

Review

## Isothermal Microcalorimetry to Investigate Non Specific Interactions in Biophysical Chemistry

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**Abstract:** Isothermal titration microcalorimetry (ITC) is mostly used to investigate the thermodynamics of “*specific*” *host-guest interactions* in biology as well as in supramolecular chemistry. The aim of this review is to demonstrate that ITC can also provide useful information about non-specific interactions, like electrostatic or hydrophobic interactions. More attention will be given in the use of ITC to investigate polyelectrolyte-polyelectrolyte (in particular DNA-polycation), polyelectrolyte-protein as well as protein-lipid interactions. We will emphasize that in most cases these “non specific” interactions, as their definition will indicate, are favoured or even driven by an increase in the entropy of the system. The origin of this entropy increase will be discussed for some particular systems. We will also show that in many cases entropy-enthalpy compensation phenomena occur.

**Keywords:** non-specific interactions; isothermal titration calorimetry

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## 1. Introduction: Specific Versus Non-specific Interactions, What Is the Best Criterion?

One of the fundamental challenge in biophysical chemistry, as well as in all physicochemical events implying a solvent, is to attribute the contribution of different non-covalent interactions (electrostatic in the most general sense, solvation and hydrophobic interactions, hydrogen bonding, Van der Waals interactions) to the free energy change of a given molecule upon its interaction with a binding partner. This is also of prime interest in pharmacology, where the design of drugs aimed at binding to a given target relies on engineering contributions that will increase the absolute enthalpy change upon binding as well as contributions that will increase the entropy change [1]. Another challenge is to investigate how conformational changes in the tridimensional structure of a protein, DNA or RNA can modify the interaction between this molecule and its binding partner [2]. This last point is directly related to the problem of cooperativity [3] which also emerges in supramolecular chemistry. This is not surprising because both biological molecules and synthetic supramolecules interact via the same interplay of “non-covalent” interactions [4]. Finally, the most important challenge is to relate structure (the high resolution X-ray or NMR structure of more and more proteins and nucleotides are available) to the “binding affinity” of these molecules with their binding partners. This means that the “binding affinities” have to be accurately measured for as many as possible systems to get a clear picture of structure-energy relationships, which is particularly important for the design of new drugs or the design of gene vectors.

In this review, on purpose, we wish to not use the general terms of “host” and “guest” because these definitions point immediately to a key and lock interaction mechanism and hence to “specificity” (we will recall the definition of this concept later). In the next lines we will discuss a definition of “specific” and “non-specific” interactions, with the aim of reviewing the major contributions of microcalorimetry (in particular isothermal titration microcalorimetry, ITC) in the investigation of the thermodynamics of “non-specific” interactions.

Let us recall that when a transformation takes place in conditions of constant temperature and pressure, the chemical potential of use is the free energy. Its change between the initial and the final state is given by:

$$\Delta G^{\circ} = \Delta H^{\circ} - T \cdot \Delta S^{\circ} \quad (1)$$

where  $\Delta H^{\circ}$  and  $\Delta S^{\circ}$  are the change in the enthalpy and entropy of the system under standard conditions (symbolised by the superscript  $\circ$ ). The standard conditions refer just to the fact that the experiment is performed at a “standard” pressure of 1 bar and that the activity of each constituent is equal to 1. The same equation (1) is valid in non standard conditions. Equation (1) shows that a given “binding affinity” and hence a given value of  $\Delta G$  can be obtained with different contributions of enthalpy and entropy changes. The affinity is indeed the change in free energy with its sign changed. Hence a high affinity means an important decrease in the free energy upon binding. Anyway, the condition for a spontaneous evolution of a system is that:  $\Delta G^{\circ} < 0$ . It has to be noted that most of the metabolic transformations proceed in conditions of non spontaneity ( $\Delta G_1^{\circ} > 0$ ) because they are coupled with at least one transformation which occurs spontaneously [5] ( $\Delta G_2^{\circ} < 0$ ) with the constraint that:

$$\Delta G_1^\circ + \Delta G_2^\circ < 0 \quad (2)$$

The free energy change upon binding is experimentally accessible (provided the interaction is an equilibrium process!) via the measurement of the macroscopic equilibrium constant  $K$ , according to the well known relationship:

$$\Delta G^\circ = -RT \cdot \ln K \quad (3)$$

where  $R$  is the gas constant ( $8.314 \text{ J} \cdot \text{mol}^{-1} \cdot \text{K}^{-1}$ ) and  $T$  the absolute temperature in Kelvin.

This means that every experimental method able to determine the binding constant of the investigated transformation will give access to the free energy change associated with this transformation. Basically if the transformation follows the chemical equation:



the global free energy change will be given by the difference in the chemical potential (the molar Gibbs free energy) between the product ( $C$ ) and the reactants ( $A$  and  $B$ ):

$$\Delta G = \mu_C - \mu_A - \mu_B \quad (5)$$

When the energy changes are only of chemical nature, i.e., in the absence of applied external fields, using the relationship between the chemical potential and the activity, equation (5) becomes:

$$\Delta G = \mu_C^\circ - \mu_A^\circ - \mu_B^\circ + RT \cdot \ln \left( \frac{a_C}{a_A \cdot a_B} \right) \quad (6)$$

The difference in the standard chemical potential (defined at 1 bar and at an activity of 1), may be written as:

$$\Delta G^\circ = \mu_C^\circ - \mu_A^\circ - \mu_B^\circ \quad (7)$$

which finally gives:

$$\Delta G = \Delta G^\circ + RT \cdot \ln \left( \frac{a_C}{a_A \cdot a_B} \right) \quad (8)$$

The equilibrium conditions correspond to  $\Delta G = 0$ , which gives equation (3). The equilibrium constant  $K$  of equilibrium (4) being then defined as:

$$K = \frac{a_C}{a_A \cdot a_B} \quad (9)$$

We spent some time to derive such a trivial equation as (9) to show that the equilibrium constant is defined from the *activities* of the species taking part to the equilibrium and not from the concentrations. For solutes of low molecular mass, this is not of major concern because the activity becomes equal to the concentration at infinite dilution (hence practically for small concentrations, typically in the millimolar range). But this does not necessarily hold true any more in the case of macromolecules, like proteins or DNA, because the volume fraction of these macromolecules can be high even at low molar concentration.

The distinction between “specific” and “non-specific” interactions explains the somewhat provocative title of this article. As we will see, it is difficult to put a clear frontier between what is

called “specific” and “non-specific”, even if the term “specific” would refer to an interaction that is unique to a couple of binding partners, i.e. to the selectivity of the binding process. In most cases, as we will see, the situation is not as simple. The distinction between these two words is as difficult as the distinction between “interactions of physical” and “interactions of chemical nature”. Similarly, in surface science it is difficult to distinguish between specific and non-specific adsorption [6]. Indeed when one considers the interactions between amino acids and surfaces, the adsorption can have a specific counterpart even when the adsorption is performed in the gas phase [7]. The contribution of specific interactions has been demonstrated for the adsorption of glycine on titania [8]. There are many examples in which the specific adsorption of surface potential determining ions modify the surface potential of surfaces, the most well known example being that of silver iodide in presence of surface potential determining ions like I<sup>-</sup> [9]. The accumulation of counterions (i.e. of opposite sign to that of the permanent charges at the interfaces) in the electrical diffuse double layer may then be considered as “non-specific”. The condensation of counterions around strongly charged polyelectrolytes may at first glance be considered as non-specific because it originates from the strong electrostatic potential of the polyelectrolyte [10]. By condensation we mean that the counter ions are bound within a few tenths of a nanometer from the polyelectrolyte backbone. The occurrence of ion condensation on polyelectrolytes or on surfaces is the result of a competition between attractive electrostatic forces and the disrupting effect of thermal motion. The strong potential on certain polyelectrolytes originates from the chemical nature of the polyelectrolyte and can hence be considered as a “specific” effect that is due to the nature and the density of the charged groups carried by the polyelectrolyte.

In addition, the nature of the electrolyte can afford some specificity [11], the so called Hofmeister effect. These effects cannot be described simply by considering the electrolyte solution as a continuous medium of dielectric constant  $\epsilon$  where the screening of the electrostatic forces is just described by a macroscopic adjustable parameter, the ionic strength of the solution.

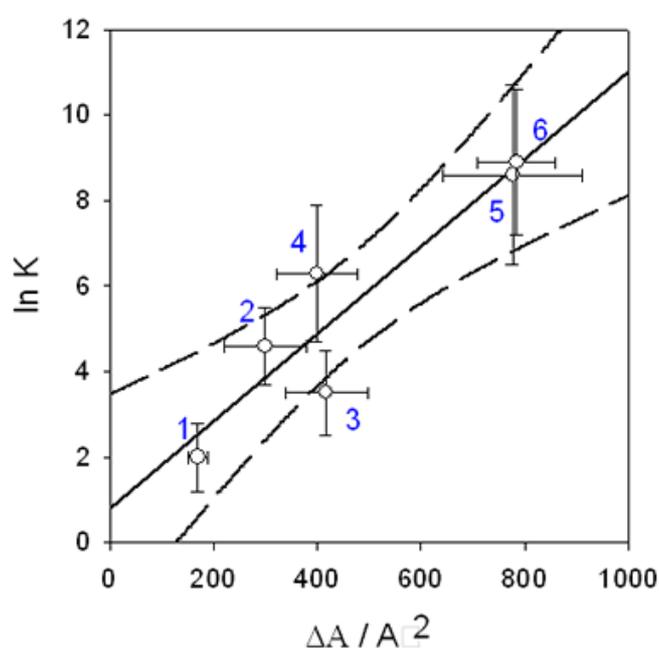
When considering interactions in supramolecular chemistry (implying cyclodextrins, or a plethora of synthetic hosts) as well as in biology (antigen-antibody complexes, protein-ligand binding and enzyme substrates complexes), which are all considered as highly “specific” interactions, it has been found out that the free energy change associated with the binding process is proportional to the solvent accessible surface area that is buried upon binding, Figure 1. These investigations have been performed by means of molecular docking [12] and analysis of crystal structures [13].

Despite the great diversity of binding partners, the correlation between  $\ln K$  (and hence the change in free energy) and the area buried from the solvent upon binding is pretty good ( $r^2=0.86$ ). Does that mean that the most important part of the interaction is related to the area that can be buried upon binding, and hence to the size of the “binding sites”? Or does it mean that the probability to have a contribution to the free energy decrease, be it “specific” or “non-specific” is proportional to the area of the part of the molecule that is implied in the molecular recognition process?

All the above examples show that the distinction between “specific” and “non-specific” effects are never clear cut. One can define an upper limit in the binding energy to distinguish “specific” from “non-specific”: this would imply that specificity is equivalent to “high affinity”. For free energy changes greater than a critical value one can define the interaction to have a “specific character” whereas for changes in free energy lower than this threshold, one assumes the interaction to be “non-specific”. It is exactly on this basis that one traditionally separates chemisorption from physical

adsorption and more generally “covalent bonds” from secondary interactions. Here again this clear separation may be arbitrary, because there are covalent bonds (established through the fact that the bond can be described by a molecular orbital constructed from atomic orbitals belonging to atoms of the molecule) implying a binding energy (the energy variation between isolated and bond atoms in the gas phase) that is very close to the above mentioned threshold. For instance the binding energy of  $\text{Li}_2$  amounts only to  $60 \text{ kJ}\cdot\text{mol}^{-1}$  [14]. However, this compound is not an aggregate of two Li atoms: The motions of both Li atoms are strongly correlated inside the molecule.

**Figure 1.** Relationship between the logarithm of the binding constant and the reduction in surface area accessible to the solvent upon binding between two partner molecules. This plot is based on the data in Table 7 of Houk *et al.* [12].



- 1: interactions between  $\alpha$ -cyclodextrins and organic guests.
- 2: interactions between catalytic antibodies and organic substrates.
- 3: interactions between albumins and organic guests.
- 4: interactions between catalytic antibodies and inhibitors.
- 5: interactions between enzymes and inhibitors.
- 6: interactions between antibodies and proteins.

The straight line is a linear regression to the data ( $r^2=0.86$ ) whereas the dashed line corresponds to the limit of the 95 % confidence interval.

When considering adsorption phenomena, it is clear that the contribution of many weak interactions (each one being of the order of  $kT$ , i.e. the average energy due to random collisions with solvent molecules) can lead to an irreversible adsorption, i.e. to high affinity, as in the case of chemisorption. Such assumptions, which become validated by experimental observations [15] and simulations [16] allow one to explain the irreversible character of protein or polymer adsorption at solid–liquid interfaces. This example clearly shows that high affinity can be reached without “specificity”. The previous example of  $\text{Li}_2$  shows that “specificity” can be reached even in the absence of high affinity. Clearly, the criterion of affinity is not satisfactory to separate “specific” from “non-specific”

interactions neither is the concept of a given stoichiometry. Many so called “non-specific” binding processes have nevertheless a defined stoichiometry. Indeed adsorption phenomena or ion binding events at surfaces often reach a saturation, but in the common sense most of them are “non-specific” (proteins stick everywhere, counterions can interact with every surface of opposite sign). At saturation of an adsorption process, there is clearly a maximal amount of bound molecules or ions (the sorbent) for a given number of surface sites (indeed it is often very difficult to have access to the density of surface sites particularly if the sorbate is heterogeneous, the situation becomes ideal only in the case of very clean monocrystalline terraces) and hence a given stoichiometry. The fact that in some adsorption experiments one not reaches the saturation value does not mean that there is no stoichiometry, it can simply mean that the sorbate is not provided in sufficient amount to cover all the adsorption sites. It has to be noted also that the notion of a 1 to 1 interaction between a sorbate and a site on the surface is a relative notion which depends on the size and the shape of the sorbate. This consideration is at the origin of improvements of the original Langmuir adsorption isotherm in which the surface exclusion function is simply considered to be proportional to the number of adsorbed molecules and hence neglects interactions between triplets and other kinds of multiplets (in a 2D crystal each adsorbed molecule can have up to 6 closest neighbours) [17].

If neither the criterion of a maximal change in free energy, nor the absence of a saturation in binding can be used to distinguish between “specific” and “non-specific” binding, what can be a reasonable criterion? Let us come back to E. Fisher’s “key and lock” analogy which is the foundation of the idea of specificity. In a “chemical lock” it is neither the geometry alone nor the presence of some given chemical functions which allows this lock to recognize some molecules with some preference with respect to other ones, *it is indeed a combination of both*. The “good” chemical groups have to be present in a given well defined but nevertheless flexible topology. Hence one can say that “specificity” corresponds to a pattern of molecular recognition (Figure 2).

There is an other important point: *Most often the affinity of “non-specific” processes is mainly due to an increase in entropy, whatever its origin* [1]. Hence many processes implying hydrophobic interactions are mainly “non-specific” in nature. Let us recall that the hydrophobic interaction between two aliphatic chains is not due to some preferential interactions between these chains nor to a repulsion between each of them and water, *it is due mainly to an entropy increase of the water molecules upon desolvation of the chains*. This desolvation of course costs some enthalpy.

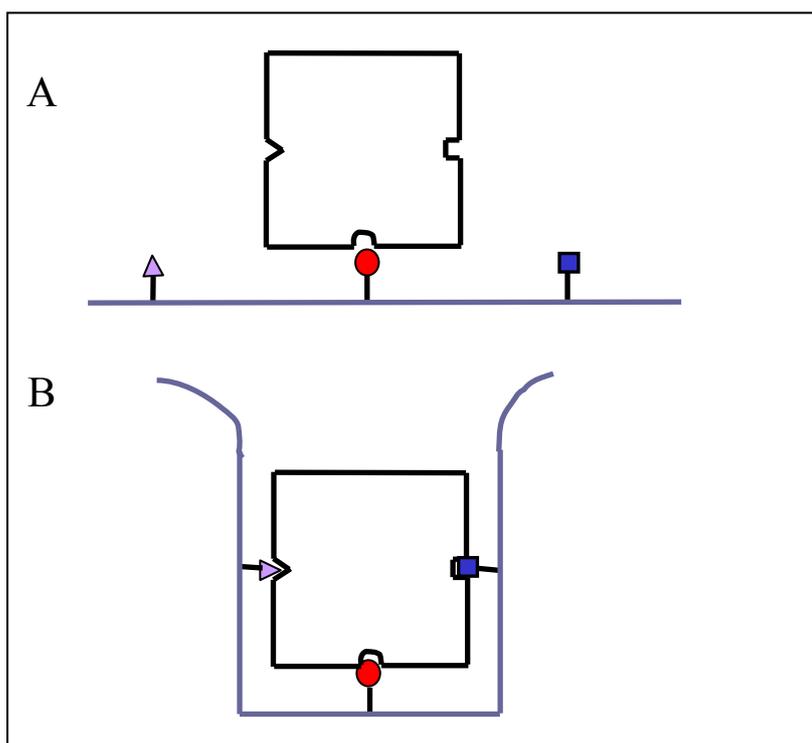
The difference in the chemical potential of an aliphatic chain with  $n$  carbon atoms between an apolar solvent and water is proportional to  $n$  at least for chains having less than 22 carbon atoms [18]:

$$\mu_{\text{Apol}}^0 - \mu_{\text{water}}^0 = \alpha - \beta.n \quad (10)$$

where  $\alpha$  and  $\beta$  are two positive constants.  $\alpha$  takes into account for the unfavorable effect the head group of amphiphiles has on its solubility in apolar solvents.

The fact that the reduction in free energy upon transfer from water to an apolar solvent is simply proportional to the chain length is clearly a “non specific” effect: the longer the aliphatic chain the less it is soluble in water.

**Figure 2.** Schematic representation of the difference in geometric disposition between three chemical groups able to interact with complementary receptor sites on a binding partner molecule allowing for only “non-specific” interactions (A) and “specific” interactions (B). Nevertheless “non-specific” interactions can also contribute to increase the binding affinity in the case of B because of desolvation of both molecules upon their contact. In the case of a given biomolecule one can go from situation B to A by a single conformational change.



With this in mind it is now clear that on the surface of:

- (i) a lipid vesicle (with a known chemical composition) even in the presence of phase boundaries (the so called “rafts”),
- (ii) on the surface of a mineral oxide,
- (iii) along a polyelectrolyte chain,
- (iv) along a single stranded oligonucleotide,

there are clearly no such defined recognition patterns. On the other hand, prosthetic groups of proteins like the well know protoporphyrin IX of hemoglobin are “specific” recognition motifs. The amino acids inside the channel of a membrane protein play also the role of a specific recognition motif.

The energetics of this kind of “specific” interactions has been reviewed in excellent fashion by many authors [19-21]. In this article we aim to review how microcalorimetry helps to determine the energetics of binding process implying non specific interactions. Such interactions are “ill defined” in the sense that there is not well defined localization and topology of the interacting chemical groups. In each investigated case, we will try to provide some relevant examples from the older as well as from very recent literature, but without the aim to be exhaustive. We will focus on interactions in which biomolecules are exposed to interfaces. Indeed in this situation, very common in biotechnology,

biomolecules having specific binding groups are exposed to chemical groups that do not display a configuration allowing for specific interactions to take place.

In general, there are plenty of experimental methods able to determine the binding constant between two interacting molecules:

- (i) NMR,
- (ii) other spectroscopic methods like fluorescence spectroscopy,
- (iii) sedimentation velocity and equilibrium,
- (iv) equilibrium dialysis [22] (which can be used only when the two binding partners have very different hydrodynamic radii and when one of them is able to diffuse across the pores of the dialysis membrane),
- (v) chromatography,
- (vi) capillary electrophoresis
- (vii) even electrospray mass spectrometry, ESI [23] (ESI measures the mass increase of the guest molecule upon binding in the dry state, which means that all the contribution of hydrophobic interactions are not taken into account)
- (viii) and of course, titration calorimetry [24].

Surface plasmon resonance can be used when one of the binding partners can be immobilized at a solid liquid-interface in contact with a noble metal. The collective modes of motions of the electrons (the surface plasmons) can be exploited to investigate the increase in refractive index which is the consequence of the binding process during which an accumulation of binding molecules occur at the interface [25].

In the next paragraph we will emphasize why calorimetry is really necessary to unravel the enthalpic and entropic contributions of binding processes. Finally, in the last and most important chapter we will highlight how ITC can help to investigate “non-specific” interactions (in the sense defined before) in the fields where molecules relevant to biology are exposed to an interface. Namely we will describe the use of ITC (and sometimes of differential scanning calorimetry, DSC) in the following subfields:

- (i) self assembly of amphiphiles,
- (ii) interactions between peptides-drugs with lipid membranes,
- (iii) proteins with surfaces,
- (iv) peptides with DNA as well as proteins or DNA with polyelectrolytes.

In all these cases the global enthalpy and entropy change which contribute to  $\Delta G^\circ$  [equation (1)] are the result of many subcontributions. The most challenging point, as already mentioned is to unravel each of these contributions. We will conclude by emphasizing the need to investigate very simple model systems to go further in this direction.

## 2. Some Other Fundamental Relationships and the Need to Measure the Enthalpy Change Independently from the Binding Constant

Assuming that the standard enthalpy and entropy changes are temperature independent, one easily derives the van't Hoff relationship from equations (1) and (3):

$$\frac{\partial \ln K}{\partial T} = \frac{\Delta H^\circ}{RT^2} \quad (11)$$

which shows, that the equilibrium constant increases upon a temperature increase for an endothermic process ( $\Delta H^\circ > 0$ ).

Upon the derivation of (11), *the assumption of constant standard enthalpy and constant standard entropy is of paramount importance* and has often been neglected in the literature [26]. It is nevertheless well known that most of the “non-specific” (as well as the “specific”) interactions are occurring with  $\Delta H^\circ$  and  $\Delta S^\circ$  being temperature dependent. This is also true for specific interactions as exemplified by the complexation of  $\text{Ba}^{2+}$  by 18-crown-6 ether (water being the solvent) [27].

When  $\Delta H^\circ$  is temperature dependant, the investigated transformation implies a change in the heat capacity of the whole system:

$$\Delta C_p = \left( \frac{\partial \Delta H^\circ}{\partial T} \right)_p \quad (12)$$

where the subscript  $P$  means that the transformation is investigated at constant pressure.

From equation (12) it is clear that after having measured the temperature dependence of  $C_p$ , one can also get the standard enthalpy change associated with the investigated process by means of integration:

$$\Delta H^\circ = \int_{T_i}^{T_f} \Delta C_p(T).dT \quad (13)$$

where  $T_i$  and  $T_f$  are the initial and final temperatures respectively.

Hence, DSC allows to measure the enthalpy of protein denaturation which provides an unestimable information about its conformational stability [28,29]. Indeed, upon denaturation, hydrophobic residues hidden from the solvent in the folded state become exposed to the solvent with an increase of the heat capacity [30].

Relying on the validity of the van'Hoff relationship, it appears that measuring the equilibrium constant of a given equilibrium at different temperatures will allow to calculate  $\Delta H^\circ$ . Before the availability of highly sensitive microcalorimeters, many investigators used the temperature dependency of the equilibrium constants to deduce the enthalpy change associated with the binding process. The use of equations (1) and (3) then allow to calculate the corresponding entropy change  $\Delta S^\circ$ . Very sensitive and fast responsive microcalorimeters now allow to alleviate this bias [26].

The knowledge of both  $\Delta H^\circ$  and  $\Delta S^\circ$  is of paramount importance to unravel the different contributions of any interaction process taking part in presence of a solvent (water). The desolvation of hydrophobic surfaces, the hearth of the hydrophobic effect [18,31,32], is a process that increases the number of accessible states of the water molecules and hence an increase in the whole entropy of the system. When one or both of the binding partners lose some of their degrees of motional freedom

(vibrational and/or rotational), the entropy of the system will decrease. Hence the global knowledge of the value of the entropy (enthalpy) change does by itself not give the value of its individual contributions [33]. Techniques complementary to calorimetry are thus necessary to decompose the enthalpy and entropy changes into their constitutive parts. This is indeed very challenging as we will see in the particular case of “non specific” interactions. For instance, NMR relaxation experiments allow to compare the mobility of a protein binding site before and after the binding event [34].

In addition to the purely thermodynamic relationships (1-13), there are some other non purely thermodynamic relationships that can be investigated empirically when the enthalpy and entropy changes upon binding are known. Among them, the enthalpy-entropy compensation phenomena [26] which occur not only in the case of “specific” interactions [12,21] but also in the case of protein adsorption at solid liquid interfaces or in the case of solute binding at fluid interfaces as we will see in the last part of this review.

The enthalpy-entropy compensation seems to be intrinsically associated with the fact that  $\Delta H^\circ$  and  $\Delta S^\circ$  are related to the heat capacity at constant pressure [35].

The enthalpy-entropy compensation expresses according to:

$$T.\Delta S^\circ = \beta + \alpha.\Delta H^\circ \quad (14)$$

Its validity has been often discussed on the basis of the lack in accuracy in the determination of  $\Delta H^\circ$  and  $\Delta S^\circ$ . However it is clear that if equation (14) holds true, it should have consequences on the thermodynamic Gibbs-Helmholtz relationship (1) which has then to be written as:

$$\Delta G^\circ = (1 - \alpha).\Delta H^\circ - \beta \quad (15)$$

Hence if one finds experimentally that  $T.\Delta S^\circ$  is a linear function of the standard enthalpy change with a slope  $\alpha$ , one has to check that the free energy change is a linear function of  $\Delta H^\circ$  with the expected slope  $1-\alpha$ . If this consistency test is not satisfied, there is no enthalpy-entropy compensation.

We will not summarize the working principle of modern isothermal titration calorimeters, because this has been extensively done elsewhere [24]. Let us just recall that there are many experimental designs of calorimeters: the hydration calorimeter [36], flow adsorption calorimeters [37,38] which are dedicated to investigate adsorption (often “non specific” phenomena).

The investigation of biophysical and biochemical processes requires the use of highly sensitive calorimeters able to measure heat fluxes of the order of some tens of  $\text{ncal}\cdot\text{s}^{-1}$  with an amount of biomolecules that should be (significantly) less than 1 mg. Indeed, if the standard enthalpy change is of  $10 \text{ kcal}\cdot\text{mol}^{-1}$  (ie  $42 \text{ kJ}\cdot\text{mol}^{-1}$ ) which is rather typical for biochemical processes, and if the protein concentration is  $1 \text{ mg/mL}$  (hence about  $10^{-5} \text{ M}$  assuming a molecular mass of  $10^5 \text{ g}\cdot\text{mol}^{-1}$ ) the total heat exchanged is of the order  $10^{-4} \text{ cal}$ . If the reaction (or titration) is lasting over 1 h, this means that the average heat flux the microcalorimeter should be able to measure is of the order of  $30 \text{ ncal}\cdot\text{s}^{-1}$ . Such sensitivities were not reached for a long time and the major technical evolution was realised only in 1989 [39].

It is not worth herein to describe how to operate such an ITC device nor to describe how to fit a binding model to the experimental data. The interested reader can read the review by O'Brien, Ladbury and Chowdhry [24].

It has to be noted that the last generation ITC devices have now sufficiently fast response to allow the investigation of thermal events occurring during enzymatic catalysis [40-42]. This opens the route for real time studies of a plethora of fascinating biochemical events in real time.

Even if we will occasionally speak about experiments done with differential scanning calorimetry (DSC) and pressure perturbation calorimetry (PPC) we will not describe their working principle. The interested reader can refer to reference [43-45] and [46] for DSC and PPC respectively.

### 3. Some Selected Examples of the Use of ITC to Investigate the Thermodynamics and Kinetics of Biophysical “Unspecific” Processes

According to the previously proposed definition of “non-specific” interactions we will now review the application of ITC (and occasionally of DSC and PPC) to the investigation of the energetics of “non-specific” processes in biophysical chemistry. We will describe phenomena of increasing complexity, where the increasing complexity corresponds to the implication of a greater number of subprocesses. All the investigated process occur at interfaces. We will review the use of microcalorimetry in:

- (i) the interactions between amphiphilic molecules
- (ii) the interactions between small ions with polyelectrolytes as well as between polyelectrolytes
- (iii) the interactions between drugs, peptides and viruses with lipid assemblies
- (iv) the interactions between proteins and solid surfaces.
- (v) the investigation of the global thermal effect of metabolic processes.

All these “non-specific” interactions are of prime importance to biology: let us briefly comment their relevance. The self assembly of lipids allows production of the compartmentalisation which is necessary for the appearance of life [7]. The interaction between charged molecules and single stranded or double stranded DNA is extremely important for the regulation of gene expression since these interactions lead to compaction of DNA [47-50] The same electrostatic interactions are used for the preparation of “complexes” between DNA and cationic species (we put quotes around the word complexes to emphasise that they are not of the same nature as the usual complexes in inorganic chemistry: they do not have a defined stoichiometry). The interaction between a polycation and DNA has to be strong enough to allow efficient DNA overcharging, a *sine qua non* condition for inducing endocytosis of the “complexes” but not too strong in order for the DNA to be liberated from its gene vector in the cytoplasm or in the lysosome [51]. This means that a deep thermodynamic understanding of polycation-DNA interactions is critical for a rational design of efficient gene vectors.

The interaction between drugs or peptides with biological membranes is at the heart of the transport of amphiphilic drugs across the lipid barrier and the interaction of venoms and viruses with cells [52]. Last but not the least protein adsorption is of tremendous importance in biomaterial science [53] and it most often induces conformational changes of the adsorbed proteins [54]. The investigation of such conformational changes on model surfaces may help to understand the fundamental mechanisms leading to the conformational transition of soluble prions (PrP<sup>C</sup>) to the pathological  $\beta$  sheet rich PrP<sup>SC</sup> [55,56].

We will not consider the thermodynamics of protein folding-unfolding, because it is a field by itself and because it is a *highly* “specific” process with uses some specific nucleation sites, the so called “molten globule” [57] as well some catalysts (chaperones) [58].

### 3.1. Investigation of the Interaction between Amphiphiles and between Amphiphiles and Polymers

Upon increasing the concentration of amphiphiles (carrying a polar headgroup and at least one hydrophobic tail) in water, after the solution-air interface is saturated with a monolayer, the amphiphiles are forced to be dissolved in water. But the hydrophobic moieties have to be shielded from water to minimise the free energy of the system. Hence the amphiphiles self assemble and there is a critical concentration, called the critical micelle concentration (*cmc*) after which all the added amphiphile is incorporated in the self assembled structures. In the case where the packing ratio, defined as the ratio between the volume of the hydrophobic part and its length multiplied by the area of the hydrophilic head [31], is lower than 1/2, hence when the amphiphile is cone shaped, the self assembled structure is a micelle. When the packing ratio is between 1/2 and 1, which typically occurs for double chained amphiphiles (and hence phospholipids and sphingolipids), the amphiphiles associate in the form of bilayers. When the packing ratio is greater than one, the stable aggregates are inverted micelles.

At a first order approximation, the value of the *cmc* allows to calculate the change in standard free energy upon micellisation, according to equation (17):

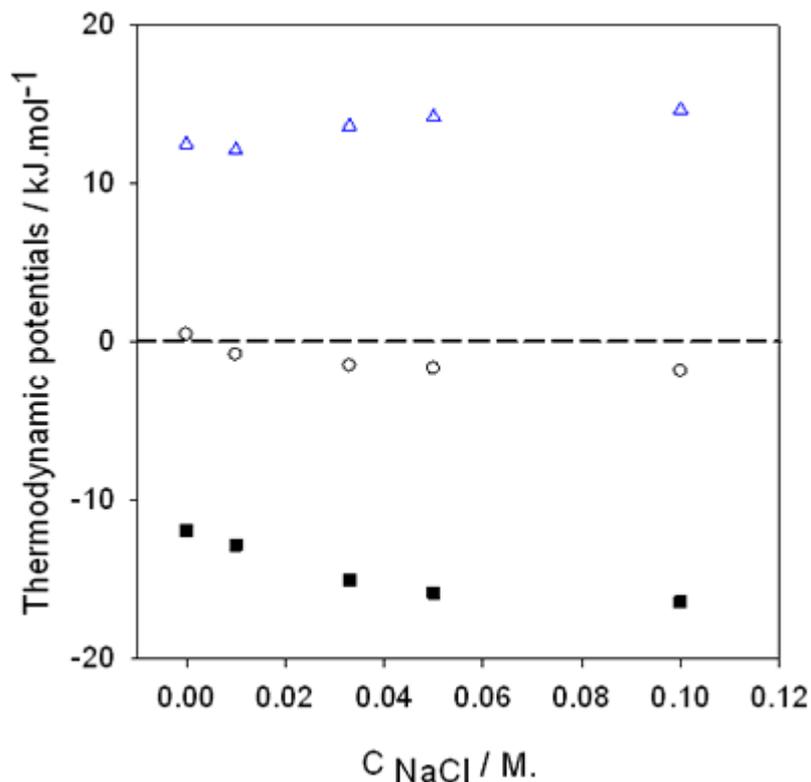
$$\Delta G_{micellisation}^0 \approx -R.T.\ln(cmc) \quad (16)$$

There are a plethora of experimental techniques allowing to measure the *cmc*, as for instance light scattering, fluorescence spectroscopy, conductometry (applicable only in the case of ionizable head groups) and the use of selective electrodes [59].

Isothermal calorimetry has been used to estimate the enthalpy of micellisation [60,61]. To that aim the amphiphile is solubilized at a concentration above its *cmc* and it is diluted in the cell of the microcalorimeter. It appears that the enthalpies of micellisation are often positive, the process of micelle formation is endothermic. This endothermicity is the balance between several contributions: The association between the hydrocarbon tails ( $\Delta H_{ass} \leq 0$ ), their dehydration, ( $\Delta H_{desolvation} \geq 0$ ), and the repulsion between the hydrophilic headgroups, ( $\Delta H_{head} \geq 0$ ), which is of particular importance in the case of charged amphiphiles. Since the sum of these contributions is endothermic, the repulsion between the headgroups and the desolvation of the hydrophobic tails outweighs the exothermic contribution due to the favourable chain-chain attraction. This is characteristic of the hydrophobic effect.

Nevertheless the micelle formation is a spontaneous process, implying that the entropy change is positive. Again this is expected for a process ruled by hydrophobic interactions [62]. The knowledge of the *cmc* and hence of free energy of micelle formation, equation (16), and the measurement of the enthalpy of micellization, allow to calculate  $T.\Delta S_{micellisation}^0$ . Figure 3 displays the data taken from the *cmc* measurement of Newberry [59] and the calorimetry data from Birdi [60] in the case of the most used amphiphile, sodium dodecyl sulfate (SDS).

**Figure 3.** Thermodynamic data describing the micellisation of sodium dodecyl sulfate as a function of the NaCl concentration and at 298 K. Data taken from Refs. [59] and [60]. (○):  $\Delta H_{micellisation}^0$ , (△):  $T \cdot \Delta S_{micellisation}^0$ , (■):  $\Delta G_{micellisation}^0$ . The dashed line corresponds to a process implying no change in energy.

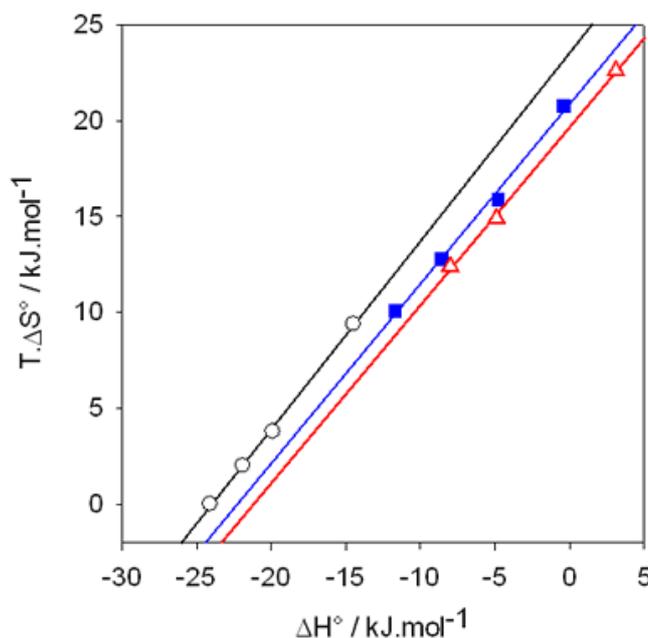


It appears from Figure 3 that the absolute value of  $T \cdot \Delta S_{micellisation}^0$  provides the major contribution to the free energy change. The finding that the micellization process is endothermic is not general, nevertheless the increase in entropy upon micellization is a general observation. There are other studies in the literature dealing with the use of isothermal microcalorimetry to investigate the formation of micelles [61-65]. ITC has been used not only to measure the enthalpy associated with the demicellization process, but also the value of the *cmc* itself [64]. The change in the nature of the counterion of alkylpyridinium surfactants has profound effects on the value of the *cmc* and the change in temperature has effects on the sign of  $\Delta H_{micellisation}^0$  (Figure 4) [65]. In addition there is an enthalpy-entropy compensation effect [equation (14)] with a slope  $\alpha$  almost equal to 1 whatever the counterion of the alkylpyridinium surfactant. This implies that the free energy change should be a constant (according to equation (15)), which coincides with the experimental finding [65].

ITC has also been employed to investigate the association of amphiphilic polyelectrolytes (like poly-(2-acrylamido)-2-methylpropanesulfonic acid) [66] as well as the interactions of poly(amidoamine) dendrimers with surfactants (the negatively charged SDS as well as cetyltrimethylammonium bromide, CTAB) [67]. This later study is of particular interest because it combines different experimental techniques like ITC, SDS selective electrodes and small angle neutron scattering to investigate the structure of surfactant- dendrimer aggregates.

The thermodynamics of polymer-surfactant vesicles has also been considered from the point of view of phase diagrams. This aspect has been reviewed recently [68].

**Figure 4.** Enthalpy-entropy compensation plots for the micellization of alkylpyridinium surfactants as a function of the used counteranion: (○): I<sup>-</sup>, the slope of the linear regression is  $\alpha=0.98$ , (■): Br<sup>-</sup>,  $\alpha=0.93$ , (△): Cl<sup>-</sup>,  $\alpha=0.93$ . The ITC experiments were performed between 303 and 333 K. Data taken from Ref. [65].



In the case of double layer forming amphiphiles the energetics of self-association is more complicated to investigate owing to their very low *cmc* value (typically of the order of  $10^{-8} - 10^{-9}$  M). There are however many DSC investigations aimed to investigate the phase transition from the ordered liquid crystalline to the gel phase transition [69-70]. The hydration thermodynamics of saturated phospholipids (with aliphatic chains carrying 12, 14 or 16 carbon atoms) has been investigated by means of ITC [36]. It has been measured that the association of the 3 first hydration molecules to dehydrated lipids carrying phosphorylcholine head groups is exothermic (typically  $-16 \pm 2$  kJ·mol<sup>-1</sup>) whereas the association of further water molecules is endothermic. This endothermicity has been attributed to the water induced melting of the phospholipid from the liquid crystalline to the gel phase.

PPC has been used to investigate the changes in the specific volume of 1,2-dimyristoyl-*sn*-glycero-3-phosphocholine (DMPC) during its pre-transition and during its main phase transition [71]. The influence of surfactants in the formation of domains in lipid bilayers has also been studied with PPC [72].

ITC has also been used to investigate the effect of osmotic stresses on the area changes of lipid membranes. When water is uptaken by vesicles in contact with an hyper-osmotic solution the vesicles undergo a lateral stretching accompanied by an uptake of thermal energy [73].

### 3.2. Investigation of the Interactions between Small Ions and Polyelectrolytes as well as between Polyelectrolytes

The interaction between charged colloids in aqueous solution is particularly important in biology and its investigation is challenging because of its complexity. The interactions are not purely electrostatic and one has not to forget that each charged colloid or macromolecule is surrounded by a diffuse electrical double layer as well as some strongly bound counterions. Desolvation is also very important, as for amphiphiles. The condensation of counterions to charged macromolecules, which we already mentioned, occurs when its linear charge density exceeds a critical value [10,74]. Such a condensation phenomenon has been observed experimentally for a lot of synthetic polyelectrolytes as well as for DNA. Upon the interaction of two oppositely charged polyelectrolytes, at low salt concentration of the solution (i.e. at low ionic strength) one frequently observes an increase in the conductivity of the solution [75,76] which is due to counterion release. Indeed upon formation of “complexes” between two oppositely charged polyelectrolytes, some of these counterions have to be removed from the contact region between the interacting species. The counterion condensation can be so strong that it can lead to charge inversion of the polyelectrolyte [77,78]. There has been considerable effort to investigate the mechanisms of polyelectrolyte-polyelectrolyte interactions [79] in terms of the influence of polymerisation degree,  $pH$  in the case of weak polyelectrolytes (among which belong proteins) [80], charge density [81-84], and the presence of low molecular weight electrolytes aimed to screen the electrostatic forces [85]. The structure of such complexes [86-90] as well as their dynamics [82,91-95] has also been intensively investigated. Proton pulsed field gradient NMR has been used to demonstrate that the complexes between poly(diallyldimethylammonium chloride) and bovine serum albumin (BSA) can disintegrate and that dense domains may reform depending on the interaction strength between both partners [91]. Depending on the nature of the polycation used to build complexes with DNA, these complexes can be redissolved by means of an increase in ionic strength [93]. The dissolution efficiency at a given ionic strength depends on the nature of the salt, the most efficient being those containing a cation that strongly interacts with DNA,  $Ca^{2+}$  for instance [94]. Even more important is the observation that the DNA may be displaced from the DNA-polycation complexes by means of a polyanion that has a stronger affinity with that polycation than DNA itself [95].

It appears that the most important phenomenological parameter determining the morphology, the charge state and hence the solubility of the complexes as well as their dynamics, is the mixing ratio,  $r$ , i.e. the ratio between the number of moles of cationic groups and the number of moles of anionic groups. In most (but not) all cases, phase separation between a complex rich and a complex poor phase occurs when  $r$  is close to 1.

From a theoretical point of view some progress has been made in unravelling the fundamental mechanism of inter-polyelectrolyte complex formation [96-99]. The observation of selectivity effects in the polyanion binding to a given polycation highlights the need to investigate the thermodynamics of the complexation process. The number of investigations aimed to determine the binding constant of the polyelectrolyte-ion or polyelectrolyte-polyelectrolyte complexes are pretty scarce [95,100-104]. Among the most efficient methods to directly measure binding constant are fluorescence quenching methods: Lohman's group investigated the interactions between positively charged lysine

oligopeptides modified with a tryptophan residue and various oligonucleotides. The binding event causes a total quenching of the tryptophan fluorescence emission [102]. In the case of complexes implying DNA it is possible to use the fluorescence emission properties of ethidium bromide (EtBr): In the DNA intercalated state it is strongly fluorescent but upon complexation with a polycation, EtBr is removed from DNA and its fluorescence quantum yield is dramatically reduced [93,95].

The binding isotherms obtained give the amount of bound molecules to their binding partner as a function of the concentration of unbound molecules. These isotherms have to be fitted to a binding model [2,105-107] which yields the equilibrium constant or a set of microscopic equilibrium constants in the case of cooperative interactions. Before the use of microcalorimetry, van't Hoff analysis of the temperature dependence of the equilibrium constant(s) was used to estimate the enthalpy change upon binding.

As in the case of interactions between amphiphiles, there are many sub-processes contributing to the enthalpy and entropy changes: hydration changes, changes in the conformation of the polyelectrolytes and of course electrostatic effects. Owing to the presence of counterions around the polyelectrolytes, these electrostatic interactions are always the result of a competition between the counterions bound to each partner before their interaction and the electrostatic bonds formed in the final state. Indeed, this competition is used in the fluorescence quenching assays using EtBr [93,95]. The importance of counterion release to the free energy change upon polyelectrolyte-polyelectrolyte binding can be estimated by studying the influence of ionic strength: its increase produces a decrease in affinity not only because the electrostatic interactions between the polyelectrolytes are screened but also because of entropic effects [108].

The dependence of the binding constant with respect to the concentration of the supporting electrolyte is given by:

$$\frac{\partial(\log K)}{\partial C_{\text{electrolyte}}} = -z.\psi \quad [17]$$

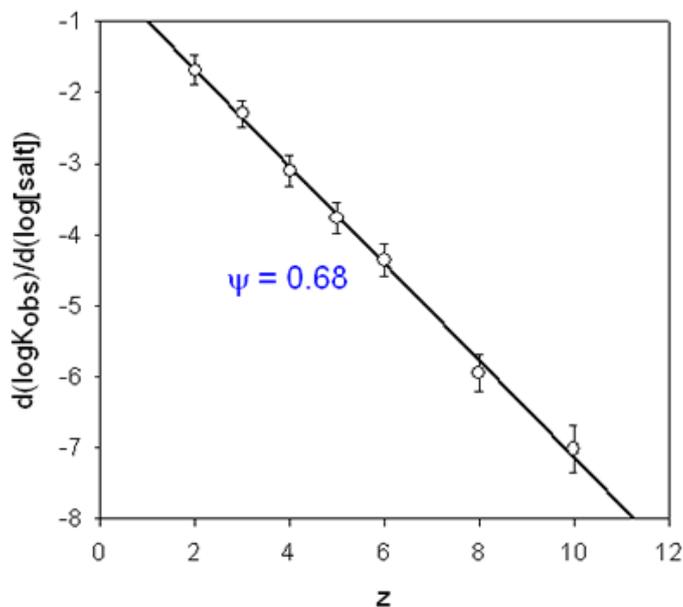
where  $z$  is the valence of the interacting polyelectrolyte with an oppositely charged binding partner, the "receptor" (of higher valency), and  $\psi$  is the average number of counterions released by a charged group of the "receptor" polyelectrolyte. A general derivation of equation [17] can be found on pages 871-873 of reference [2]. An example of such an analysis of the binding data between a series of oligolysines (modified with a single tryptophan residue to monitor fluorescence quenching) and single-stranded homopolynucleotides (polyU) is displayed in Figure 5 [109]. This plot shows that on average 7 potassium counterions are lost by every 10 phosphate group of polyU upon its binding with Trp-(Lys)<sub>*n*</sub> ( $2 \leq n \leq 8$ ).

Additional examples of such counterion release phenomena can be found in the literature [110-112]. In most of these studies, the enthalpy and entropy changes have been calculated from a van't Hoff analysis of the data [equation (11)] with some exceptions however, where the enthalpy changes were measured directly by means of ITC [111]. When changing the NaCl concentration, the enthalpy change associated with the single-stranded binding tetramer and (polyT)<sub>69</sub> follows the following law [111]:

$$\Delta H_{obs} = \alpha \cdot \log[NaCl] + \beta \quad (18)$$

with:  $\alpha = 46.3 \pm 1.8 \text{ kcal} \cdot \text{mol}^{-1}$  and  $\beta = -109.8 \pm 0.9 \text{ kcal} \cdot \text{mol}^{-1}$ .

**Figure 5.** Variation of the logarithm of the Trp-(Lys)<sub>n</sub> ( $2 \leq n \leq 8$ )-polyU binding constant as a function of the valence of the polypeptide. The slope of the straight line yields  $\psi=0.68$ , according to equation (17). Data from Table 1 of reference [109].

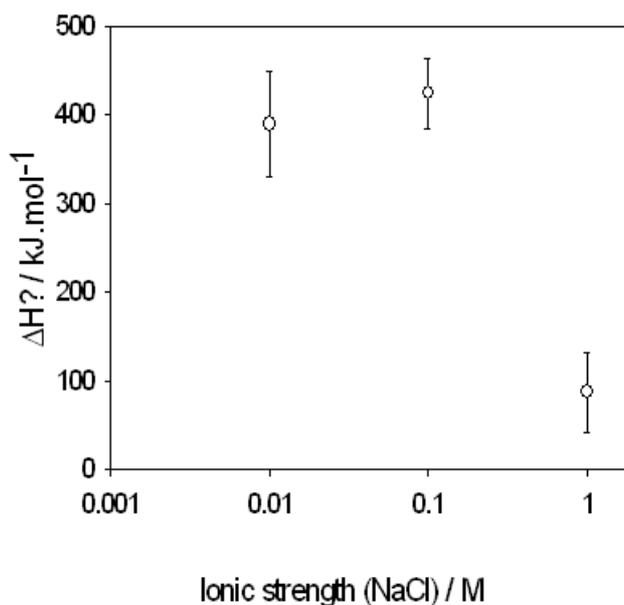


These experimental data are in reasonable agreement with those obtained from a van't Hoff analysis but not identical [111]. At low ionic strength, the interaction enthalpy is exothermic and decreases in absolute value when the ionic strength increases. The same trend has been observed for the interactions between bovine serum albumin (BSA) and poly(allylamine) (PAH) in conditions where the protein and the polycation are oppositely charged (10 mM Tris buffer,  $x$  M NaCl at  $pH$  7.4) [113], Figure 6. In this case, the interaction enthalpy was *endothermic*, which clearly shows that the BSA-PAH complexation process is driven by an increase in entropy. Unfortunately, a whole titration curve could not be obtained by means of ITC because of phase separation phenomena occurring upon an increase in the BSA/PAH ratio. This seems to be a recurrent difficulty in the investigation of polyelectrolyte–polyelectrolyte complexation, even if some data are available [114–116]. It appears that the inter-polyelectrolyte complexation process is driven through an increase in entropy, as was already suggested very early in the literature [117]. In addition, the ITC binding curves have been interpreted *with a very simple and unrealistic binding model*: a one to one stoichiometry between anionic and cationic sites. This model totally neglects cooperative binding effects as well as a possible mismatch between the cationic and anionic sites. From this point of view it seems urgent to perform ITC titrations as well as measurement of the binding constant by an independent method (for instance fluorescence quenching) in the case of monodisperse polyelectrolytes of variable charge density. Charged homopolypeptides (cationic: (Lys)<sub>n</sub>, anionic (Glu)<sub>n</sub> or (Asp)<sub>n</sub>) as well as aliphatic  $n,n$ -ionenes [93] seem to be very promising candidates to achieve this aim.

For a whole set of polycation-polyanion combinations it has been found that the enthalpy change upon complexation turns from exothermic to endothermic upon an increase in salt concentration [118]. These data have been obtained from ITC in the case where the mixing ratio was small (hence assuming that all the injected moles of anions find a positively charged binding partner). This trend was correlated with a change in the growth regime of layer-by-layer polyelectrolyte multilayer films from a linear growth at low salt concentration to an “exponential growth” at higher salt concentration. The polyelectrolyte multilayer films do not grow anymore above a critical ionic strength [118]. This observation may be correlated with the dynamics of the interpolyelectrolyte complexes as recently suggested by Cohen Stuart *et al.* [92]: the complexes seem to be in a frozen state at low salt concentration and highly hydrated and flexible at high salt concentration.

The interactions between synthetic polyelectrolytes and water [119], as well as the interactions between DNA and ions [120-122] or between proteins and ions have been investigated by means of ITC [123,124].

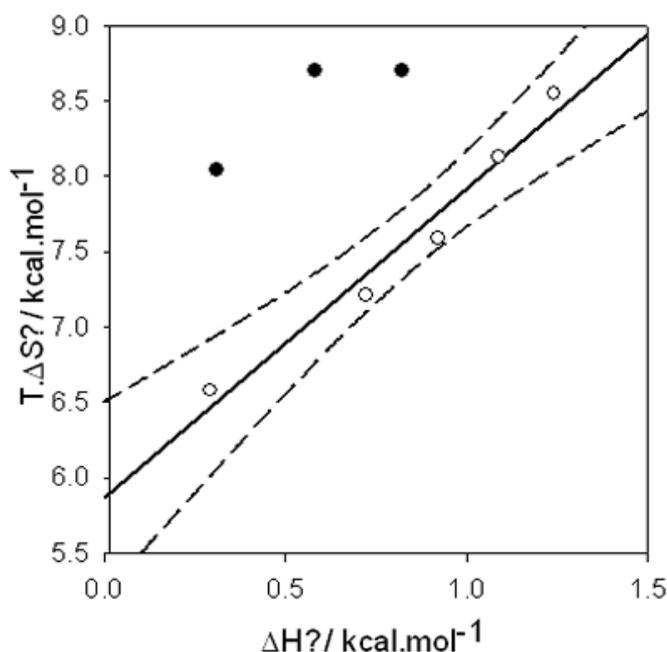
**Figure 6.** Variation of the binding enthalpy between BSA and PAH as a function of the ionic strength, as obtained from ITC [113].



The dilution heat of polystyrene sulfonate [119] as well as of other polyelectrolytes [118,123] is endothermic as expected from the counterion condensation theory [10]. The interaction between multivalent ions like cobalt hexaamine and circular pUC118 DNA displays a biphasic behavior, both events being endothermic. The first one is associated with the binding of  $Co(NH_3)_6^{3+}$  to isolated phosphate groups whereas the second one is associated with the cation binding induced condensation of DNA. The transition from the first to the second binding regime is shifted to higher  $\frac{Co(NH_3)_6^{3+}}{phosphate}$  ratios when the NaCl concentration is increased. This reflects again a competition between  $Na^+$  and  $Co(NH_3)_6^{3+}$  for the phosphate groups of DNA [121]. Most interestingly, the trivalent spermidine cations are less efficient than  $Co(NH_3)_6^{3+}$  to induce condensation of DNA, which is expected on the basis of the higher charge density of  $Co(NH_3)_6^{3+}$ . Of additional interest is the fact that

the first binding event displays an enthalpy-entropy compensation phenomenon whereas this seems to be hardly the case for the second one (Figure 7). The same kind of biphasic titration has been found during the investigation of the interactions between cetyltrimethylammonium bromide and DNA [122].

**Figure 7.** Enthalpy-entropy compensation plot for the ITC data of Bloomfield *et al.* [121] describing the two interaction regimes between  $Co(NH_3)_6^{3+}$  and DNA. Enthalpy and entropy changes associated with: (○)  $Co(NH_3)_6^{3+}$ -pUC118 binding and: (●) condensation of pUC118. The full and dashed lines correspond to the linear regression and the limit of the 95 % confidence interval respectively.



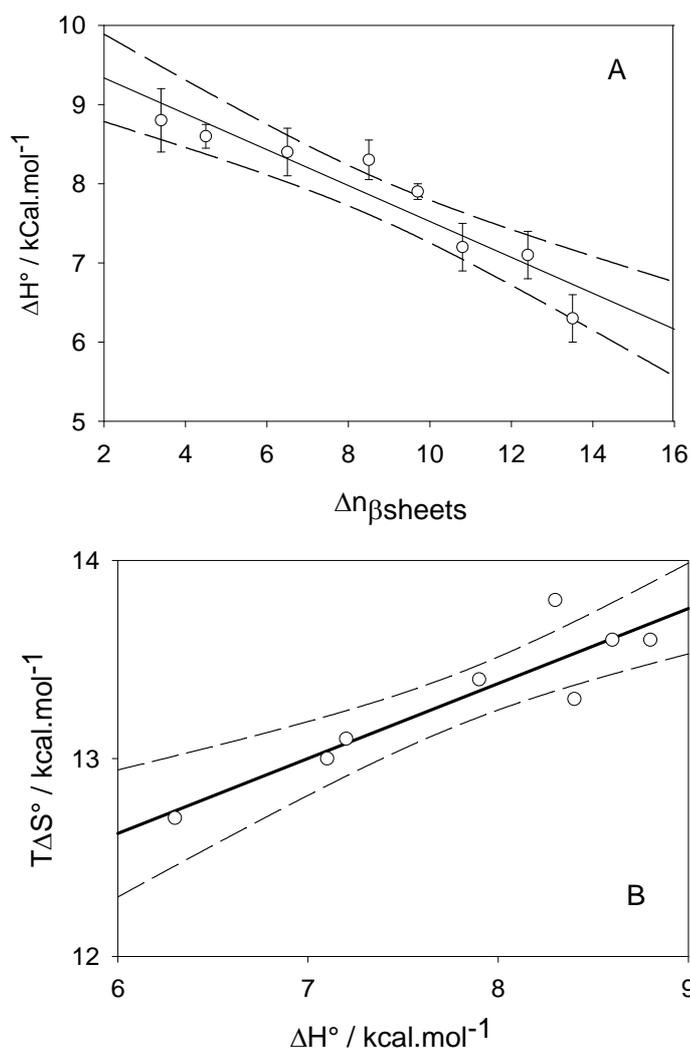
We will now shift to the description of the use of ITC to the investigation of drug-lipid assemblies interactions. We will also describe the interactions between charged molecules (among which polypeptides, polyelectrolytes and viruses) and lipid assemblies.

### 3.3. Investigation of the Interactions between Drugs, Peptides and Viruses with Lipid Assemblies

Less attention will be given on these kinds of interactions than on those occurring upon inter-polyelectrolyte or small ions-polyelectrolyte interactions, because very good reviews are already available [124-126] in addition to a plethora of research articles [127-141]. The interactions taking place at the surface of lipid membranes imply not only electrostatic interactions, of the same nature as those described in the previous paragraph, but also some conformational changes, as well as some partitioning events between the aqueous phase and the membrane phase, and eventually some membrane fusion events. NMR in addition to circular dichroism (CD) investigations will allow to estimate the contribution of conformational changes to the binding process [135-137]. In the case of (KIGAKI)<sub>3</sub> polypeptides (K, I, G and A are the one letter representation of lysine, isoleucine, glycine and alanine respectively) having some L-enantiomers of alanine substituted by D-enantiomers and interacting with POPE/POPG/pegylated POPE (70/25/5 mol%) vesicles, it has been found that the

peptides bound to the vesicles undergo a progressive conformational transition to  $\beta$  sheets. CD has been used for this aim. The enthalpy of binding is endothermic, meaning that the binding process is driven by a global increase in entropy and  $\Delta H^\circ$  is directly proportional to the increase in the number of amino acids that become incorporated in a  $\beta$  sheet structure (Figure 8) [137].

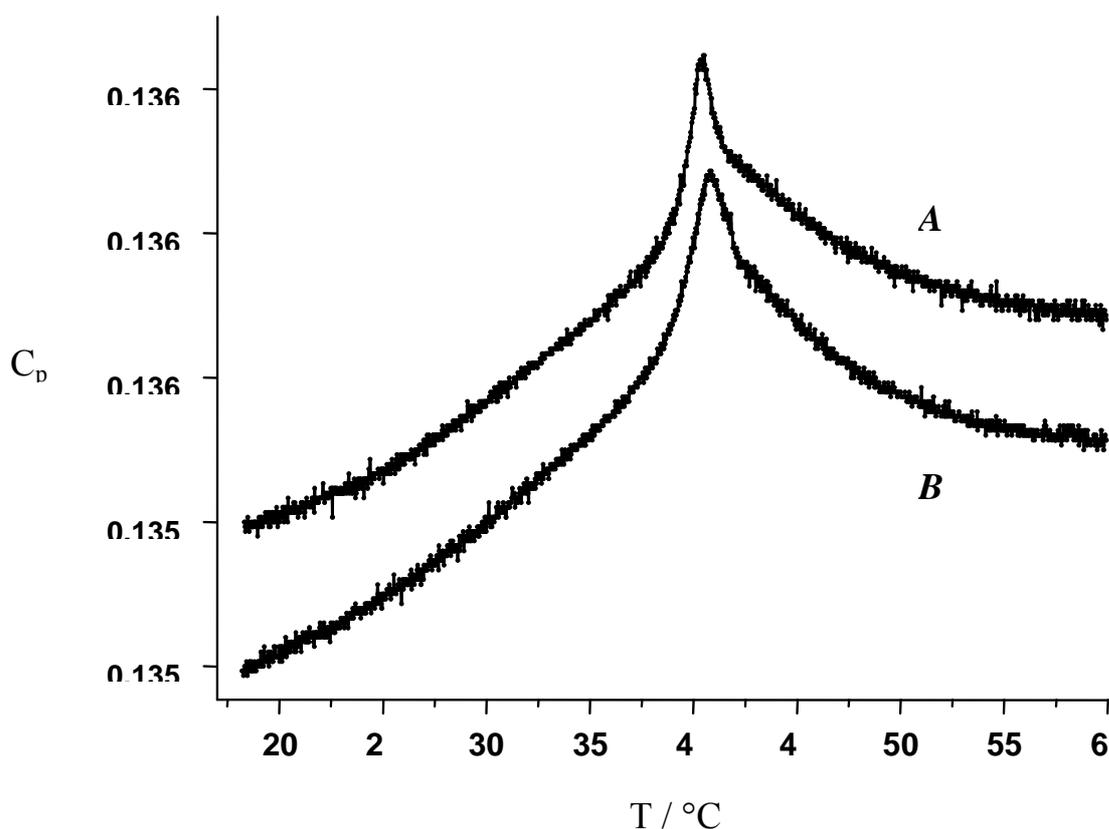
**Figure 8.** Thermodynamic data describing the interactions between (KIGAKI)<sub>3</sub> peptides (in 5 mM cacodylate buffer at pH 7.5) and small unilamellar vesicles made of POPE/POPG/pegylated POPE (70/25/5 mol%). Part A: relation between the enthalpy change (recorded from an ITC titration) and the increase in the number of amino acids implied in  $\beta$  sheet structures (obtained from CD spectroscopy). The full line corresponds to a linear regression to the data ( $r^2=0.89$ ) whereas the dashed line corresponds to the limit of the 95 % confidence interval. Part B: Enthalpy-entropy compensation plot corresponding to the same peptide/vesicle system. The full line corresponds to a linear regression to the data ( $r^2=0.83$ ) whereas the dashed line corresponds to the limit of the 95% confidence interval. Data taken from Ref. [137].



In general, the contribution from electrostatic interactions and from hydrophobic interactions can be separated when the charge state of the binding molecule is known, using for instance a modified form of the Gouy-Chapman theory [142]. In a very interesting investigation, it has been demonstrated that the interaction between magainin-2-amide with membranes made from 1-palmitoyl-2-oleoyl-sn-glycero-3-phosphocholine (POPC) (75 mol%) and 1-palmitoyl-2-oleoyl-sn-glycero-3-phosphoglycerol (POPG) displays a biphasic trace: at low peptide to lipid ratios, the enthalmograms obtained by ITC reflect the peptide binding process ( $-17 \pm 1 \text{ kcal}\cdot\text{mol}^{-1}$ ) whereas at high peptide to lipid ratios an endothermic process ( $6.2 \pm 1.6 \text{ kcal}\cdot\text{mol}^{-1}$ ) is due to the peptide induced pore formation. ITC has also been used to investigate the fusion of the Influenza virus with vesicles and a biphasic binding process was also monitored [145].

Very interestingly there are some drug-vesicle interactions that are of purely “specific nature” [133].

**Figure 9.** DSC traces of large unilamellar vesicles made from a DPPC/DPPG/CL mixture (80/10/10 w/w) in the absence (A) and in the presence of adsorbed PLL (B). Modified from reference [144].  $C_p$  is given in  $\text{kCal}\cdot\text{mol}^{-1}\cdot\text{K}^{-1}$ .



DSC is also very useful to estimate the conformational destabilization of proteins upon their interaction with membranes [138] as well as to answer the question if polyelectrolytes interact with charged membranes with a perturbation [143] or not of the membrane integrity [144]. The former phenomenon seems to occur when the polyelectrolyte carries hydrophobic side chains whereas the later occurs for non modified poly-L-Lysine (PLL) interacting with large unilamellar vesicles made from a DPPC/DPPG/CL mixture (80/10/10 w/w) [144]. In this case the DSC trace of the PLL

decorated vesicles is identical (Figure 9) to that of the pure dipalmytoyl phosphatidylcholine/dipalmytoyl phosphatidylglycerol/ cholesterol (CL) mixture, reflecting that the main phase transition of the lipid mixture (here at 41 °C) is not modified by the presence of the adsorbed PLL (charge inversion of the vesicles upon PLL adsorption has been demonstrated by means of zeta potential measurements).

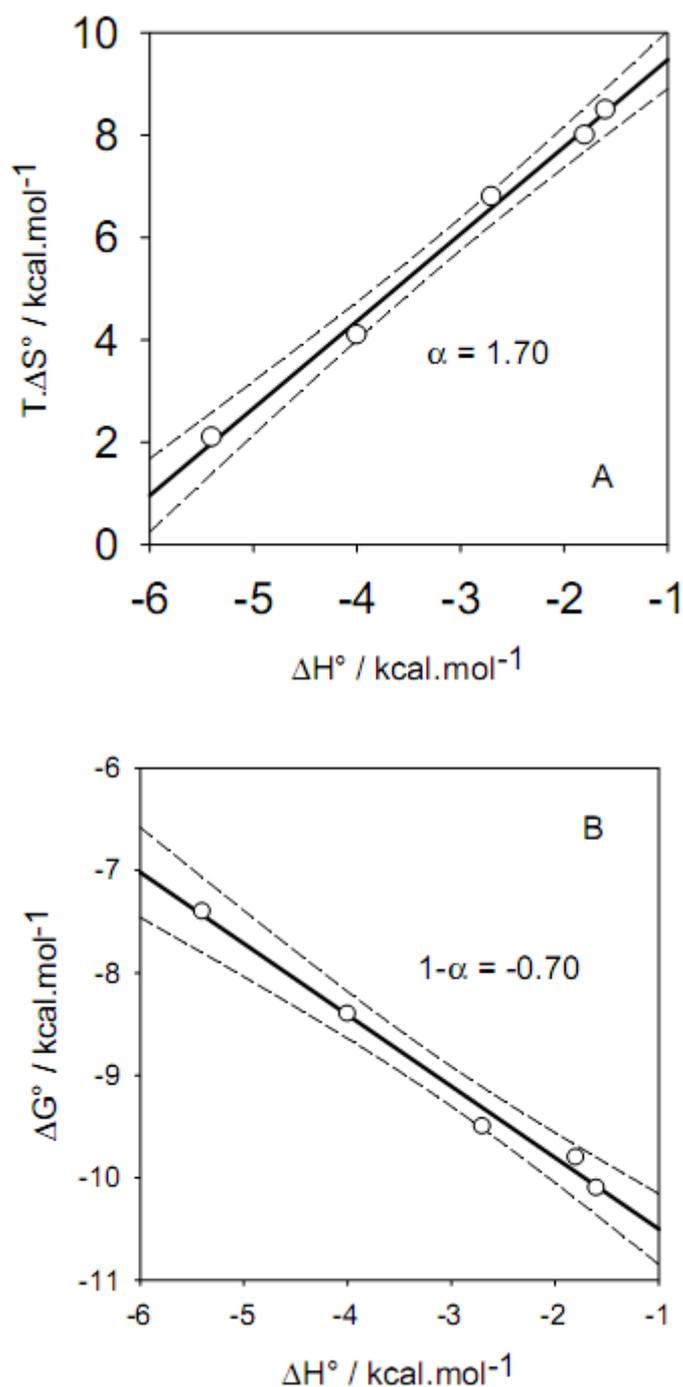
#### 3.4. Investigation of the Interactions between Proteins and Solid Surfaces

As already mentioned, the interactions between proteins and solid surfaces are extremely important in modern technology, for instance in fouling processes and in biomaterials science. Chromatographic analysis of amino acid retention on solid supports has allowed investigation of the adsorption behaviour of single amino acids on solid surfaces [146], but extrapolation to polypeptides and to proteins is difficult because of the complexity of the process. Major advances have been made in the understanding of this very ubiquitous phenomenon by Norde [147-149]. ITC as well as DSC played a major contribution in this research. It was found that proteins can be classified mostly into two categories with respect to their adsorption behaviour at solid/liquid interfaces: the classification between “hard” and “soft” proteins refers to the difference in free energy between the unfolded and folded conformations [147]. In general “soft” proteins are able to adsorb at any kind of sorbent even if it is hydrophilic and electrostatically repulsive, whereas “hard” proteins, having a high conformational stability, only adsorb at hydrophilic surfaces in the case of favourable electrostatic interactions. At hydrophobic surfaces, dehydration of that surface is usually the dominant driving force for adsorption, so that both “hard” and “soft” proteins adsorb, even under electrostatically adverse conditions. Clearly, DSC is extremely useful to distinguish between “hard” and “soft” proteins. There are many examples in which protein adsorption at solid/liquid interfaces is driven through an increase in entropy. Dehydration of the sorbent and of the protein surface (which is never purely hydrophilic, [147]) as well as partial protein unfolding are at the origin of this entropy increase. The combination between DSC and infra red spectroscopy [150] as well as between IR spectroscopy and hydrogen-deuterium exchange mass spectrometry [151] allows to directly correlate the thermodynamic decrease in protein stability at the surface to the change in its average conformation.

Recently, much effort has been devoted to the investigation of protein adsorption on the stationary phases of chromatographic columns [152-156]. Even if the enthalpy changes upon adsorption have been directly measured in some cases, most of the investigations rely on the fit of an adsorption model to the adsorption isotherm. This was done to calculate the adsorption equilibrium constant. Such purely empirical fitting of the adsorption isotherms, using for instance the Langmuir isotherm may be very arbitrary in the sense that this model totally neglects the interactions between the adsorbed proteins (see reference [17] and references therein).

ITC data of protein adsorption at colloid particles have also revealed enthalpy-entropy compensation relationships [157-158], Figure 10. It has been demonstrated by performing the ITC experiments in buffers having different ionisation enthalpies (phosphate, Tris and TES buffer) that every single protein adsorption event is accompanied by the incorporation of one proton in the adsorbed layer [157].

**Figure 10.** A: Enthalpy-entropy compensation plot for the adsorption of statherin onto hydroxyapatite particles (having a specific surface area of  $53 \text{ m}^2\cdot\text{g}^{-1}$ ) at different temperatures (between 15 and  $37^\circ\text{C}$ ) in the presence of phosphate buffer. Data from Table 1 of reference [157]. The slope of the linear regression curve ( $r^2=0.995$ ) is  $\alpha=1.70$ , calculated according to equation (14). B: correlation between the change in standard free energy upon adsorption with the enthalpy change. The slope of the linear regression curve ( $r^2=0.989$ ) is equal to  $-0.70$  in full agreement with the  $\alpha$  value obtained in part A and with equation (15), showing that there is a “true” enthalpy-entropy compensation. The dashed lines represent the limits of the 95 % confidence intervals.



With the aid of ITC it has been demonstrated recently that the interaction between salivary proteins and *Streptococcus Mutans* is a non specific process when the microorganism is depleted of its specific surface antigens [159].

### 3.5. Investigation of the Global Thermal Effect of Metabolic Processes

Very interestingly, microcalorimetry has been used to investigate the heat exchanges implied in extremely complicated processes such as the metabolisms of living cells [161,162]. It is possible to distinguish the exponential growth phase of cells from the initial lag phase with a single microcalorimetry measurement. This offers the opportunity to compare the metabolism of different cell lines, and possibly the difference between health cells and cells implied in a pathological process.

## 4. Conclusions and Perspectives

In this review article we have recalled the difference between “specific” and “non-specific interactions” and have emphasized how difficult it is to distinguish between both interaction modes. Based on many data from the biophysical and biochemical literature (as well as from supramolecular chemistry) it appears possible that many interactions have contributions coming from “non-specific” interactions. These “non-specific” contributions originate mostly from electrostatic and hydrophobic interactions. We have then shown that ITC (as well as DSC) gives reliable enthalpy and entropy changes of “non-specific” binding events. We focused on interactions between amphiphiles, amphiphiles and polymers, polyelectrolyte-polyelectrolyte, polyelectrolyte-small electrolytes, molecules (drugs, peptides) and lipid membranes and proteins with surfaces. It appears that the field of “ligand” binding at membrane/aqueous solution interfaces is the most mature of these fields in the sense that it is possible to unravel different contributions to the global enthalpy and entropy changes. The complete understanding of the interactions between polyelectrolytes is challenging in order to improve the efficiency of gene transfection and surface coating by the layer-by-layer deposition. It appears that even if ITC provides now accurate values of enthalpy changes, it will be extremely difficult to quantify the (positive) entropy changes upon complexation owing to the fact that phase separation occurs when the inter-polyelectrolyte complexes become electroneutral. Hence the determination of binding constants by traditional titration methods, for instance fluorescence spectroscopy, coupled with ITC measurement of enthalpy changes will allow to gain better understanding in the thermodynamics of such fascinating (but ill defined) processes. It is also mandatory to investigate complexation processes between extremely well characterised and monodisperse polyelectrolytes to unravel the contributions from counterion release and those from conformational changes upon inter-polyelectrolyte complexation. The combination of purely experimental approaches with simulations (Monte Carlo as well as molecular dynamics) will also be a source of progress in understanding the “non-specific” interactions between polyelectrolytes. In all the investigated cases, interesting enthalpy-entropy compensations were observed. Some more research is needed to understand their origin.

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