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Abstract: Lung cancer is one of the serious malignant tumors with high morbidity and mortality due to the poor diagnosis and early metastasis. The developing nanotechnology provides novel concepts and research strategies for the lung cancer diagnosis by employing nanomaterials as diagnostic reagents to enhance diagnostic efficiency. This commentary introduces recent progress using nanoparticles for lung cancer diagnosis from two aspects of in vivo and in vitro detection. The challenges and future research perspectives are proposed at the end of the paper.

Keywords: nanomaterials; lung cancer diagnosis; imaging test; biomarker detection

1. Introduction

Environmental pollution and unhealthy living habits have caused a climbing morbidity of lung cancer. The rapid proliferation, early metastasis, low sensitivity, and poor specificity in early diagnosis cause the lung cancer the highest mortality rate among all cancers [1-3]. At present, many methods have been developed to diagnose lung cancers including sputum cytology, and pleural fluid cytology as well as the autofluorescence bronchoscopy (AFB), endoscopic ultrasound (EUS), endobronchial ultrasound (EBUS) and imageological examination, such as chest radiograph (CXR), computed tomography (CT) scan (computerized axial tomography (CAT) scan, low-dose helical CT scan) bone scans, positron emission tomography (PET) and magnetic resonance imaging (MRI) [4–9]. However, the detection of cancer biomarkers (such as specific proteins, nucleic acids, cells, and volatile organic compounds) in blood, urine, sputum, exhaled breath, and tissues are limited by the low detection sensitivity, poor specificity, complex operations, and low adsorptivity of gaseous molecules on solid substrates [10–13]. During the imageological examination, patients suffer from a heavy burden of cost and the risk of cumulative radiation [14]. Additionally, poor tissue penetration of ray and low specificity of photographic developer can cause false-negative results [15]. In clinical practice, X-ray chest imaging is a basic method to detect lung cancer without providing detailed images of inside information. Therefore, low dose computed tomography (LDCT) becomes a promising method for lung cancer screening with lower radiation and higher security [16-18]. These detection methods possess a bottleneck of an unsatisfactory sensitivity with sputum cytology of 66%, pleural fluid cytology of 70%, PET scan of 88%, CT scan of 55% and bone scan of 77% [19]. Therefore, it is essential to establish low-cost, sensitive, convenient, and non-invasive detection approaches for lung cancer diagnosis.

Nanomaterials have been widely applied in cancer diagnosis and treatment because of their excellent plasticity, controllable shapes and sizes, as well as adjustable thermal, magnetic, and optical properties [20–27]. The nanoparticles can be used as carriers to de-liver anti-cancer drugs (such as small molecule drugs, RNA, and protein) [28–30]. Moreover, they can function as direct diagnostic agents according to their inherent properties, such as the superparamagnetic properties of Fe_3O_4 nanoparticles [31], and the photoacoustic properties of melanin nanoparticles [32]. In addition to stabilizing drugs, functional nanoparticles can be obtained by surface modification, including specificity targeting,



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stimulus response, improving the detection sensitivity, and increasing the biocompatibility [14,31,33,34]. Moreover, a novel idea has been demonstrated to discriminate non-small cell lung cancer patients from healthy volunteers through exploiting the biomolecular corona that forms around nanoparticles to identify the differences of protein patterns between cancer patients and healthy subjects in blood [35]. Through the combination of nanotechnology and diagnostic targets, the novel diagnostic strategies with high efficiency and specificity have been developed, which are expected to improve the detection efficiency at an early stage and monitor the development trend and accurate therapeutics in the follow-up treatment of lung cancer [36].

In the past five years, the treatment of lung cancer by employing nanomaterials was reviewed [37–41], but the relationship between lung cancer diagnosis and nanomaterials still needs to be further summarized. In this commentary, we focus on the characteristics of some dominant nanomaterials, primary functions, and improvement strategies to commentate the progress in improving detection specificity, diagnosis accuracy and internalization efficiency, when using nanomaterials in the early-stage diagnosis of lung cancer from in vivo detection (imageological examination) and in vitro detection (biomarker detection). Besides, the current challenges and the future development prospects of nanomaterials in the diagnosis of lung cancer are also discussed.

2. Applications of Nanoparticles in Diagnosis of Cancer

The occurrence and progression of cancer are normally accompanied by a series of changes at the molecular or cellular level, which can in turn provide specific targets for effective diagnosis. Imageological examination and biomarker detection are common diagnose methods associated with the specific target in niduses.

2.1. In Vivo Examination

The in vivo methods mainly include AFB, EUS, CT, PET, MRI, which can reflect the disease information by visual image. The anatomical structure and boundary range of tumor can be seen clearly due to the ultrahigh resolution of MRI, but it was limited by longer imaging time and the lack of molecular imaging information. Although PET imaging showed high sensitivity and provided systemic lesions information, it is still limited by insufficient spatial resolution and possible false positive caused by unsatisfactory specificity. Low dose CT-scans provides information to indicate size, shape, and position of cancer cells in lymph nodes, but it has the disadvantages of low sensitivity and low specificity due to severe artifacts in pictures caused by internal organ motion and tattoos.

2.1.1. Single-Modal Imageological Examination-MRI

MRI is a high resolution and large-scale imaging technique facilitating the tumor observation of anatomical structures and subtle features. Nevertheless, MRI cannot yet be directly applied in the lung detection due to the motion artifacts, numerous susceptibility gradients, and low proton density [42]. By combining with the optimized proton MRI sequences based on ultrashort echo time (UTE), ultrashort echo-time magnetic resonance imaging (UTE-MRI) can be applied in lung tissue imaging [43]. Gadolinium is clinically used as the MRI contrast material, showing that non-invasive detection of non-small cell lung cancer by UTE-MRI can be achieved via the orotracheal administration of nebulized gadolinium nanoparticles with enhanced signal. Moreover, Gadolinium can be selectively deposited in tumor tissues while removed by healthy tissues [44].

Accurate and detailed detection information can be obtained through simultaneous usage of two MRI contrast agents [45–47]. MRI contrast agents can be divided into longitudinal relaxation contrast medium (T1 contrast medium, such as Gd-DTPA, Mn-DPDP) and transverse relaxation contrast medium (T2 contrast medium, such as superparamagnetic iron oxide), among which T1 contrast medium can effectively decrease the T1 relaxation time by the interactions with the neighboring T2 contrast medium [48]. The strong magnetic coupling between T1 and T2 contrast medium could disturb the relaxation effect of the paramagnetic T1 contrast medium, leading to an undesirable weakening and quenching of magnetic resonance signal [49]. According to this, a smart MRI contrast agent with Fe₃O₄ nanoparticles in core (T2 contrast medium) and the silica shell containing water-soluble Mn-porphyrin (T1 contrast medium) and anticancer drug DOX in shell was constructed (Figure 1a). After the modification by poly (acrylic acid) (PAA) and c(RGDyK) peptides (cRGD), the dual-mode MRI contrast medium was equipped with functions of tumor-specific target and pH response (Figure 1b). When the contrast medium was internalized by cancer cells, the tumor acidic microenvironment facilitated the release of porphyrin and recovered the quenched signal caused by the combination of Fe₃O₄ and Mn-porphyrin (Figure 1a) [31].



Figure 1. (a) Schematic illustration for the preparation, release, and imaging process of Fe₃O₄@SiO₂ @PAA-cRGD as dual-mode MRI contrast medium. Reprinted from [31] with permission by Creative Commons License. (b) UV–Vis spectra analysis of drug release: a pH-dependent drug release of DOX and Mn-porphyrin in the nanoparticles in different physiological environments Reprinted from [31] with permission by Creative Commons License. (c) Schematic illustration for the contrast agent preparation and imaging mode of MRI/PET/PAI multi-modal imaging. This contrast agent can internalize by tumor cell specifically due to the interaction between Oct and SSTR2 surface receptors highly expressed in tumor cells. Reproduction from Ref. [32] with permission from The Royal Society of Chemistry. (d) The gold nanoparticles that modified by various antibodies on the surface combine with microarray for detecting various biomarkers simultaneously. Reprinted from Ref. [50] with permission from Elsevier. (e) The gold nanoparticles were constituted into gold superparticles (GSPs) by self-assembly to amplify the detection signal. Reprinted from [51] with permission of Wiley.

2.1.2. Single-Modal Imageological Examination-PET

PET is a diagnosis imaging technology with high sensitivity, temporal resolution, systemic image quantitative analysis, and unlimited tissue penetration [52,53]. Radio isotope used in PET imaging possesses a short half-life with ¹¹C of 20 mins, ¹³N of 10 mins and ¹⁵O of 2 mins. ⁶⁴Cu was widely studied due to its half-life up to 12.7 h. Researchers found that polyglucose nanoparticles consisting of cross linked dextrans and their derivatives (dextran nanoparticles) had noteworthy affinity to tumor associated macrophages (TAMs) [54,55]. ⁶⁴Cu-labeled dextran nanoparticles by macrocyclic chelators can be applied in PET imaging for clinical oncologic diagnosis. However, the poor stability of radiometal-chelator complexes in vivo [56] greatly influenced the physicochemical properties of nanoparticles in PET imaging. Hence, the chelator-free ⁶⁴Cu nanoclusters were developed through a simple one-pot chemical reduction method by employing bovine serum albumin (BSA) as a framework for PET lung cancer detection to improve the stability and accumulation [57]. Although Cu-based radionuclide has been studied extensively and made some progress, the blemishes of its instability and higher accumulation in the liver are still the focus of lung diagnosis studies in the future.

2.1.3. Multi-Modal Imageological Examination

Compared to single-contrast medium imaging, multi-modal imaging with several contrast mediums can provide complementary imaging information for cancer diagnosis. Co-delivery of various contrast mediums without the imaging signal interference is a great challenge. USRPs-Cy5.5 was constructed by covalently conjugating cyanine 5.5 on nebulized gadolinium nanoparticles for fluorescence tomography and ultrashort echotime magnetic resonance imaging (UTE-MRI) to detect lung cancer non-invasively [58]. Melanin nanoparticles photoacoustic imaging (PAI) can be used as nanocarriers to codeliver ¹²⁴I (PET contrast agent) and Mn²⁺ (MRI contrast agent) by an electrophilic substitution reaction and a chelation reaction respectively, which is an ideal vector for tri-mode imaging (Figure 1c) to improve the efficiency of lung cancer diagnosis at an early stage effectively [32].

2.2. In Vitro Detection

Biomarker testing has been demonstrated as an effective method to analyze and diagnosis cancer, including proteins (carcinoembryonic antigen (CEA), cytokeratin 19 fragment antigen 21-1 (CYFRA21-1), neuron specific enolase (NSE), dickkopf-1 (DKK1), etc.), nucleic acids (DNA, RNA), cells (TAMs), and volatile organic compounds (aldehydes) [51,59–65]. The detection of biomarker allows for serial sampling by a non-invasive way, but unsatisfactory specificity ascribe the vast inter-tumor heterogeneity [66,67]. The use of nanoparticles can enhance the sensitivity and specificity prominently (Table 1).

Nanoparticles	Cancer Biomarkers	Limit of Detection (LOD)	Methods	Ref.
Gold nanoparticles	EGFR, CK, Nap	_	Fluorescence and surface enhanced Raman scattering	[68]
	CEA, CYFRA21-1, NSE, Dkk1	<1000 pg/mL	Co-detection method based on NPs and microarrays	[50]
	MiR-205		Localized surface plasmon resonance	[51]
	MUC1	8 cells/mL	Chronoamperometry	[33]
	Aldehydes	10 ppb	Surface enhanced Raman scattering	[69]
Quantum dots	CEA, CYFRA21-1, NSE	CEA: 190 pg/mL; CYFRA21-1: 970 pg/mL; NSE: 370 pg/mL	Microarray immunoassay (bead bases sandwich assay)	[70]
	CYFRA21-1	0.3 pg/mL	Electrochemiluminescent immunoassay	[71]

Table 1. Nanoparticles for lung cancer biomarker detection.

Nanoparticles	Cancer Biomarkers	Limit of Detection (LOD)	Methods	Ref.
	HER2	_	Western Blot, ELISA, confocal microscopy, flow cytometry	[72]
Carbon nanomaterials	CEA/EGFR	14 cells/mL	Differential pulse voltammetry	[73]
Liposome	TKTL1, TTF1	_	TIRF and TLN biochip	[15]
Fe0 nanomaterials	ctDNA	0.1 pg/mL	Inductively coupled plasma mass spectrometry	[62]
Fluorescent nanoparticles	EGFR		Western Blot, confocal microscopy, flow cytometry	[14]
Fe ₃ O ₄ /Au/Ag nanocomposites	Adenosine		Surface enhanced Raman scattering	[74]

Table 1. Cont.

2.2.1. Gold Nanoparticles

Gold nanoparticles have been extensively used for cancer biomarker detection owing to the surface plasmon resonance (SPR) effect, controllable particle volume and size, and excellent biocompatibility. SPR effect was used to generate and magnify the detection signal. The mucin 1 (MUC1) specific aptamer [75,76] was covalently conjugated with gold nanoparticles through the self-assembly of 4-([2,2':5',2"-terthiophen]-3'-yl) benzoic acid (TTBA). This ultrasensitive cytosensing can prominently amplify the selective detection signal of lung cancer with the detection limit of 8 cells/mL [33]. In order to control the detection process, an enzyme was added to trigger the detection. The gold nanoparticles were linked with dual-functional Raman active luciferin by a peptide linker, and the peptide linker was engineered with a cathepsin B enzyme (CathB) cleavage site. Assisted by these antibodies (epidermal growth factor receptor (EGFR), cytokeratin-19 (CK), and napsin-A (Nap)) and CathB enzyme in vivo, the nanoprobes are endowed with multi-target to lung cancer and enzyme-driven fluorescence imaging [68]. The gold nanocubes can be used to test infinitesimal lung cancer biomarker miR-205 after modified by thiolated single strand DNA (ssDNA), which can realize real-time monitoring of the slight LSPR scattering peak displacement caused by the hybridization process of target miRNA with ssDNA [51]. In order to improve the detection sensitivity, two nanoparticles were combined for the detection of circulating tumor DNA (ctDNA). The amorphous Fe⁰ nanomaterials are featured with excellent magnetic performances and high monodispersity, which allows the separation and enrichment of the subtle ctDNA, and the Au nanoparticles enables the prominent amplifying detection signal. Taking the detection of Kirsten rat sarcoma-2 virus (KRAS) mutation as an example, 0.1 pg/mL gene mutation can be detected by Fe–Au nanoparticle, which refers to the stage I diagnosis. This method avoided the test deviation caused by the amplification of traditional PCR [62].

Assisted with microarray technology, gold nanoparticles conjugated to detection antibodies on microarrays can further enhance the amplifying detection signal through immersing in a solution of HAuCl₄ and H₂O₂, which can be used to detect four kinds of markers (CEA, CYFRA21-1, NSE, DKK1) at the same time (Figure 1d) [50]. The gold nanoparticles can constitute gold superparticles (GSPs) through self-assembly to amplify the Raman signal (Figure 1e) [51]. Despite their ultrahigh sensitivity for lung cancer noninvasive diagnosis in vitro, the potential toxicity of nanoparticles needs to be addressed [69].

2.2.2. Quantum Dots (QDs)

QDs were often used to establish electrochemical luminescence (ECL) sensor due to its high fluorescence intensity, unique size-dependent electrochemical properties, long fluorescence lifetime, strong photostability, and ECL parameter tenability [77–80]. The detection limit based on QDs (0.3 pg/mL) was much lower than that of other detection

method (0.65 pg/mL) [71]. A suspension and planar microarray system can be set up based on the low cost and high throughput detection of multiple markers (CEA, CYFRA21-1, NSE). Briefly, the suspension state was ground on the target proteins to constitute a sandwich structure between the magnetic beads and the QDs through specific antibody–antigen interactions [70]. Inherently, the modification of lung cancer-specific antibody on the surface of QDs can realize the target detection theoretically. Undesirable issues came up for practical applications, such as decreasing the detection sensitivity for intracellular tumor biomarker due to the larger complexes formed between QDs and antibody as well as the inactivity of the lung cancer-specific antibody engineered on the QDs surface. Fortunately, the traditional antibody can be substituted by the single domain antibody (sdAb), which can reduce the molecular weight prominently [72,81,82]. Although the surface modification of QDs can be used to improve biocompatibility to alleviate the biological toxicity to cells, the security and targeting specificity are still major obstacles that QDs face [83].

2.2.3. Carbon Nanomaterials

Carbon nanomaterials are potential candidates for constructing electrochemical biosensors due to the large surface area, chemical, and thermal stabilities, excellent electrical and thermal conductivity, extraordinary electron transport rate, tunable band gap, and great mechanical strength [59,84,85]. Graphene oxide and ordered mesoporous carbon can be deposited onto nano-carrier surface by two-step electropolymerization to improve electrical conductivity and electrochemical effective surface area [86]. An electrochemical cytosensor based on 3D carbon nanosphere was prepared through a microwave-hydrothermal method, and then gold nanoparticles were self-assembled on its surface to detect CEA, showing that the detection sensitivity was significantly improved and detection limit decreased to 14 cells/mL, due to the promotion of electron transfer caused by the synergism of monodisperse colloidal carbon nanospheres and gold nanoparticles [73]. Single-wall carbon nanotubes decorated by platinum-group transition metals were prepared as biosensors to enhance the detection of toluene, which was a biomarker of the lung cancer in the patients exhaled breath, and the effective detection contributed to the strong overlapping between d orbital of the metal atoms and p orbital of C atoms in the benzene ring of toluene [87].

2.2.4. Others

Additionally, there are some other nanomaterials that have been studied and applied to detect lung cancer biomarker. The lipid bilayer is composed of phospholipids and cholesterol, which is similar to the cell membrane [59,88–94]. Hence liposomes have higher biosafety and biocompatibility compared to other synthetic materials [95]. As the vehicles of transketolase 1 (TKTL1) and thyroid transcription factor 1 (TTF1), liposomes can capture circulating extracellular vesicles by electrostatic interaction to constitute a larger nanoscale compound and detect RNA concentration in the plasma of lung cancer patients [15]. The Fe₃O₄/Au/Ag nanocomposites and fluorescent nanoparticles have also been used in early diagnosis due to the magnetism assisted surface enhanced Raman scattering (SERS) effect of Fe₃O₄/Au/Ag nanocomposites, the advantages of highly efficient red emission, high resolution, and excellent photostability of fluorescent nanoparticles [14,74].

3. Cellular Uptake of Nanomaterials

Understanding the lung cancer cells internalization pathway of nanomaterials is essential to realizing the detection of lung cancer, particularly in vivo detection. Cellular uptake is a dynamic process which is determined to a great extent by physicochemical property of nanomaterials, such as size, shape, surface charge, hydrophilia/hydrophobicity, and the specific ligand [96–98]. According to the characteristics of size and shape, several common pathways for uptake mainly include phagocytosis, clathrin mediated endocytosis, receptor-mediated endocytosis, caveolae-dependent endocytosis, and membrane permeation. High specificity, low systematic side effects, and escaping from the capture of reticuloendothelial system permit pulmonary delivery to be widely used in pulmonary disease treatment, as well as in lung cancer diagnosis. The inhalant 5 μ m in diameter can effectively deposit in the lungs, because the mission of phagocytosis is to transmit larger particles greater than 200 nm [96,99]. The nanoparticles of ~100 nm in diameter were commonly used as tumor agents (diagnosis or imaging) and carriers because of their enhanced permeability and retention (EPR) effect in systemic delivery system. These nanoparticles internalized not only through clathrin mediated endocytosis [100], but also through receptor-mediated endocytosis after modified by lung cancer specific ligand [101]. Cellular uptake of nanoparticles about 50 nm was via caveolae-dependent endocytosis, but these particles were not suitable for lung cancer detection due to the cumulation in liver and kidney. The 2D morphology allowed nanomaterials to enter cells and bypass the lysosome by a membrane permeation, such as black phosphorus nanosheets and 2D graphene sheet [102]. In addition, nanoparticles with moderate positive charge can easily enter cells with negative charge with the assist of electrostatic interaction, which can also contribute to intracellular escape [103,104].

4. Conclusions

The challenges in application of nanomaterials for diagnosing lung cancer have been widely summarized. Although various nanoparticles have been demonstrated for detecting lung cancer and have already made significant progress in increasing detection limit, sensitivity, simplifying the detection operations, and shortening the detection time, it still needs to break through the limitations from the specificity and biosafety, detection efficiency, diagnostic cost, and patient tolerance. Nanomaterials are expected to contribute to overcoming the above challenges through increasing the internalization of diagnostic reagent into lung cancer cells instead of normal cells, or specifically binding to lung cancer biomarkers in vitro, due to the controllable sizes, shapes, physicochemical property (such as thermal, magnetic, and optical properties), and the characteristics of modifiable surfaces. Meanwhile, the combination of nanotechnology, array technology, and chip technology is a good option to surmount the barriers of inefficiency and high expenditure in lung cancer detection. The improvement of non-invasive detection methods should be paid more attention, aiming to increase the detection efficiency without additional harm. In the future, the combination of clinical diagnostic and biomedicine, nanotechnology, and material science will contribute to overcoming the current challenges in lung cancer early diagnosis.

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