires/Wrinkled Graphene Film. *Small* 2018, 14, e1704149. https://doi.org/10.1002/smll.201704149.
- Sun, X.; Wang, C.; Chi, C.; Xue, N.; Liu, C. A highly-sensitive flexible tactile sensor array utilizing piezoresistive carbon nanotube–polydimethylsiloxane composite. *J. Micromech. Microeng.* 2018, 28, 105011. https://doi.org/10.1088/1361-6439/aaceb9.
- Li, T.; Luo, H.; Qin, L.; Wang, X.; Xiong, Z.; Ding, H.; Gu, Y.; Liu, Z.; Zhang, T. Flexible Capacitive Tactile Sensor Based on Micropatterned Dielectric Layer. Small 2016, 12, 5042–5048. https://doi.org/10.1002/smll.201600760.
- Choi, D.; Jang, S.; Kim, J.S.; Kim, H.-J.; Kim, D.H.; Kwon, J.-Y. A Highly Sensitive Tactile Sensor Using a Pyramid-Plug Structure for Detecting Pressure, Shear Force, and Torsion. *Adv. Mater. Technol.* 2018, *4*, 1800284. https://doi.org/10.1002/admt.201800284.
- Shu, Y.; Tian, H.; Yang, Y.; Li, C.; Cui, Y.; Mi, W.; Li, Y.; Wang, Z.; Deng, N.; Peng, B.; et al. Surface-modified piezoresistive nanocomposite flexible pressure sensors with high sensitivity and wide linearity. *Nanoscale* 2015, 7, 8636–8644. https://doi.org/10.1039/c5nr01259g.
- 27. Park, C.-S.; Park, J.; Lee, D.-W. A piezoresistive tactile sensor based on carbon fibers and polymer substrates. *Microelectron. Eng.* **2009**, *86*, 1250–1253. https://doi.org/10.1016/j.mee.2008.12.072.
- Pan, L.; Chortos, A.; Yu, G.; Wang, Y.; Isaacson, S.; Allen, R.; Shi, Y.; Dauskardt, R.; Bao, Z. An ultra-sensitive resistive pressure sensor based on hollow-sphere microstructure induced elasticity in conducting polymer film. *Nat. Commun.* 2014, *5*, 3002. https://doi.org/10.1038/ncomms4002.
- 29. Tang, Z.; Jia, S.; Shi, S.; Wang, F.; Li, B. Coaxial carbon nanotube/polymer fibers as wearable piezoresistive sensors. *Sensors Actuators A Phys.* **2018**, *284*, 85–95. https://doi.org/10.1016/j.sna.2018.10.012.
- A Dobrzynska, J.; Gijs, M.A.M. Polymer-based flexible capacitive sensor for three-axial force measurements. J. Micromech. Microeng. 2013, 23, 015009. https://doi.org/10.1088/0960-1317/23/1/015009.
- Kim, M.-S.; Ahn, H.-R.; Lee, S.; Kim, C.; Kim, Y.-J. A dome-shaped piezoelectric tactile sensor arrays fabricated by an air inflation technique. Sensors Actuators A Phys. 2014, 212, 151–158. https://doi.org/10.1016/j.sna.2014.02.023.
- Chiappim, W.; Fraga, M.A.; Furlan, H.; Ardiles, D.C.; Pessoa, R.S. The status and perspectives of nanostructured materials and fabrication processes for wearable piezoresistive sensors. *Microsyst. Technol.* 2022, 28, 1561–1580. https://doi.org/10.1007/s00542-022-05269-w.
- Ahmadi, R.; Packirisamy, M.; Dargahi, J.; Cecere, R. Discretely Loaded Beam-Type Optical Fiber Tactile Sensor for Tissue Manipulation and Palpation in Minimally Invasive Robotic Surgery. *IEEE Sensors J.* 2012, 12, 22–32. https://doi.org/10.1109/jsen.2011.2113394.
- Li, X.; Huang, W.; Yao, G.; Gao, M.; Wei, X.; Liu, Z.; Zhang, H.; Gong, T.; Yu, B. Highly sensitive flexible tactile sensors based on microstructured multiwall carbon nanotube arrays. *Scr. Mater.* 2017, 129, 61–64. https://doi.org/10.1016/j.scriptamat.2016.10.037.
- Hasan, S.A.U.; Jung, Y.; Kim, S.; Jung, C.-L.; Oh, S.; Kim, J.; Lim, H. A Sensitivity Enhanced MWCNT/PDMS Tactile Sensor Using Micropillars and Low Energy Ar+ Ion Beam Treatment. *Sensors* 2016, 16, 93. https://doi.org/10.3390/s16010093.
- Wang, J.J.; Lu, C.E.; Huang, J.L.; Chen, R.; Fang, W. Nano-composite rubber elastomer with piezoresistive detection for flexible tactile sense application. In Proceedings of the 2017 IEEE 30th International Conference on Micro Electro Mechanical Systems (MEMS), Las Vegas, NV, USA, 22–26 January 2017; pp. 720–723. https://doi.org/10.1109/memsys.2017.7863509.
- Chun, S.; Hong, A.; Choi, Y.; Ha, C.; Park, W. A tactile sensor using a conductive graphene-sponge composite. *Nanoscale* 2016, 8, 9185–9192. https://doi.org/10.1039/c6nr00774k.
- Zhang, J.; Zhou, L.J.; Zhang, H.M.; Zhao, Z.X.; Dong, S.L.; Wei, S.; Zhao, J.; Wang, Z.L.; Guo, B.; Hu, P.A. Highly sensitive flexible three-axis tactile sensors based on the interface contact resistance of microstructured graphene. *Nanoscale* 2018, 10, 7387– 7395. https://doi.org/10.1039/c7nr09149d.

- Pei, Z.; Hu, H.; Liang, G.; Ye, C. Carbon-Based Flexible and All-Solid-State Micro-supercapacitors Fabricated by Inkjet Printing with Enhanced Performance. *Nano-Micro Lett.* 2017, *9*, 19. https://doi.org/10.1007/s40820-016-0119-z.
- Wang, J.; Jiu, J.; Araki, T.; Nogi, M.; Sugahara, T.; Nagao, S.; Koga, H.; He, P.; Suganuma, K. Silver Nanowire Electrodes: Conductivity Improvement Without Post-treatment and Application in Capacitive Pressure Sensors. *Nano-Micro Lett.* 2015, 7, 51– 58. https://doi.org/10.1007/s40820-014-0018-0.
- 41. Weng, L.; Xie, G.; Zhang, B.; Huang, W.; Wang, B.; Deng, Z. Magnetostrictive tactile sensor array for force and stiffness detection. *J. Magn. Mater.* **2020**, *513*, 167068. https://doi.org/10.1016/j.jmmm.2020.167068.
- 42. Bica, I.; Anitas, E.M. Electrical devices based on hybrid membranes with mechanically and magnetically controllable, resistive, capacitive and piezoelectric properties. *Smart Mater. Struct.* **2022**, *31*, 045001. https://doi.org/10.1088/1361-665x/ac4ea7.
- Pascu, G.; Bunoiu, O.M.; Bica, I. Magnetic Field Effects Induced in Electrical Devices Based on Cotton Fiber Composites, Carbonyl Iron Microparticles and Barium Titanate Nanoparticles. *Nanomaterials* 2022, 12, 888. https://doi.org/10.3390/nano12050888.
- Bica, I.; Bălăşoiu, M.; Sfirloaga, P. Effects of electric and magnetic fields on dielectric and elastic properties of membranes composed of cotton fabric and carbonyl iron microparticles. *Results Phys.* 2022, 35, 105332. https://doi.org/10.1016/j.rinp.2022.105332.
- Bica, I.; Iacobescu, G.-E. Magneto-Dielectric Effects in Polyurethane Sponge Modified with Carbonyl Iron for Applications in Low-Cost Magnetic Sensors. *Polymers* 2022, 14, 2062. https://doi.org/10.3390/polym14102062.
- 46. Ercuta, A. Sensitive AC Hysteresigraph of Extended Driving Field Capability. *IEEE Trans. Instrum. Meas.* **2020**, *69*, 1643–1651. https://doi.org/10.1109/tim.2019.2917237.
- 47. Japka, J.E. Microstructure and Properties of Carbonyl Iron Powder. JOM 1988, 40, 18–21. https://doi.org/10.1007/bf03258115.
- Atkins, A.J.; Bauer, M.; Jacob, C.R. High-resolution X-ray absorption spectroscopy of iron carbonyl complexes. *Phys. Chem. Chem. Phys.* 2015, 17, 13937–13948. https://doi.org/10.1039/c5cp01045d.
- König, R.; Müller, S.; Dinnebier, R.E.; Hinrichsen, B.; Müller, P.; Ribbens, A.; Hwang, J.; Liebscher, R.; Etter, M.; Pistidda, C. The crystal structures of carbonyl iron powder—revised using in situ synchrotron XRPD. Z. Krist. Cryst. Mater. 2017, 232, 835–842 https://doi.org/10.1515/zkri-2017-2067.
- 50. Huang, C.; Niu, H.; Wu, J.; Ke, Q.; Mo, X.; Lin, T. Needleless Electrospinning of Polystyrene Fibers with an Oriented Surface Line Texture. *J. Nanomater.* **2012**, 2012, 473872. https://doi.org/10.1155/2012/473872.
- Bica, I.; Anitas, E.M.; Choi, H.J.; Sfirloaga, P. Microwave-assisted synthesis and characterization of iron oxide microfibers. J. Mater. Chem. C 2020, 8, 6159–6167. https://doi.org/10.1039/c9tc05687d.
- 52. Bica, I.; Anitas, E. Magnetic flux density effect on electrical properties and visco-elastic state of magnetoactive tissues. *Compos. Part B Eng.* **2019**, *15*, 13–19. https://doi.org/10.1016/j.compositesb.2018.09.058.
- 53. Genç, S. Synthesis and Properties of Magnethoreological (MR) Fluids. Ph.D Thesis, University of Pitsburgh, Pittsburgh, PA, USA, 2002.
- Bica, I.; Anitas, E.M.; Chirigiu, L. Hybrid Magnetorheological Composites for Electric and Magnetic Field Sensors and Transducers. *Nanomaterials* 2020, 10, 2060. https://doi.org/10.3390/nano10102060.
- 55. Terman, F.E. Radio Engineers' Handbook; McGraw-Hill: New York, NY, USA, 1943.
- 56. Rawlins, A. Note on the Capacitance of Two Closely Separated Spheres. *IMA J. Appl. Math.* **1985**, 34, 119–120. https://doi.org/10.1093/imamat/34.1.119.