



Article Laser-Induced Motion of a Nanofluid in a Micro-Channel

Tran X. Phuoc *, Mehrdad Massoudi and Ping Wang

National Energy Technology Laboratory, U.S. Department of Energy, P.O. Box 10940, Pittsburgh, PA 15236, USA; mehrdad.massoudi@netl.doe.gov (M.M.); ping.wang@netl.doe.gov (P.W.)

* Correspondence: tran@netl.doe.gov; Tel.: +1-412-386-6024

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Abstract: Since a photon carries both energy and momentum, when it interacts with a particle, photon-particle energy and momentum transfer occur, resulting in mechanical forces acting on the particle. In this paper we report our theoretical study on the use of a laser beam to manipulate and control the flow of nanofluids in a micro-channel. We calculate the velocity induced by a laser beam for TiO₂, Fe₂O₃, Al₂O₃ MgO, and SiO₂ nanoparticles with water as the base fluid. The particle diameter is 50 nm and the laser beam is a 4 W continuous beam of 6 nm diameter and 532 nm wavelength. The results indicate that, as the particle moves, a significant volume of the surrounding water (up to about 8 particle diameters away from the particle surface) is disturbed and dragged along with the moving particle. The results also show the effect of the particle refractive index on the particle velocity and the induced volume flow rate. The velocity and the volume flowrate induced by the TiO₂ nanoparticle (refractive index *n* = 2.82) are about 0.552 mm/s and 9.86 fL, respectively, while those induced by SiO₂ (*n* = 1.46) are only about 7.569 µm/s and 0.135, respectively.

Keywords: nanofluid; microchannel; photon pressure; laser power

1. Introduction

Micro-channels are devices that are used to transport, process, and manipulate extremely small volumes of fluids ranging from 10^{-15} m³ to 10^{-6} m³. Such devices have been found to be of significant importance in a variety of technologies such as cooling of electronic chips, inkjet printers, drug delivery, biomedical diagnostics, and biochemical processing, etc.

Generally, transporting fluids (or nanofluids) in micro-sized devices is achieved by a pumping mechanism that can be generated either by an external mechanical pumping system or non-mechanical pumping techniques using electro-osmosis [1–3], electrophoresis [4], electromagnetics [5], electrowetting [6,7], etc. There are some drawbacks associated with the use of a conventional mechanical pump because it has many components that are typically large relative to the small dimensions of microchannels. Although micropumps that are able to provide sufficient pumping power are available, the small size of the moving parts makes them difficult to fabricate and maintain. Non-mechanical pumping techniques have many disadvantages. For example, a device that utilizes electro-osmosis needs to be electronically reconfigured in order to maintain an electric field of about 30 KV/m; this is high enough to electrolyze the water base generating hydrogen peroxide, hydrogen ions (acid) and hydroxide (base) as well as oxygen and hydrogen gas bubbles. The hydrogen peroxide and/or pH changes generated can adversely affect biological cells and biomolecules such as proteins, while the generated gas bubbles tend to "clog" the microfluidic systems.

In this paper, we explore the use of a laser beam to manipulate and control the flow of nanofluids in micro-scaled devices. The concept is based on the fact that, when a nanofluid is irradiated by a laser beam, if the fluid base is transparent to the laser beam, interactions between the laser beam and the suspended nanoparticles via reflection, transmission, and absorption occur. Since the laser beam carries both energy and momentum, such interactions create (mechanical) forces acting on the suspended particles. If the particles are absorptive, they are heated and temperature gradients on their surfaces prevail. The surrounding gas molecules are heated unevenly and rebound off the particles at different velocities, resulting in a force called photophoretic force acting on the particles. If the particles are non-absorptive, the momentum transfer during refraction and reflection of the photon become dominant. In this case, the resulting force is called the pressure force which is composed of two components: the gradient component acts transversely and the scattering (axial) component acts in the direction of the laser propagation. Thus, the particles will be pulled into the higher intensity region of the beam in the transverse direction by the gradient component of the force, and they will be simultaneously pushed along in the direction of the beam propagation by the scattering component. As the particles move they disturb and drag the surrounding fluid with them. As a result, a flow field, as shown in Figure 1, is generated.



Figure 1. Representation of the streamlines and the x-component velocity, v_x (velocity along with the direction of the particle motion) for flow of the surrounding fluid due to the moving particle, r, θ , are the spherical coordinates of the surrounding fluid described by Equations (13) and (14), U: particle velocity, x: particle flow direction, R: radius of the flow channel relative to the centerline.

Use of a laser beam to induce and manipulate the motion of micron/nano-size particles has been reported previously [8–16]. In these studies, laser-induced motion of transparent particles such as glass, silica, Poly(methyl methacrylate) (PMMA), polystyrene, nickel and aluminum oxides particles in water using a loosely focused Gaussian beam were investigated. The effects of various parameters including numerical aperture, focal length, laser power, particle size, refractive index, and medium velocity on the parting distance, and the number of particles separated per unit time were studied. Phuoc et al. [16] also reported a study on the laser-induced motion and the travel distances of some rare earth and mineral oxides that are commonly found in coal ashes. Their results indicated that, under laser action, these oxide particles were moving in the direction of the laser propagation and finally dropped out of the laser beam into two small areas that were several millimeters apart. The rare earth oxides were seen to concentrate in the area near the beam waist while the mineral oxides were mainly concentrated in the area further away from the beam waist.

In order to demonstrate that the flow of a nanofluid in a micro-channel can be controlled by a laser beam, we present some preliminary results on the particle velocity and its impact on the surrounding fluid in terms of its velocity and the flowrate. The calculations are carried out for five typical nanoparticles (TiO₂, Fe₂O₃, Al₂O₃·MgO, and SiO₂) with water as the liquid medium. We use these typical particles because they are commonly used as the solid component in many nanofluids.

2. Forces Acting on a Single Particle

Tchen [17] synthesizes the work of Basset, Boussinesq, Stokes, and Oseen on the motion of a sphere settling under the force of gravity in a fluid at rest. The resulting force balance, sometimes known as the Basset-Boussinesq-Oseen (BBO) equation, is given by:

$$\frac{4\pi a^3}{3}\rho_s \dot{u} = -\frac{2\pi a^3}{3}\rho_f \dot{u} - 6\pi\mu_f a u -6\pi\mu_f a \frac{a}{\sqrt{\pi\nu_f}} \int_{-\infty}^t \frac{\dot{u}(t_1)}{\sqrt{t-t_1}} dt_1 - \frac{4\pi a^3}{3}g(\rho_s - \rho_f),$$
(1)

where *u* is the velocity of the particle, ρ_f and ρ_s are density of the fluid and particle, respectively, *a* is the particle radius, *g* is the acceleration of gravity, μ_f and ν_f are viscosity and kinematic viscosity of the fluid, respectively. The terms on the right-hand side of the above equation are related to the virtual mass effects, Stokes drag, Basset history effects, and buoyancy. Maxey and Riley [18], proposed a generalization of the above equation for the forces acting on a sphere in a nonuniform flow:

$$m_{s} \frac{\mathrm{d}u_{i}}{\mathrm{d}t} = (m_{s} - m_{f})g_{i} + m_{f} \frac{\mathrm{D}v_{i}}{\mathrm{D}t}\Big|_{\mathbf{Y}(t)} \\ - \frac{1}{2}m_{f} \frac{\mathrm{d}}{\mathrm{d}t} \{u_{i}(t) - v_{i}[\mathbf{Y}(t), t] - \frac{1}{10}a^{2}\nabla^{2}v_{i}\Big|\mathbf{Y}(t)\} \\ - 6\pi a\mu_{f} \{u_{i}(t) - v_{i}[\mathbf{Y}(t), t] - \frac{1}{6}a^{2}\nabla^{2}v_{i}\Big|\mathbf{Y}(t)\} \\ + 6\pi a^{2}\mu_{f} \int_{0}^{t} \mathrm{d}\tau \frac{\left(\frac{\mathrm{d}}{\mathrm{d}\tau} \{u_{i}(\tau) - v_{i}[\mathbf{Y}(\tau), \tau] - \frac{1}{6}a^{2}\nabla^{2}v_{i}\Big|\mathbf{Y}(\tau)\}\right)}{\sqrt{\pi}v_{f}(t - \tau)}$$
(2)

The terms involving $\nabla^2 v_i$ correspond to the physical effect known as the Faxen forces. Although Equation (2) appears to be complete for a single particle in Stokes flow, there are, in general, other forces that must be considered (even for a purely mechanical system). For example, the spin of the particle is not taken into account in the above equations (see Massoudi [19,20]).

Briefly, the linear momentum equation for a single particle, using the vector notation is:

$$\rho \frac{\mathrm{d}u}{\mathrm{d}t} = \rho b + F_E \tag{3}$$

where ρ is the density, *u* is the velocity vector, *b* the body force, and *F*_E. represent the various forces acting on the particle which can include the terms on the right hand side of Equation (2) and also forces due to the electric current, magnetic field interactions (see Kim et al. [21]), and the radiation due to the laser, etc. In this paper, we ignore all the forces except that due to the laser. In the next section we discuss this force.

3. Forces Due to the Laser

Here we consider the interaction between a CW Gaussian beam and a nanofluid (See Figure 2). The laser beam is slightly focused with a beam waist $2w_o$ at the focal point located at x = 0. Its wavelength λ is very long compared to the suspended particle size and it is chosen so that the fluid base with the refractive index n_f is transparent to it. The suspended nanoparticle of radius a is considered to be non-absorptive relative to the laser wavelength and it is located at a position r = (x, y, z) relative to the beam waist center. The particle refractive index is n_p . Since the particle is non-absorptive, the momentum transfer during refraction and reflection of the photon becomes dominant. In this case, the resulting forces are the scattering force, F_{sctr} , and the force due to the gradient of intensity, often called the gradient force. The scattering force acts in the direction of the photon propagation. In contrast, the gradient force has, in a Cartesian coordinate system, three components: two transverse

components ($F_{grad,y}$, and $F_{grad,z}$) which act to restore the particle to the beam center and a longitudinal component, $F_{grad,x}$ which acts against the scattering force to pull the particle toward the beam waist. Since the size of the nano-particle is very small compared to the wavelength of the laser beam, these forces are in the Rayleigh scattering regime and they are given as [22,23]:

The scattering force

$$F_{sctr} = \frac{8\pi n_f k^4 a^6}{3c} \left(\frac{m^2 - 1}{m^2 + 2}\right)^2 \frac{2P_o}{\pi w_o^2 \left[1 + (2\bar{x})^2\right]} \exp\left[-\frac{2\left(\bar{z}^2 + \bar{y}^2\right)}{1 + (2\bar{x})^2}\right]$$
(4)

The gradient force components

$$F_{grad,x} = -\frac{2\pi n_f a^3}{c} \left(\frac{m^2 - 1}{m^2 + 2}\right) \left(\frac{8\bar{x}/kw_o^2}{1 + (2\bar{x})^2}\right) \\ \left[1 - \frac{2(\bar{z}^2 + \bar{y}^2)}{1 + (2\bar{x})^2}\right] \left(\frac{P_o}{\pi w_o^2}\right) \left(\frac{1}{1 + (2\bar{x})^2}\right) \exp\left[-\frac{2(\bar{z}^2 + \bar{y}^2)}{1 + (2\bar{x})^2}\right]$$
(5)

$$F_{grad,y} = -\frac{2\pi n_f a^3}{c} \left(\frac{m^2 - 1}{m^2 + 2}\right) \left(\frac{4\bar{y}/w_o}{1 + (2\bar{x})^2}\right) \left(\frac{P_o}{\pi w_o^2}\right) \left(\frac{1}{1 + (2\bar{x})^2}\right) \exp\left[-\frac{2\left(\bar{z}^2 + \bar{y}^2\right)}{1 + (2\bar{x})^2}\right]$$
(6)

$$F_{grad,z} = -\frac{2\pi n_f a^3}{c} \left(\frac{m^2 - 1}{m^2 + 2}\right) \left(\frac{4\bar{z}/w_o}{1 + (2\bar{x})^2}\right) \left(\frac{P_o}{\pi w_o^2}\right) \left(\frac{1}{1 + (2\bar{x})^2}\right) \exp\left[-\frac{2\left(\bar{z}^2 + \bar{y}^2\right)}{1 + (2\bar{x})^2}\right]$$
(7)

where $k = 2\pi/\lambda$ is the wave number, λ is the beam wavelength, c is the beam speed, *a* is the particle radius, $m = n_p/n_f$ is the particle relative refractive index, P_o is the beam power, w_o is the beam waist, $\overline{x} = x/kw_o^2$, $\overrightarrow{y} = y/w_o$, and $\overline{z} = z/w_o$ are the dimensionless coordinates. If the focal region of the beam is assumed to be cylindrical in shape, the focal spot size, in terms of the beam waist w_o is given as

$$w_o = \frac{2\lambda}{\pi} \frac{f}{d} \tag{8}$$

From the system of forces given above, we can see that the particles having m > 1 at any location of the beam center will be quickly attracted to the beam center due to the transvers components $F_{grad,y}$ and $F_{grad,z}$ where they are pushed along the direction of the beam propagation or pulled back to the beam waist depending on the magnitudes of the scattering force and the longitudinal component of the gradient force. The magnitudes of these forces depend significantly on the particle size, as shown in Figure 3.



Figure 2. Representation of the interaction between a Gaussian continuous laser beam and a nanofluid in a micro-channel. The laser beam is slightly focused using a focusing lens, w_0 is half of the beam waist which is at the channel entrance (x = 0), a is the particle radius, r is the location of the particle relative to center of the beam waist.



Figure 3. Scattering force, F_{sctr} and the longitudinal component of the gradient force $F_{grad,x}$ as a function of the dimensionless \overline{x} acting on a particle in water located on the beam center ($\overline{y} = \overline{x} = 0$), $n_p = 1.592$, $n_f = 1.332$, $P_o = 100$ mW, lens focal length f = 75 mm, beam diameter D = 4 mm, wavelength $\lambda = 532$ nm.

In Figure 3 the radiation forces acting on a particle located at the beam center are presented. Since the particle is at the beam center, the force components $F_{grad,y}$ and $F_{grad,z}$ are zero and the remaining non-zero forces are the longitudinal component of the force due to the gradient of intensity, $F_{grad,x}$ and the scattering force, F_{scat} . The longitudinal component $F_{grad,x}$ is acting toward the beam waist, and its magnitude increases negatively from zero at the beam waist to a maximum value at $\overline{x} = 0.288$ ($x = kw_o^2/2\sqrt{3}$) away from the beam waist. The scattering force is acting along the direction of the propagation of the laser beam. Its magnitude has a maximum value at the beam waist and decreases rapidly as the particle location moves in the direction of the laser propagation. For the particle sizes shown here, the longitudinal component of the gradient force is significantly larger than the scattering force for the particle size of \leq 5 nm and it becomes less significant for the particle sizes larger than 10 nm. Thus, smaller particles are pulled back to the beam waist and the larger particles are pushed along the laser beam. Therefore, in order to induce the flow of a nanofluid in a micro-channel by a laser beam, the nanofluid must contain nanoparticles whose sizes are determined by the ratio of the scattering force *F_{sctr}* to the maximum backward longitudinal component of the gradient force. For a Gaussian beam of wavelength λ , a focal spot size w_0 , the maximum longitudinal component of the gradient force occurs at y = z = 0 and $x = kw_0^2/2\sqrt{3}$ where this ratio becomes

$$R = \frac{F_{sctr}}{\left|F_{grad,xmax}\right|} = \frac{256\pi^5}{3\sqrt{3}} \left(\frac{m^2 - 1}{m^2 + 2}\right) \frac{a^3 w_o^2}{\lambda^5}$$
(9)

If R > 1, the magnitude of F_{sctr} is greater than that of $F_{grad,x}$. Thus, the required particle size to move in the direction of the laser propagation is

$$a > \left\{ \frac{\lambda^5}{15075.95w_o^2} \left(\frac{m^2 + 2}{m^2 - 1} \right) \right\}^{1/3}$$
(10)

Under the action of the laser beam, if the particle size satisfies condition (12), the particle will move in the direction of the laser propagation against the surrounding fluid. If we assume that the resisting force by the fluid on the moving particle is described by the Stokes law, then the particle velocity can be calculated using

$$U = \frac{F_{sctr} + F_{grad,x}}{6\pi a\mu_f} \tag{11}$$

As the particle moves, the fluid surrounding it begins to move, with the streamlines represented in Figure 1 and the motion is given by [24] using the spherical coordinate system

$$\psi = Ur^2 \sin^2 \theta \left(\frac{3}{4}\frac{a}{r} - \frac{a^3}{4r^3}\right) \tag{12}$$

where ψ is the stream function. The corresponding velocity components of such a flow (Stokes flow) are given by

$$u_{f,\theta} = -\frac{1}{r\sin\theta} \frac{\partial \psi}{\partial r} = -U\sin\theta \left(\frac{3}{4}\frac{a}{r} + \frac{a^3}{4r^3}\right)$$
(13)

$$u_{f,r} = \frac{1}{r^2 \sin\theta} \frac{\partial \psi}{\partial \theta} = 2U \cos\theta \left(\frac{3}{4} \frac{a}{r} - \frac{a^3}{4r^3}\right) \tag{14}$$

It is clear that the induced flow due to a moving particle can extend to a large distance away from the particle where the flow velocity approaches zero. As a result, for many general flow situations such as flow in pipes and channels, and where many particles are present, the motion can be modified significantly.

4. Results

We have carried out calculations for five typical nanoparticle materials. The fluid base is water with a refractive index of $n_f = 1.332$ and viscosity $\mu_f = 0.98 \times 10^{-3}$ kg/m-s. The particle velocity is calculated using Equation (11) with F_{sctr} and $F_{grad,x}$ given by Equations (4) and (5), respectively. Referring to Figure 1, the velocity profile of the surrounding water, v_x (in the direction of the particle motion), across the flow field is calculated from the velocity field described by Equations (13) and (14). The flowrate due to the motion of the particle is $\dot{Q} = 2\pi \int_0^R R v_x dR$ where $R = a \tan \theta$. We use the Simpson's 1/3 rule to calculate its value from $\theta = 0$ to θ where $v_x \to 0$. Typical results for the axial forces, the particles velocities, and the flowrate are shown in Table 1.

Table 1. Typical axial forces, particle velocities, and volume flowrate transported by nanoparticles under laser action, ($P_o = 4$ W, focal length = 75 mm, beam diameter d = 6 mm, $\lambda = 532$ nm, refractive index of water $n_f = 1.332$, water viscosity $\mu_f = 0.98 \times 10^{-3} \text{ kg/m}^{-s}$, a = 50 nm, the particle is at the beam waist, v_p : particle velocity, $v_{f,ave}$: fluid average velocity, Q: fluid volume flowrate).

Particle	Refractive Index	$F_x(\mathbf{pN})$	v_p (mm/s)	Q(fl/s)	v _{f,ave} (mm/s)
TiO ₂	2.82	0.4628	0.55182	9.86	0.009
Fe ₂ O ₃	1.986	0.1345	0.16039	2.867	0.0028
Al_2O_3	1.773	0.0671	0.08006	1.431	0.0014
MgO	1.73	0.0557	0.06637	1.186	0.0015
SiO ₂	1.46	0.00635	0.007569	0.135	0.00013

Velocity profiles for flow of water induced by the motion of TiO_2 nanoparticle, Fe_2O_3 nanoparticle, and SiO_2 nanoparticle are shown in Figure 4.



Figure 4. Velocity profiles in axial plane of the flow of water induced by the moving particle ($P_o = 4$ W, focal length = 75 mm, beam diameter d = 6 mm, $\lambda = 532$ nm, nm ($w_o = 4.2375 \mu$ m, Equation (8)), refractive index of water $n_f = 1.332$, water viscosity $\mu_f = 0.98 \times 10^{-3}$ kg/m-s, a = 50 nm, the particle is at the beam waist).

It is clear that, as the particle moves, a significant portion of the surrounding water is disturbed and dragged along with the moving particle. On the particle surface, the velocity of the water is equal to that of the moving particle (no-slip condition) and it decreases quickly to zero at a distance of about 8 particle diameters away from the particle surface. The results reported here indicate the significant effect of the particle refractive index on the radiation force and the particle velocity. For example, with the laser power and the optical configuration used in this work, the velocity and the flowrate induced by TiO₂ nanoparticle, (refractive index n = 2.82), are about 0.552 mm/s and 9.86 fL, respectively, while those of SiO₂ (n = 1.46) are only about 7.569 µm/s and 0.135, respectively. Thus, using a laser beam to activate the flow of a nanofluid in a microchannel is more effective if the fluid contains high refractive index nanoparticles.

We have also performed a parametric study showing the effects of the laser conditions and particle size on the flowrate and the average velocity induced by the motion of TiO₂, Fe₂O₃, Al₂O₂, and MgO nanoparticles; these are shown in Figures 5 and 6, respectively. With the typical conditions used here, the results show that a volume up to 4×10^{-11} L/s could be transported which depends significantly on the laser power, the particle size, and the beam waist. The effects of these parameters on the fluid average velocity can be seen in Figure 6. To consider the electroosmotic effect on the velocities Sinton and Li [25] and Sinton et al. [26] showed that velocities increased in a linear fashion in 100 µm and 200 µm diameter circular channels and in 100 µm and 50 µm width square channels from about 0.2 mm/s when the external applied field was 5 kV/m; whereas the velocity was 1.2 mm/s when the external applied field was 20 kV/m. A similar velocity range is also obtained in our present calculations for TiO₂ and Fe₂O₃ particles. For example, for a 5 W laser power the fluid average velocity increases up to about 2.1 mm/s with a 150 nm particle while for the same laser power with a 1 µm beam waist, the velocity is about 5 mm/s for a 100 nm particle. However, for Al₂O₃ and MgO particles, due to their low refractive indexes, the average velocity up to 0.5 mm/s is calculated.



Figure 5. Effects of the laser power, P_o , beam waist, W_o , and particle size on the fluid volume flowrate (focal length = 75 mm, beam diameter d = 6 mm, $\lambda = 532$ nm, nm ($w_o = 4.2375 \ \mu$ m, Equation (8)), refractive index of water $n_f = 1.332$, water viscosity $\mu_f = 0.98 \times 10^{-3} \text{ kg/m-s}$, the particle is at the beam waist).



Figure 6. Effects of the laser power, P_o , beam waist, W_o , and particle size on the fluid average velocity (focal length = 75 mm, beam diameter d = 6 mm, $\lambda = 532 \text{ nm}$ ($w_o = 4.2375 \text{ µm}$, Equation (8)), refractive index of water $n_f = 1.332$, water viscosity $\mu_f = 0.98 \times 10^{-3} \text{ kg/m-s}$, the particle is at the beam waist).

The parametric calculations presented here indicate that the particle refractive index, size, the laser power, and the laser beam waist are the important parameters that can be used to induce and control the flow in microchannels. Use of either high laser power or large particles for delivering high volume of fluid, however, is not of practical interest, since the high laser power can cause significant particle heating which, in turn, can vaporize or alter the integrity of the surrounding fluid. Most conventional nanofluids contain nanoparticles with sizes of 50 nm or less, and using larger particles will lead to other problems associated with the stability of the nanofluid. Thus, we can see that the remaining parameter that can be of practical importance is the beam waist. A beam delivery optics system can be designed to deliver the laser beam via a network of micro-sized fiber optics. In this case, even with a micro watts laser beam, the laser intensity at the output end of the fiber optics will be sufficient for many practical applications.

5. Conclusions

Our simple calculations presented here show that, under the action of a laser, a nanoparticle suspended in a fluid will move and drag a sizable volume of the fluid with it in the direction of the laser propagation. Thus, using a laser beam to manipulate the flow of a nanofluid in a microchannel is possible and it has many advantages over other conventional methods. Such advantages are deduced from the fact that there are no moving parts and no external pumps, which are required, and that there is no need to electronically reconfigure the channel. Additionally, using a fiberoptic cable, the laser beam can be distributed and delivered to multiple micro-channels which can be operated either

sequentially or simultaneously. The location of the beam waist can be varied and thus the flow can be initiated at different locations throughout the micro-channel.

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