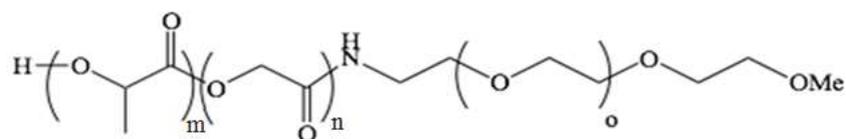


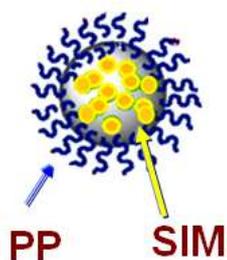


Supporting information



PP: PLGA-PEG copolymer

(a)



(b1)



(b2)

Figure S1. The methoxy-functionalized diblock copolymer of PLGA-PEG-methoxy (PP) was synthesized by conjugating the heterofunctional PEG with a terminal amine and carboxylic acid functional group to PLGA-COOH using standard *N,N'*-dicyclohexylcarbodiimide (DCC)-mediated chemistry (a). The simvastatin (SIM) agent was encapsulated in PLGA-PEG-methoxy nanoparticles to form SIM-PP NPs by the precipitation-solvent evaporation technique (b1,b2).

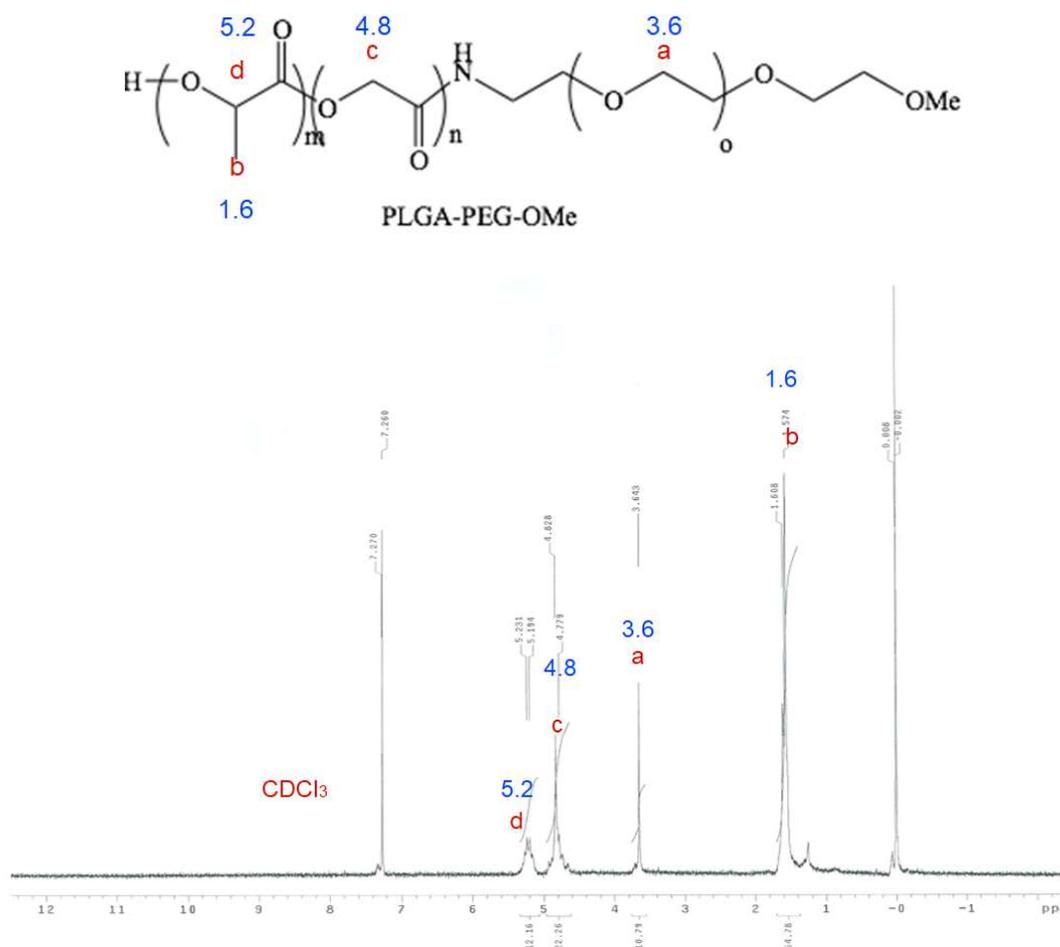


Figure S2. ^1H NMR spectrum confirms to the PLGA-PEG-OMe structure. ^1H NMR (CDCl_3 , 200 MHz) d: δ 5.219(m, 11H), c: δ 4.667-4.817(m, 22H), b: δ 3.641(s,1H), a: δ 1.562(m,33H).

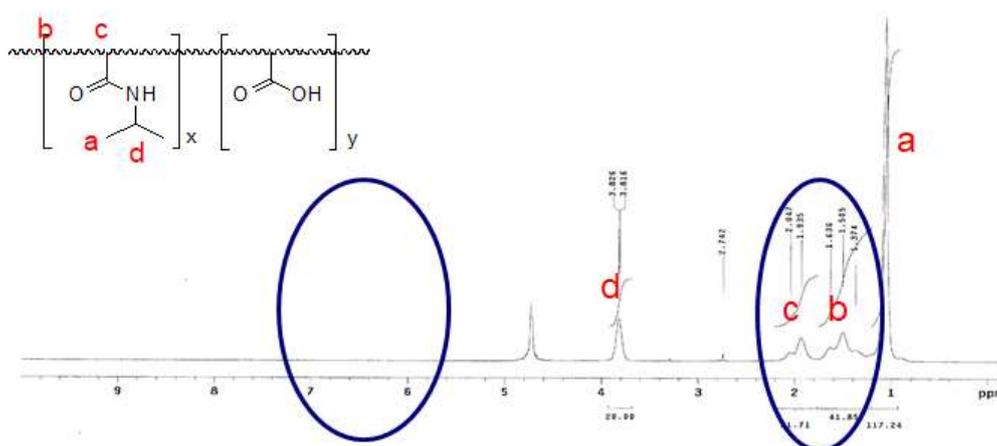


Figure S3. ^1H spectrum of p(NiPAAm-co-MAA) = 97:3 (PNM97:3) copolymer were examined by NMR.

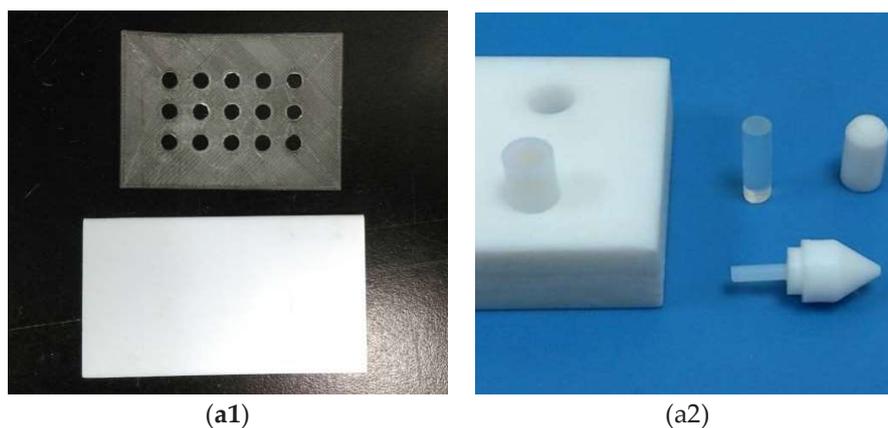


Figure S4. Two types of plastic molds for forming biphasic (hydroxyapatite and β -calcium phosphates) porous bone substitutes: a disk mold (**a1**, ϕ 5 mm; h 0.7 mm) and hollow cylinder mold (**a2**, ϕ_1 3.5 mm; ϕ_2 1.5 mm; h 10 mm).

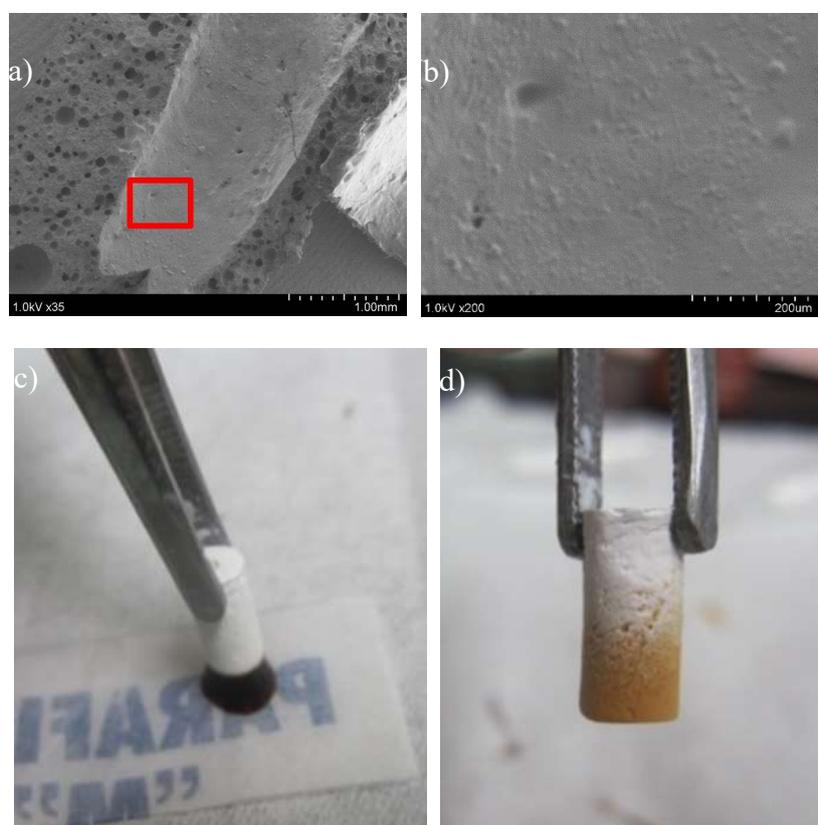


Figure S5. The SEM morphology of the SIM-PP NPs loaded within porous bioceramic of hollow cylinder after sintering at 1200 °C for 2h (**a,b**). The porous bioceramic of hollow cylinder absorb red ink to rise photos by liquid permeability test (**c,d**).

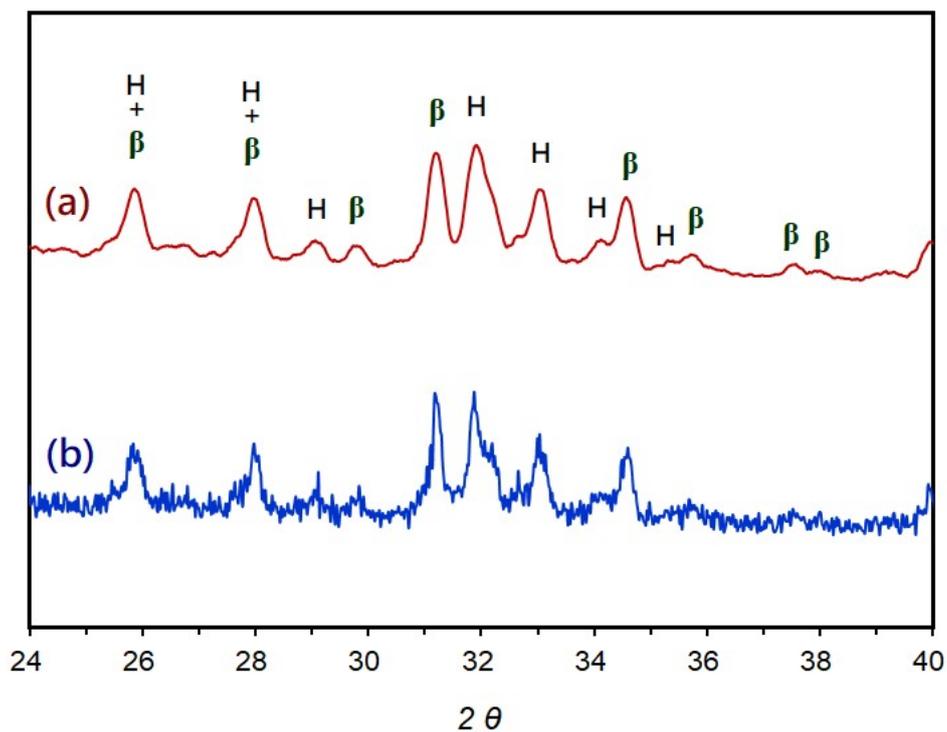
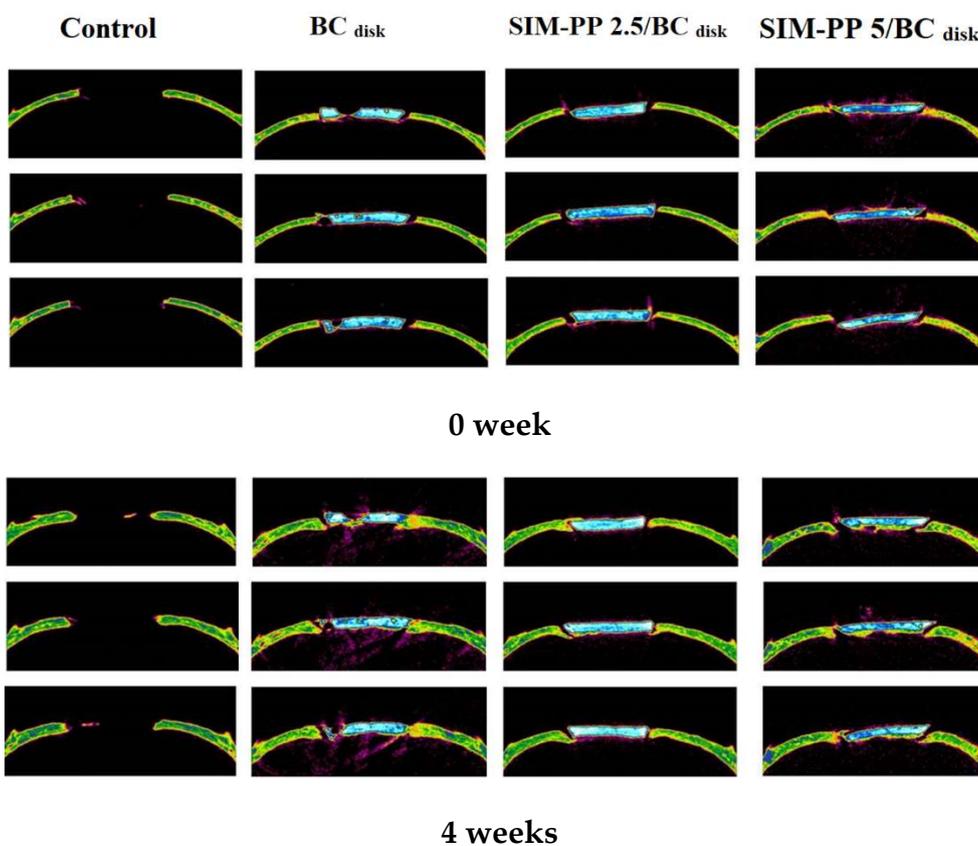
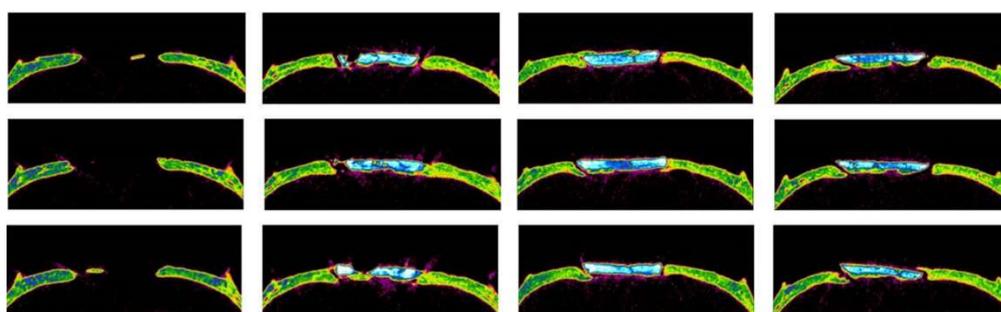


Figure S6. XRD patterns of the porous HAp/β-TCP (50/50) bioceramics after 1200 °C sintered for 2 h (a), commercial raw materials of HAp/β-TCP (b). (β = β-TCP, H = HAp).





8 weeks



Figure S7. Cross-section slices of calvarial bone from the Hounsfield unit [HU] calibration of micro-CT images for the rat model at 8 weeks after implantation of BC_{disk} samples (ϕ 5 mm; h 0.7 mm), 2.5 μ mol of SIM in SIM-PP/BC_{disk} samples and 5.0 μ mol of SIM in SIM-PP/BC_{disk} samples. Notes: calvarial bone defects only were used as controls and the rat number is tree).