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Parameter Estimation in the Mathematical Model of Bacterial Colony Patterns in Symmetry Domain

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Abstract: The paper presents a solution to the problem related to the reconstruction of parameters in the mathematical model of bacterial colony patterns in a domain with symmetry. The inverse problem consists of determining the value of the diffusion coefficient of active bacteria. The model describing the distribution of active bacteria in a given region, as well as the concentration of the substrate over time is considered. Such a model consists of a system of partial differential equations with appropriate initial-boundary conditions. The finite element method was used to solve the direct problem. However, the Fibonacci search method was used to minimize the functional description of the error of the approximate solution.

Keywords: inverse problem; mathematical modeling; bacterial colony pattern; diffusion coefficient

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1. Introduction

Each ecosystem on the Earth is inhabited by communities of bacteria and other microorganisms. They occur on the surfaces of objects, in soil, and in water, and they live in the body of humans and animals. They often form on surfaces dense colonies called biofilms. Its structure of it depends on physical, chemical and biological factors. Among the many specific factors of growth and functioning of the colony, the most important should be access to water and nutrients, and the characteristics of the substrate [1–3].

Most biofilms found in nature are mixtures of different species of bacteria. In such cases, competition for a specific ecological niche is most often observed. When studying single-species biofilm, the development of a given colony can be observed depending on the variety of environmental conditions. A common microorganism used in bacterial colony studies is the Gram-positive bacterium *Bacillus subtilis*. It is a model organism, in particular, used to observe the formation of biofilm by bacteria and the way bacteria move in various environments and on various substrates [1,2,4]. This type of bacteria is quite widespread and also does not show pathogenic properties in the basic form. *B. subtilis* is an important component of the human microflora, it is present, inter alia, on the skin surface and in the gastrointestinal tract. It is a symbiote that produces a compound called bacitracin, which inhibits the growth of other Gram-positive bacteria. As a result, these bacteria are used in the pharmaceutical industry [2,5,6].

Experimental and mathematical modeling is an important study of bacterial colonies with regard to their application in various branches of the economy. Due to the fact that *B. subtilis* is a bacterium that differentiates quickly and shows the possibility of various types of motility, the microorganism can be used to model the behavior of Gram-positive bacteria, in general, [5,7]. Modeling the behavior of *B. subtilis*, as for example, in the papers [8–11], change the behavior of the colony depending on the parameters of the environment. The

adaptive abilities of bacteria allow the observation of various types of motility, communication and reproduction methods. As a result, it is possible to determine the mechanisms shaping the desired development of bacterial colonies and the patterns adopted by them, which is conducive to the optimization of biological research and production of substances using Gram-positive bacteria [8–11].

Inverse problems have an important role in science. Solving inverse problems of various kinds allows for more accurate modeling of various processes [12–18]. For example, in [12], authors compared various mathematical models of heat conduction based on temperature measurements of porous aluminum. In order to perform the comparison, an inverse problem had to be solved, consisting in identifying several model coefficients. The Ant Colony Optimization algorithm was used to solve this problem. In paper [14] a novel spatially and temporally controlled heating method was proposed. The laser configuration was achieved by solving the inverse heat conduction problem. In papers [17,18] from the knowledge of temperature measurements the aerothermal heating of a reusable launch vehicle is reconstructed. For solving the direct problem the implicit scheme of the finite difference method is used, whereas the solution to the inverse problem is determined with the aid of the Levenberg–Marquardt method. More about inverse problems can be found in [19–21].

Examples of the application of inverse problems in biological sciences can be found in the papers [22–26]. Abdulla and Poteau in paper [23] describe the identification of parameters for a model of a biological system described by a system of nonlinear ordinary differential equations. The presented method is a combination of Bellman's quasilinearization, Tikhonov's regularization and sensitivity coefficients. The examples in the article concern the Lotka–Volterra model, the bistable switch model in genetic regulatory networks, gene regulation and repressilator models from synthetic biology. However, Capasso et al. [24] describes the application of Barnsley's Collage Theorem [27] to solve the inverse problem for the model described by first-order ordinary differential equations. In the examples, the following models are considered: population dynamics, mRNA and protein concentration, bacteria and amoeba cells interaction, and tumor growth. Models described by the system of ordinary differential equations are also considered by Kabanikhin and Krivorotko [25]. This time the solution was based on the gradient method. Numerical examples concerned models of infectious disease, HIV dynamics, and the spread of tuberculosis. In the inverse problem considered by Doumic et al. [26], the division rate from the cell volume distribution data in certain structured population models is reconstructed. The quasi-reversibility method and filtering method were used in the calculations. In paper [28] a novel 2-hydr_Ensemble residues' identification algorithm was proposed. Several typical classification models can be employed to compare. Presented algorithm has the ability to find out the potential information among several feature vectors. Paper [29] focuses on the application of a capsule network (CapsNet) to identify the pneumonia-related compounds in Qingre Jiedu injection. Obtained results show that CapsNet can identify disease-related compounds more accurately than other methods like SVM or RF. In the work [30], the authors propose and develop a tool called Phage_UniR_LGBM to classify the virion proteins.

In mathematical modeling, it is very important to properly determine the values of parameters in the model. Some of these parameters cannot be accurately determined on the basis of theory or direct measurements. In that case, we can try to measure a different quantity and then solve the inverse problem of identifying the value of the parameter we are interested in. Such an inverse problem is considered in this paper. Namely on the basis of the knowledge density of active bacteria at a given point the diffusion coefficient of active bacteria is determined. This paper considers a model describing the density distribution of *B. subtilis* as well as the concentration of the substrate. A model consisting of two non-linear partial differential equations is considered. The assumed symmetry consists of the fact that homogeneous boundary conditions of the second kind are given for both functions on the boundary of the area. Thus, there is no flow of bacteria or substrate through the

boundary of the area. As a consequence, the obtained solution to the direct problem can be symmetrically reflected with respect to the boundary of the region (analog to thermal symmetry). The finite element method was used to solve the direct problem. However, to determine the minimum of the functional, describing the error of the approximate solution, the Fibonacci search method was used. The inverse problem was solved for different noises of the input data.

2. Bacterial Colonies Model

In this section, a model of a bacterial colony is presented, which is describing the distribution of active bacteria in space and time and the concentration of the substrate (nutrient field). Both, bacteria cells and the nutrient, diffuse when bacteria cells multiply by consuming nutrients. We assume that the distribution of active bacteria and concentration of the substrate meets the conditions of symmetry. Therefore, it is possible to consider a fragment of the entire area with symmetry conditions set on the boundary. We consider region $\Omega = \{(x, y) : x \in (x_l, x_r), y \in (y_l, y_r)\}$ where $-\infty < x_l < x_r < \infty$ and $-\infty < y_l < y_r < \infty$ for time $t \in [0, t^*]$. By *b* we denote the density of active bacteria and by *s* concentration of substrate. Their distribution is described by the system of partial differential Equations [31]:

$$\frac{\partial b}{\partial t} = \nabla \left(D_b(b,s) \,\nabla b \right) - \nabla \left(\chi(s) \, b \,\nabla s \right) + g(s) \, b, \tag{1}$$

$$\frac{\partial s}{\partial t} = D_s \, \nabla^2 s - g(s) \, b, \tag{2}$$

where $D_b(b, s)$ is nonlinear diffusion for bacterial cells, $\chi(s)$ is chemotactic response, g(s) is function describing specific bacterial growth rate and D_s is constant diffusion coefficient for substrate. The first term of Equation (1) describes the motility, the second mortality and the third reproduction. Using the equations, it is possible to model different types of bacterial motility, such as swimming, sliding and swarming, as well as the motility of a single bacterium, in smaller clusters or larger agglomerates [5,8]. It is also possible to determine the conditions of secretion of substances by bacteria and the formation of various patterns, such as a ring pattern, resulting from cyclical changes in the differentiation of bacteria from swimming to swarming forms [8–10].

To the system of differential Equation (1) and (2) the initial conditions are posed:

$$b(x,y,0) = b_0(x,y), \qquad \text{for } (x,y) \in \Omega, \qquad (3)$$

$$s(x, y, 0) = v_0,$$
 for $(x, y) \in \Omega.$ (4)

Due to the assumed symmetry, on the boundary $\partial \Omega$ of the Ω , homogeneous boundary conditions of the second kind are set:

$$\frac{\partial b}{\partial n}(x,y,t) = 0, \qquad \text{for } (x,y) \in \partial\Omega, \ t \in [0,t^*], \tag{5}$$

$$\frac{\partial s}{\partial n}(x,y,t) = 0, \qquad \text{for } (x,y) \in \partial\Omega, \ t \in [0,t^*]. \tag{6}$$

In the presented model, we assume [31,32]:

$$D_h(b,s) = D\,b\,s,\tag{7}$$

$$g(s) = k \frac{s}{1+s},\tag{8}$$

$$\chi(s) = v \, s. \tag{9}$$

where *D* is linear diffusion coefficient for bacterial cells, *v* is chemotaxis coefficient and *k* is arbitrary constant. Taking into account (7)–(9), system of differential Equations (1) and (2) has following form:

$$\frac{\partial b}{\partial t} = D\left(\frac{\partial}{\partial x}\left(bs\frac{\partial b}{\partial x}\right) + \frac{\partial}{\partial y}\left(bs\frac{\partial b}{\partial y}\right)\right) - v\left(\frac{\partial}{\partial x}\left(bs\frac{\partial s}{\partial x}\right) + \frac{\partial}{\partial y}\left(bs\frac{\partial s}{\partial y}\right)\right) + k\frac{bs}{1+s}, \quad (10)$$

$$\frac{\partial s}{\partial t} = D_s \left(\frac{\partial^2 s}{\partial x^2} + \frac{\partial^2 s}{\partial y^2} \right) - k \frac{b s}{1+s}.$$
(11)

3. Inverse Problem and Its Solution

In this section, we consider the inverse problem which consists of reconstructing the value of diffusion coefficient *D*. Additional information which we used for the identification of the *D* coefficient is the values of the *b* function (density of active bacteria) in a given point in the Ω region. We denote this data by $\overline{b}(x_p, y_p, t_i)$, where $(x_p, y_p) \in \Omega$ are the coordinates of the measuring point, and t_i , i = 1, 2, ..., N, are measurement times. By solving the direct problem for a fixed value of the coefficient *D* (solving the system of Equations (1) and (2)), we obtain the values of the *b* function in the measuring point— $b_D(x_p, y_p, t_i)$. Next, by comparing the data obtained from the model for the given *D* coefficient $b_D(x_p, y_p, t_i)$ with the measurement data $\overline{b}(x_p, y_p, t_i)$, we create a function describing the error of approximate solution:

$$J(D) = \sum_{i=1}^{N} \left(b_D(x_p, y_p, t_i) - \overline{b}(x_p, y_p, t_i) \right)^2.$$
(12)

By minimizing the above objective function, we can identify the approximate value of the *D* coefficient.

In order to solve the direct problem, the finite element method supplemented with the method of lines was used. In the case of determining the minimum of the objective function, the Fibonacci search method [33,34] was used. Now, we present the algorithm of the Fibonacci search method.

1. Input: objective function *f* (unimodal function), interval [*a*, *b*],

required absolute precision ε .

- 2. Determine the smallest number $k \in \mathbb{N}$ for which $F_k > \frac{b-a}{\varepsilon}$, where F_k is the Fibonacci number.
- 3. Set $a^{(0)} = a$ and $b^{(0)} = b$.
- 4. Determine $x_1^{(0)} = b^{(0)} \frac{F_{k-1}}{F_k} \left(b^{(0)} a^{(0)} \right)$ and $x_2^{(0)} = a^{(0)} + b^{(0)} x_1^{(0)}$.
- 5. For $i = 0, 1, \dots, k 4$:

5a. If
$$f(x_1^{(i)}) < f(x_2^{(i)})$$
, then $a^{(i+1)} = a^{(i)}$ and $b^{(i+1)} = x_2^{(i)}$, otherwise $a^{(i+1)} = x_1^{(i)}$ and $b^{(i+1)} = b^{(i)}$.

5b. Determine

$$\begin{aligned} x_1^{(i+1)} &= b^{(i+1)} - \frac{F_{k-i-2}}{F_{k-i-1}} \left(b^{(i+1)} - a^{(i+1)} \right), \\ x_2^{(i+1)} &= a^{(i+1)} + b^{(i+1)} - x_1^{(i+1)}. \end{aligned}$$

6. Result $x_1^{(k-3)}$.

The designed algorithm was implemented in Wolfram language on Mathematica 12.3 platform [35] and the calculations were performed by using the computer with processor Intel Core i7-8565U, 1.80 Ghz, 2.00 GHz, equipped with 16 GB RAM memory.

The block diagram of the calculation procedure is shown in Figure 1. However, the implementation of the Fibonacci search method in Wolfram language [35] is shown in

Figure 2. In each step of the procedure for solving the inverse problem the values of the objective function should be determined in consecutive points x_1^i and x_2^i . This is related to the solution of the direct problem composed of Equations (10) and (11) with boundary conditions (3)–(6). Solving single direct problem took about 2.7 *s*, while solving inverse problem took about 130 s.

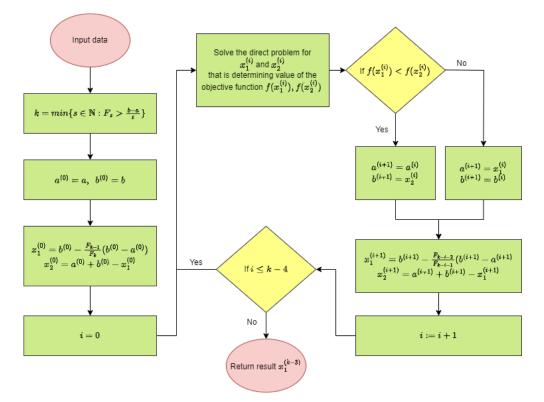


Figure 1. Block diagram of the procedure solving inverse problem.

```
In[1]:= Clear[fibonacciSearchMethod];
```

```
fibonacciSearchMethod[objFunction_, a_, b_, e_] := Module {ul, k, ak, bk, x1, x2, i, fx1, fx2},
  ul = (b - a) / e;
  k = 1;
  While[Fibonacci[k] ≤ ul, k++];
  ak = a; bk = b;
  x1 = bk - \frac{Fibonacci[k-1]}{m} (bk - ak);
             Fibonacci[k]
  x2 = ak + bk - x1;
  For i = 0, i \le k - 4, i + +,
   fx1 = objFunction[x1];
   fx2 = objFunction[x2];
   If[fx1 < fx2, bk = x2, ak = x1];</pre>
   x1 = bk - \frac{Fibonacci[k-i-2]}{Fibonacci[k-i-1]} (bk-ak);
   x2 = ak + bk - x1;;;
  Return[x1]
]
```

Figure 2. Implementation of the Fibonacci search method in Wolfram language.

4. Results

In the numerical experiment, input data for the inverse problem have been obtained by solving a direct problem. To prepare the input data, a mesh consisting of 986 finite elements

was used. In the calculations necessary to solve the inverse problem, a mesh composed of 602 finite elements was used. This mesh is presented in Figure 3. How changing the mesh affects the values of bacterial density *b* and substrate concentration *s* is presented in Figures 4 and 5. The error plot looks similar at two different points of the region. The reason for using a different mesh to generate the input data and a different mesh for solving the inverse problem is related to avoiding the inverse crime [20,21].

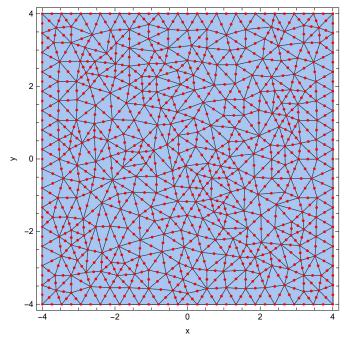


Figure 3. Division of the considered region into finite elements.

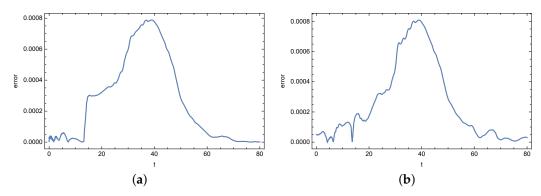


Figure 4. Error in determining the density of active bacteria *b* when changing the mesh: (**a**) in point (0.5, 0.5) and (**b**) in point (3, 3).

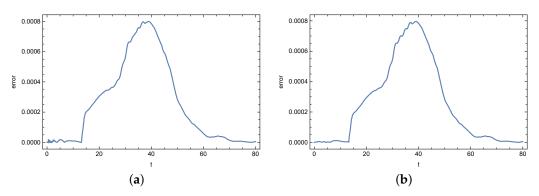


Figure 5. Error in determining the concentration of substrate *s* when changing the mesh: (**a**) in point (0.5, 0.5) and (**b**) in point (3, 3).

The calculations are performed in the region $\Omega = \{(x, y), x \in (-4, 4), y \in (-4, 4)\}$ and for $t \in [0, 80]$. Following parameters are assumed [31]: v = 2.0, $D_s = 1$, k = 0.1, $v_0 = 1.5$ and $b_0(x, y) = a_0 \exp\left(\frac{-x^2-y^2}{a}\right)$, where a = 6.25 and $a_0 = 0.5$. The exact value of the diffusion coefficient is D = 0.5. The contour plots of the *b* (density of active bacteria) and *s* (concentration of substrate) functions for t = 20 are shown in Figure 6.

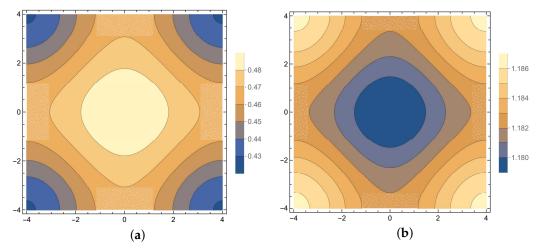


Figure 6. Density of active bacteria b (**a**) and concentration of substrate s (**b**) for t = 20 s.

Region Ω contains one measuring point, while the measurements are taken every 1 s. The calculations are taken for different positions of the measuring point: (0,0), (0.5,0.5), (4,0) and (4,4). The exact and noised input data are used in the calculations. The noise of input data was implemented in such a way that a random value from $\left[-\frac{p b_e}{100}, \frac{p b_e}{100}\right]$ was added to the exact value of b_e , where p was the percent disturbance level. The random values are uniformly distributed. Perturbations of 0.5%, 1%, 2%, 5% and 10% were used in the calculations. The exact input data and their noises are shown in Figure 7.

To find the minimum of the objective function J (12) the Fibonacci algorithm was used, which is described in Section 3. The diffusion coefficient D was searched in (0, 1] interval with a precision of 10^{-7} .

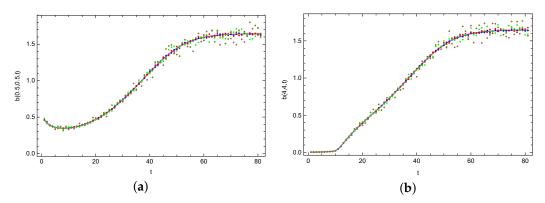


Figure 7. Exact (solid line) and noised values of input data for different measuring points: (0.5, 0.5) (a) and (4, 4) (b) (orange points—p = 0.5%, blue points—p = 1%, red points—p = 2%, green points—p = 5%, brown points—p = 10%).

Figures 8 and 9 present plots of the objective function *J* in the case of exact input data and 10% noised input data. As we can see in Figures 8 and 9, for small values (≤ 0.2) of the diffusion coefficient *D*, the values of the objective function *J* are relatively large. The minimum is for *D* = 0.5.

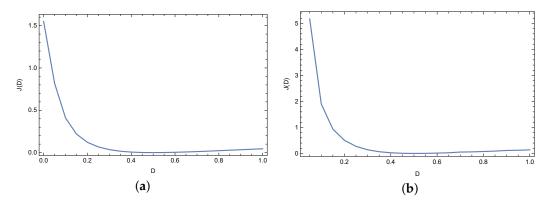


Figure 8. Objective function *J* for exact input data and for different measuring points: (0.5, 0.5) (a) and (4, 4) (b).

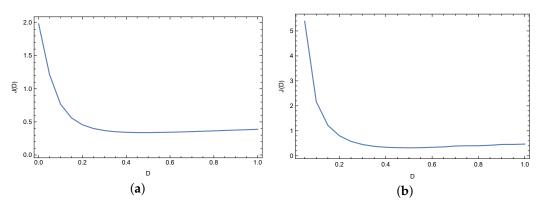


Figure 9. Objective function *J* for noised input data (p = 10%) and for different measuring points: (0.5, 0.5) (**a**) and (4, 4) (**b**).

In Tables 1 and 2 are presented reconstructed values of coefficient D in the case of calculations for measurement point (0.5, 0.5) and (4, 4). In the case of noised input data, the percentage error of reconstruction is smaller than the noisy input data. Even for p = 10%, the error of reconstruction is less than 3.7% which is satisfying. In the case of calculations for the remaining measuring points, the D coefficient is also reconstructed very well. Table 3 presents errors of reconstruction functions b (density of active bacteria) and s (concentration of substrate) in measurement point (0.5, 0.5). In all cases, these errors are minimal and do not exceed 0.13%. A similar situation occurs in the case of identification of the functions b and s in the entire region Ω (see Table 4). Even in case of 10% noised input data, relative errors of reconstruction b and s are equal to 8.86×10^{-2} % and 2.06%, respectively. In the case of calculations for the remaining measurement points, similar results were obtained. This is illustrated by Figure 10, which shows the mean errors of identifying the b and sfunctions obtained during the calculations for various measurement points and selected noises of the input data. Each time, the values of both functions in the measuring point are estimated very well. The identification errors are much smaller than the input errors. They slightly depend on the location of the measurement point. The *b* function reconstruction error is slightly greater than in the case of the *s* function. In the case of the *b* function, the biggest error occurred for the (0,0) measurement point and the 5% disturbance of the input data and this error is equal to 0.282%. On the other hand, in the case of the *s* function, the largest error occurred for the (4.0) measurement point and 10% disturbance and is equal to 0.076%. Plots of reconstructed density of active bacteria b and concentration of substrate s in measurement point (0.5, 0.5) and (4, 4) for input data noised by 10% error are presented in Figure 11.

	D _r	Δ_D	δ_D [%]	$J(D_r)$
0%	0.498745	$1.25463 imes 10^{-3}$	0.25093	$5.92104 imes 10^{-6}$
0.5%	0.501232	$1.23154 imes 10^{-3}$	0.24631	$9.76260 imes 10^{-4}$
1%	0.500935	$9.34980 imes 10^{-4}$	0.18700	$3.72183 imes 10^{-3}$
2%	0.492409	$7.59105 imes 10^{-3}$	1.51821	$1.80198 imes 10^{-2}$
5%	0.513011	$1.30115 imes 10^{-2}$	2.60229	$9.91133 imes 10^{-2}$
10%	0.481519	$1.84813 imes 10^{-2}$	3.69626	3.38221×10^{-1}

Table 1. Result of reconstruction diffusion coefficient *D* for measuring points (0.5, 0.5) (D_r —reconstructed value, Δ_D —absolute error, δ_D —percentage relative error, $J(D_r)$ —value of objective function).

Table 2. Result of reconstruction diffusion coefficient *D* for measuring points (4, 4) (D_r —reconstructed value, Δ_D —absolute error, δ_D —percentage relative error, $J(D_r)$ —value of objective function).

	D _r	Δ_D	δ _D [%]	$J(D_r)$
0%	0.500749	$7.49011 imes 10^{-4}$	0.14980	$3.64599 imes 10^{-5}$
0.5%	0.502123	$2.12259 imes 10^{-3}$	0.42452	$1.05587 imes 10^{-3}$
1%	0.495409	$4.59132 imes 10^{-3}$	0.91826	3.36342×10^{-3}
2%	0.493628	$6.37232 imes 10^{-3}$	1.27446	1.64222×10^{-2}
5%	0.502123	$2.12259 imes 10^{-3}$	0.42451	$9.19305 imes 10^{-2}$
10%	0.490746	$9.25410 imes 10^{-3}$	1.85082	$3.23392 imes 10^{-1}$

Table 3. Errors of reconstruction *b* and *s* in measurement point (0.5, 0.5) (Δ —absolute error, δ —percentage relative error).

	Δ_b	δ_b [%]	Δ_s	δ_s [%]
0%	1.77444×10^{-5}	$1.35385 imes 10^{-2}$	1.5003×10^{-5}	$1.63783 imes 10^{-2}$
0.5%	$1.55925 imes 10^{-5}$	$1.18967 imes 10^{-2}$	$1.32981 imes 10^{-5}$	$1.45171 imes 10^{-2}$
1%	$1.42339 imes 10^{-5}$	$1.08601 imes 10^{-2}$	$1.32816 imes 10^{-5}$	$1.44991 imes 10^{-2}$
2%	$6.99296 imes 10^{-5}$	$5.33545 imes 10^{-2}$	2.2793×10^{-5}	$2.48823 imes 10^{-2}$
5%	$1.09808 imes 10^{-4}$	$8.37807 imes 10^{-2}$	$1.47364 imes 10^{-5}$	$1.60872 imes 10^{-2}$
10%	$1.63983 imes 10^{-4}$	$1.25115 imes 10^{-1}$	$2.31277 imes 10^{-5}$	$2.52477 imes 10^{-2}$

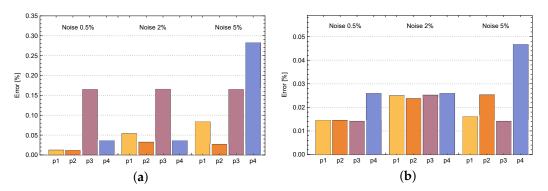


Figure 10. Mean relative errors of density of active bacteria *b* (**a**) and concentration of substrate *s* (**b**) for various measurement points: p1-(0.5, 0.5), p2-(4, 0), p3-(4, 4), p4-(0, 0).

	Δ_b	δ_b [%]	Δ_s	δ_s [%]
0%	$3.44446 imes 10^{-7}$	$2.14275 imes 10^{-2}$	$1.84832 imes 10^{-7}$	$1.62498 imes 10^{-2}$
0.5%	$2.76896 imes 10^{-7}$	1.72253×10^{-2}	$1.65205 imes 10^{-7}$	$1.45242 imes 10^{-2}$
1%	$2.70628 imes 10^{-7}$	$1.68353 imes 10^{-2}$	$1.64835 imes 10^{-7}$	$1.44917 imes 10^{-2}$
2%	$6.26896 imes 10^{-7}$	$3.89982 imes 10^{-2}$	$2.69966 imes 10^{-7}$	$2.37345 imes 10^{-2}$
5%	$9.48329 imes 10^{-7}$	$5.89941 imes 10^{-2}$	$1.56614 imes 10^{-7}$	$1.3769 imes 10^{-2}$
10%	$1.42314 imes 10^{-6}$	$8.85313 imes 10^{-2}$	$2.33235 imes 10^{-7}$	$2.05052 imes 10^{-2}$

Table 4. Errors of reconstruction *b* and *s* in entire region in the case of calculations for measurement point (0.5, 0.5) (Δ —absolute error, δ —percentage relative error).

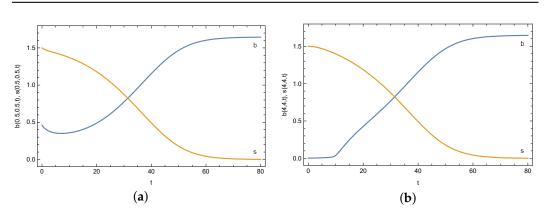


Figure 11. Density of active bacteria *b* and concentration of substrate *s* in measurement point reconstructed for noised input data (p = 10%) and for different measuring points: (0.5, 0.5) (**a**) and (4, 4) (**b**).

Figure 12 presents the mean relative errors of reconstructing the functions b and s in the entire considered area obtained during calculations for various measurement points and selected disturbances of the input data. Furthermore, the obtained errors for the entire area are much smaller than the input data errors. Changing the position of the measuring point has a small effect on the obtained errors. In all cases, errors are very small. In the case of the b function, the largest error is noted for (0,0) and 5% disturbances and it is equal to 0.185%. In turn, in the case of the s function, the largest error occurred for the point (4.0) and 10% disturbances and it is equal to to 0.077%.

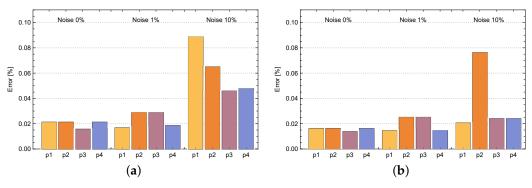


Figure 12. Mean relative errors of density of active bacteria *b* (**a**) and concentration of substrate *s* (**b**) in the entire area obtained during calculations for various measurement points: p1-(0.5, 0.5), p2-(4, 0), p3-(4, 4), p4-(0, 0).

At the end of this section, we present Figures 13-18 showing the errors of the reconstruction of functions *b* and *s* in measurement points for different noises of the input data. In the case of the density of active bacteria (function *b*) and low input data noise (p = 0%, 0.5%, 1%), the greatest errors are noted around the time t = 40 s, while for the input data noised by p = 2%, 5%, 10% the highest value of error is around t = 10 s. In the case of the concentration of substrate, the highest error is around t = 40 s for all input data.

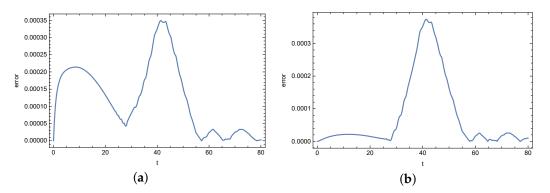


Figure 13. Absolute error of reconstruction functions b (**a**) and s (**b**) in measurement point (0.5, 0.5) for exact input data.

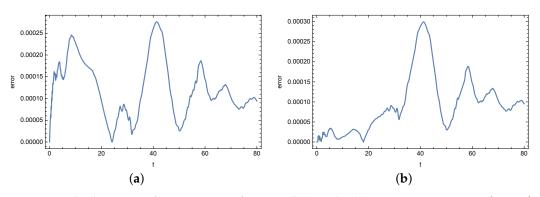


Figure 14. Absolute error of reconstruction functions *b* (**a**) and *s* (**b**) in measurement point (0.5, 0.5) for noised input data (p = 0.5%).

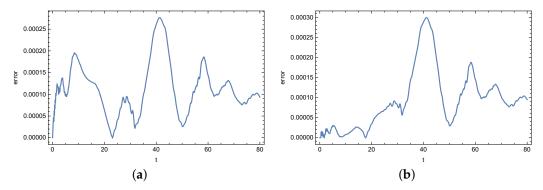


Figure 15. Absolute error of reconstruction functions *b* (**a**) and *s* (**b**) in measurement point (0.5, 0.5) for noised input data (p = 1%).

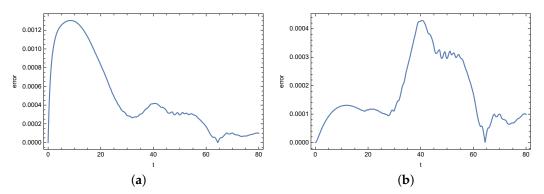


Figure 16. Absolute error of reconstruction functions *b* (**a**) and *s* (**b**) in measurement point (0.5, 0.5) for noised input data (p = 2%).

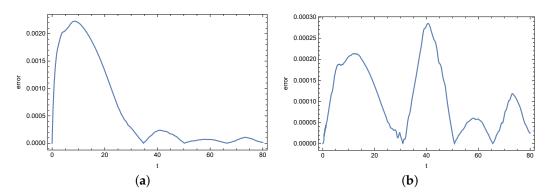


Figure 17. Absolute error of reconstruction functions *b* (**a**) and *s* (**b**) in measurement point (0.5, 0.5) for noised input data (p = 5%).

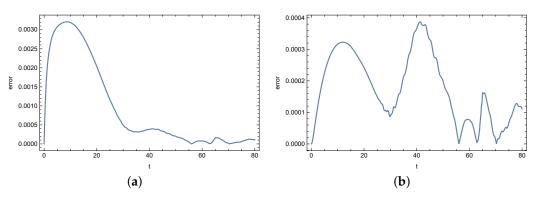


Figure 18. Absolute error of reconstruction functions *b* (**a**) and *s* (**b**) in measurement point (0.5, 0.5) for noised input data (p = 10%).

5. Conclusions

The model presented in the paper describes the distribution of active bacteria (function b) and the concentration of the substrate (function s) in space and time. For solving a system of differential equations with initial-boundary conditions, the finite element method was used. In modeling various types of phenomena, it is sometimes necessary to determine some model parameters that are difficult to measure by sensors. To determine these parameters is needed to solve the inverse problem. A method of solving the inverse problem, consisting in determining the diffusion coefficient of active bacteria based on measurements of the density of bacteria at a fixed point of the region, is presented. The considered method, based on the minimization of the objective function with the Fibonacci algorithm, gives good results. Even for noisy input data, the errors are at a satisfactory level. The errors of reconstruction of the b and s functions, in all cases, are less than 0.3%, while the error of diffusion coefficient D does not exceed the noise of input data.

Furthermore, changing the location of the measurement point does not have a large impact on the obtained results. The method was implemented in the Wolfram language, and the calculations were performed in the Mathematica 12.3 platform. The computation time for the inverse problem was about 130 s. This time can be shortened by using more advanced Wolfram statements or implementing it in another language. The obtained results confirm the accuracy and stability of the presented method.

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